

Fundamental and IVUS measurement

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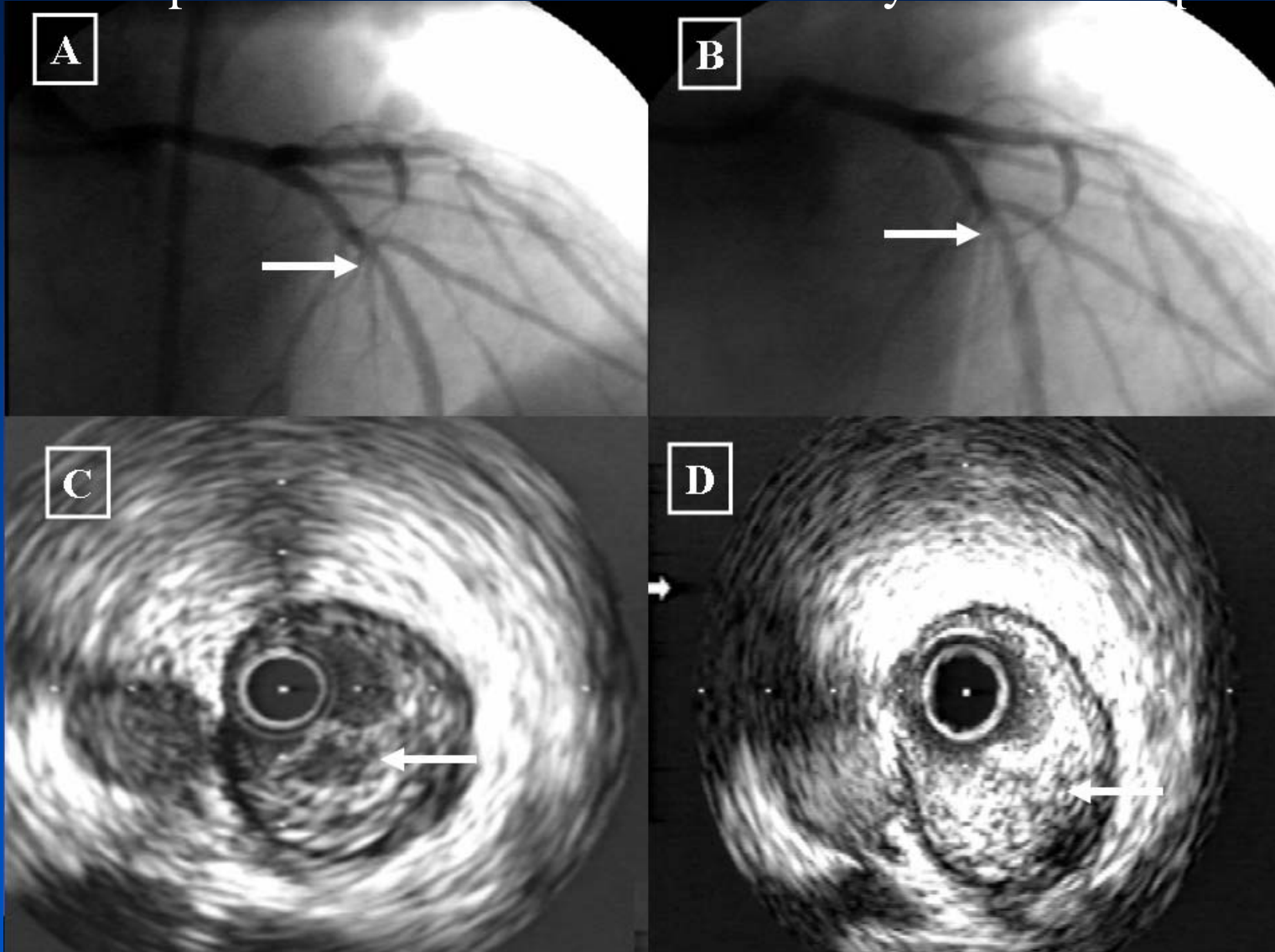
University of Ulsan College of Medicine

Asan Medical Center, Seoul, Korea

We needed another method

Index procedure

1-year follow-up



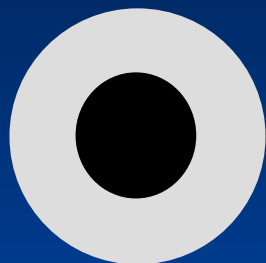
We needed another method

Cross Section

RAO View

LAO View

A



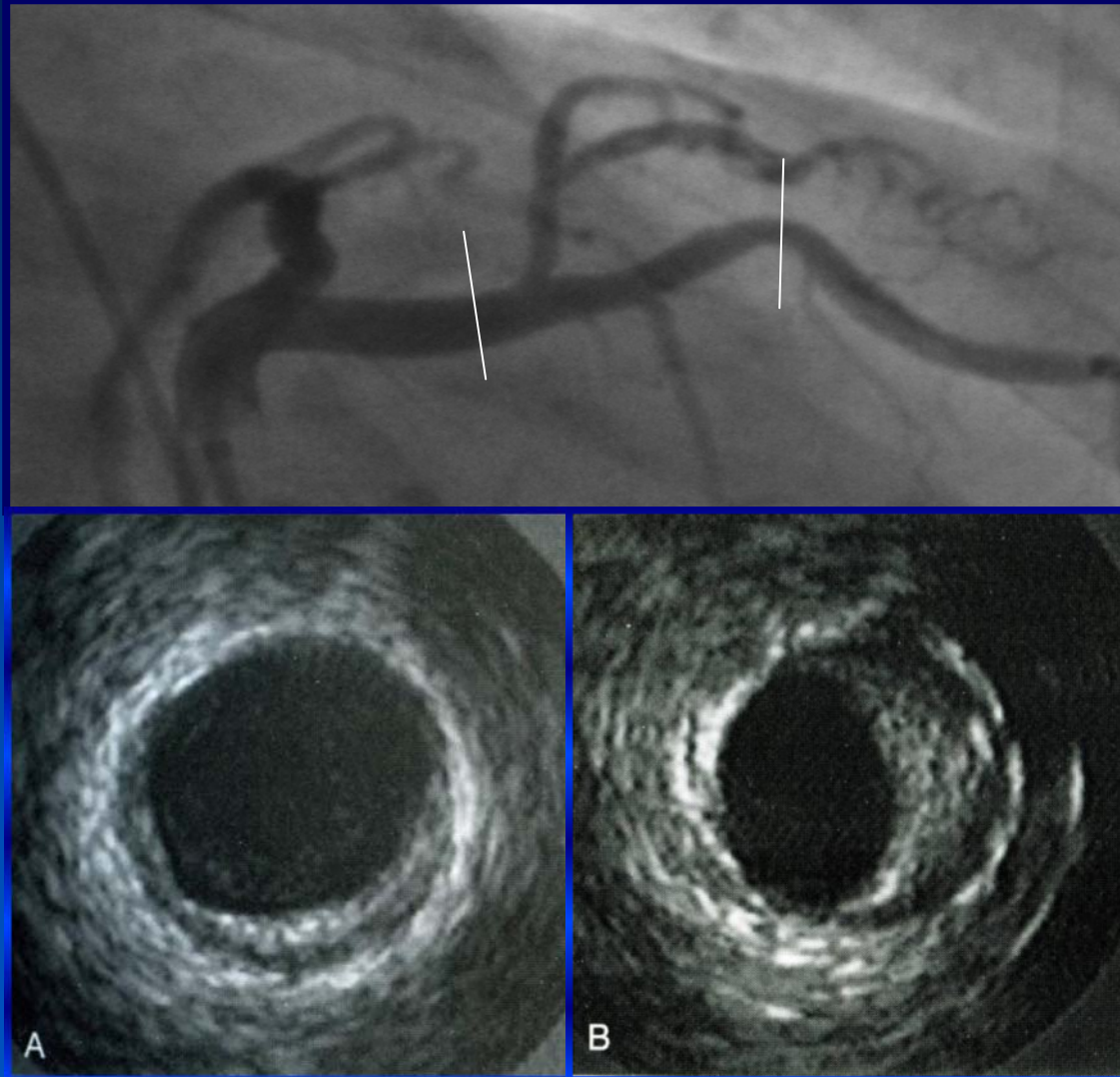
B



C



IVUS is a solution!



Contents

- **Basic Physics and Equipment**
- **Image Acquisition and IVUS Artifacts**
- **Histology**
- **Quantitative and Qualitative Assessment**
- **Reporting**



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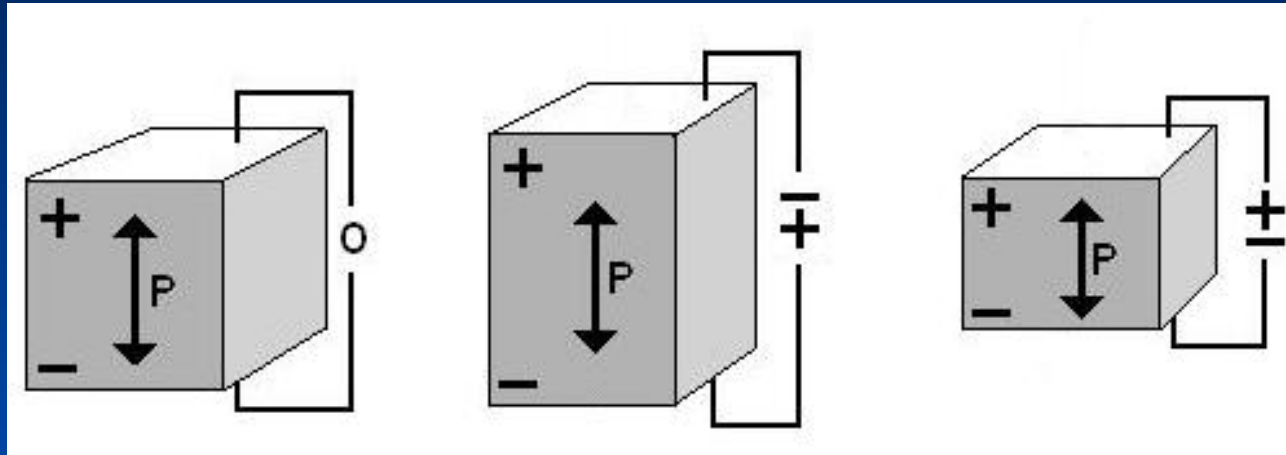
Basic Physics of Sound

- Sound is a physical phenomenon that transfers energy from one point to another.
- Sound can pass only through matter.
- Ultrasound can be focused into small, well-defined beams that can probe the human body and interact with the tissue structures to form images



Piezoelectricity

- Piezo- : from piezein (*Greek*), squeeze or press
- Conversion electricity to sound and vice versa

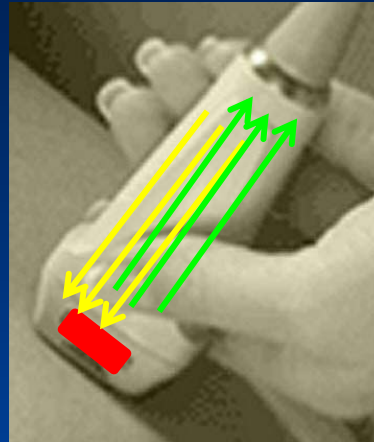


When a piezoelectric crystal is placed in an electric field, or when charges are applied by external means to its faces, the crystal exhibits strain, i.e. the dimensions of the crystal change.

Ultrasound imaging process

electric impulse

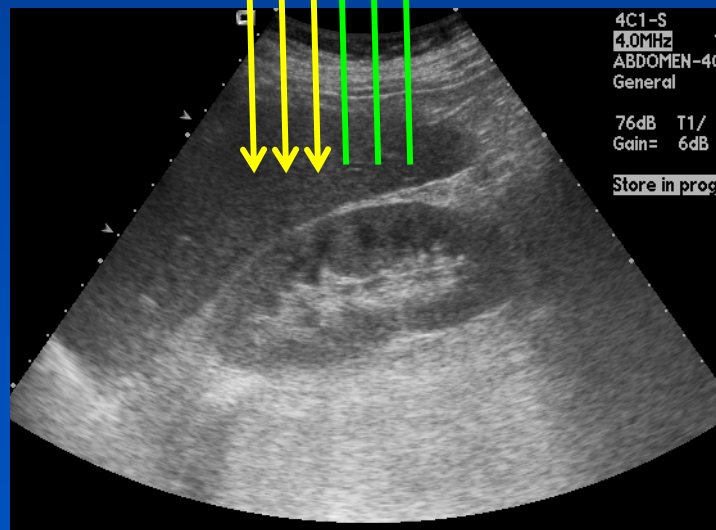
crystal



electric impulse

sound beam

returning beam

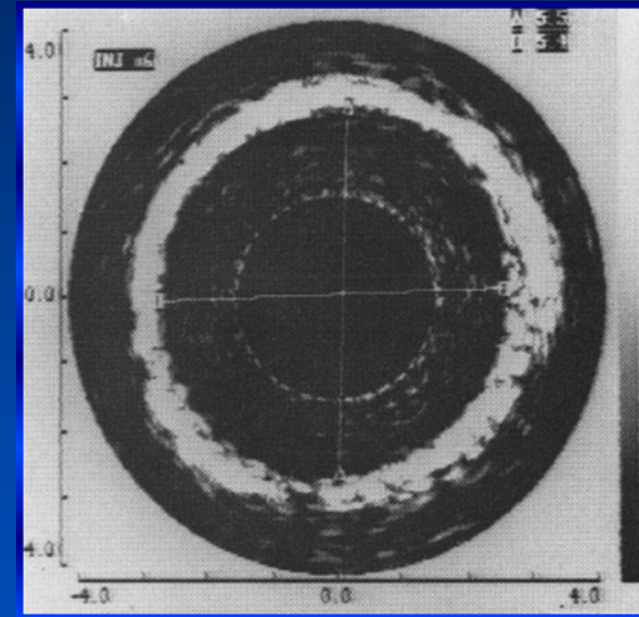
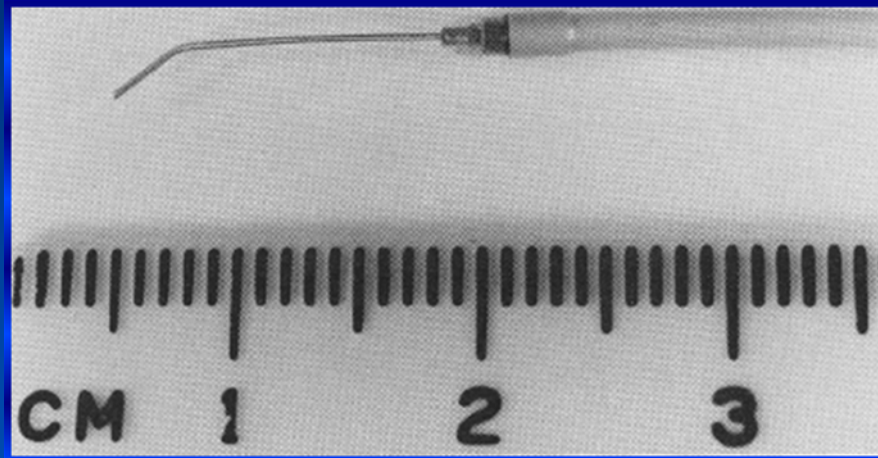


Comparison of IVUS with other ultrasound

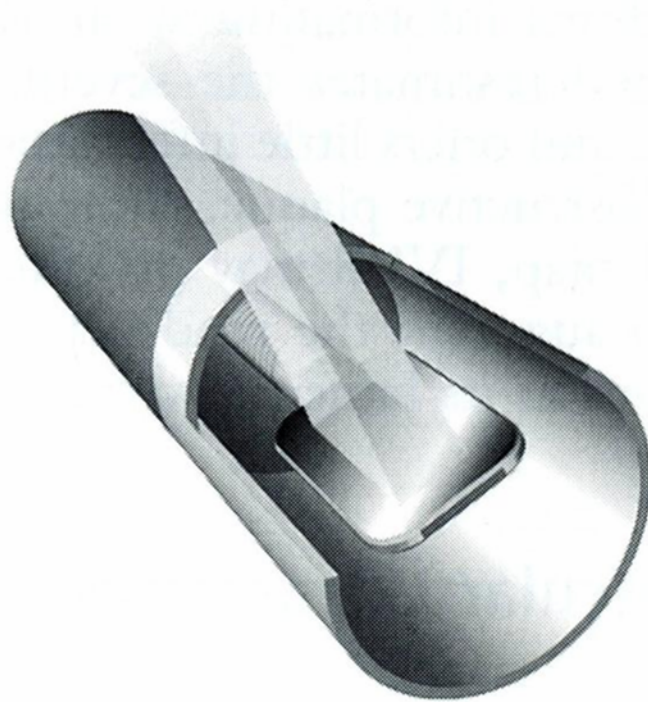
Technique	Transducer size (cm)	Depth (cm)	Intervening tissues
Trans-thoracic	> 2	~3 – 20	Skin, fat, muscle
Trans-esophageal	< 1.2	~2 – 20	Esophagus, atrium
Intravascular	< 0.26	~0.05 – 4	blood



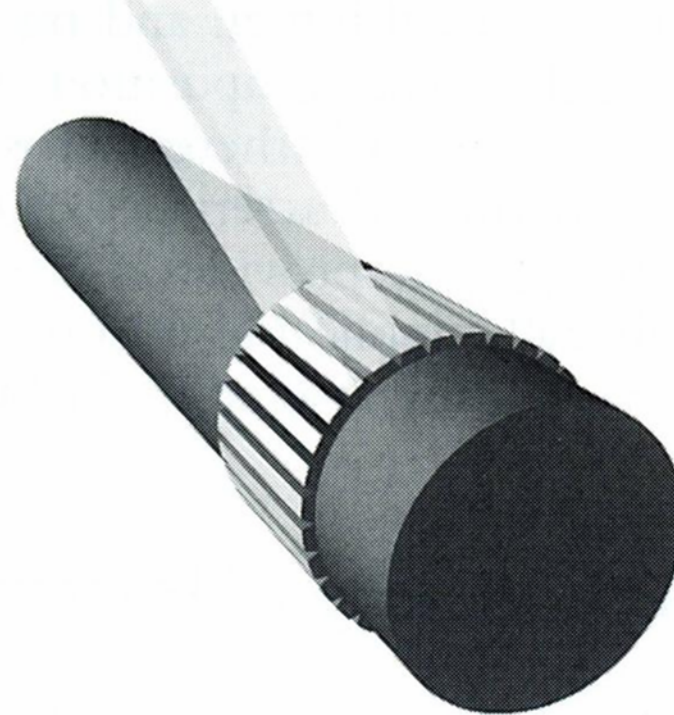
In early period



Equipment



Mechanical systems



Electronic systems

Image quality

- Spatial resolution
 - The ability to discriminate small objects within the ultrasound image
 - Axial : parallel to the beam
 - Lateral : perpendicular to both the beam and the catheter



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- Reporting



Image Acquisition

pullback method

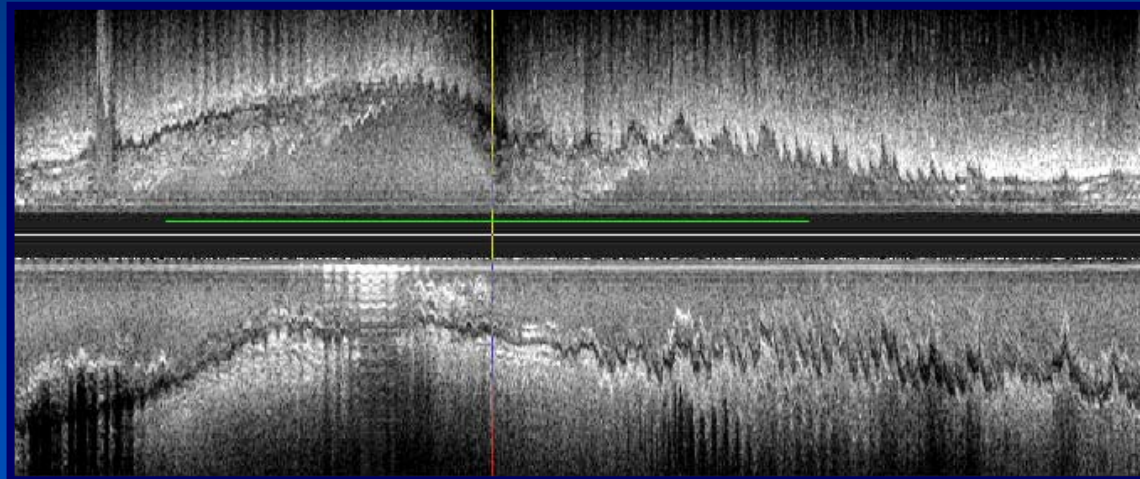
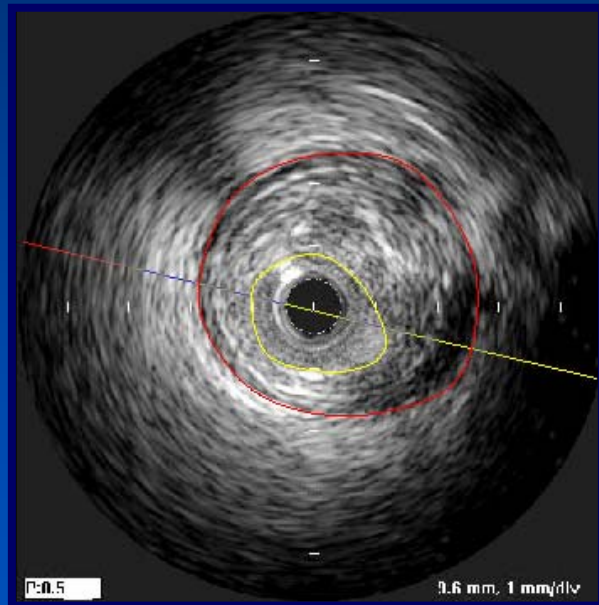
- Manual pullback
 - to concentrate on specific regions of interest
 - But, possible to skipping over and not to perform precise measurement
 - not reproducible
- Motorized pullback
 - precise, reproducible
 - to reconstruct image (L-mode, 3D)



Image Acquisition

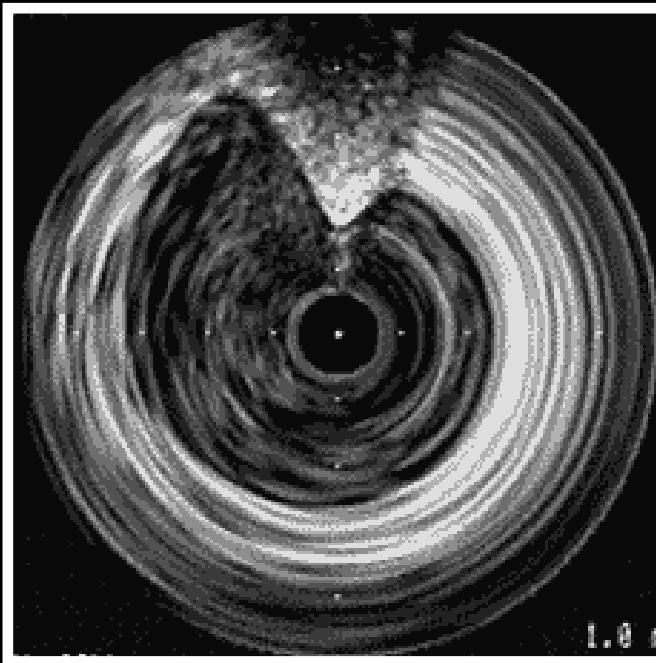
Longitudinal display (L-mode)

- For spatial orientation, assessment of length, and distribution of plaque

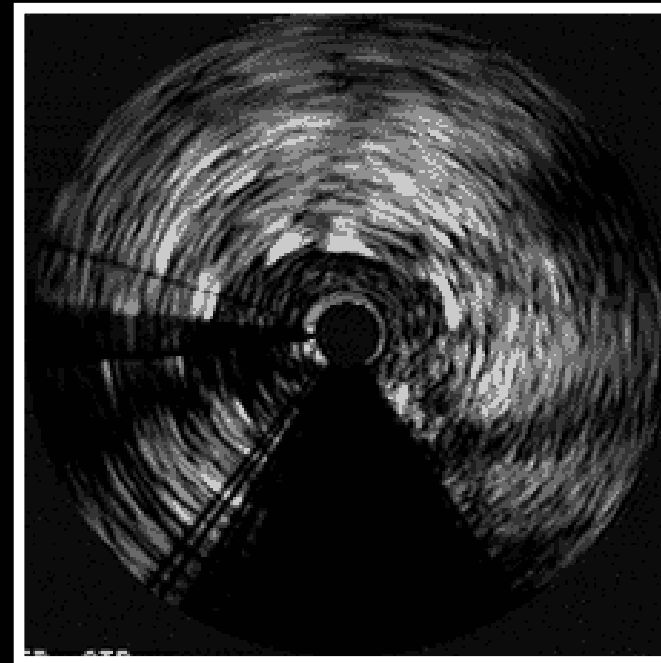


IVUS artifacts

non-uniform rotational distortion (NURD)



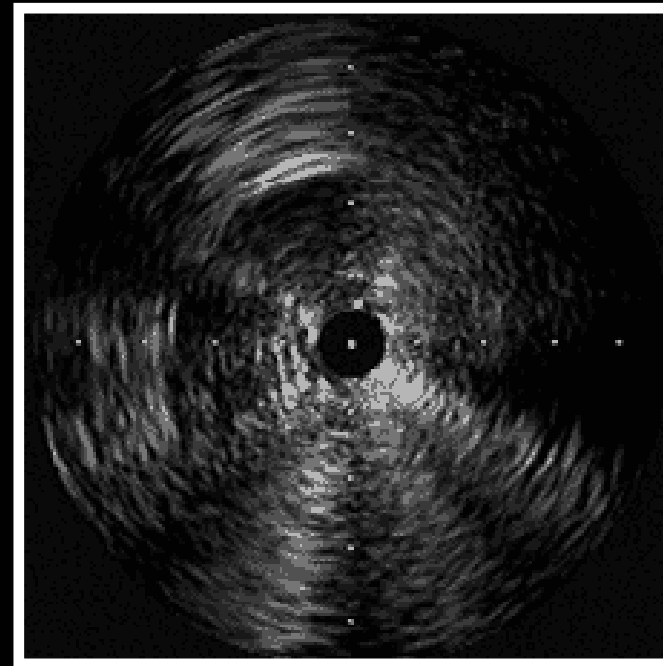
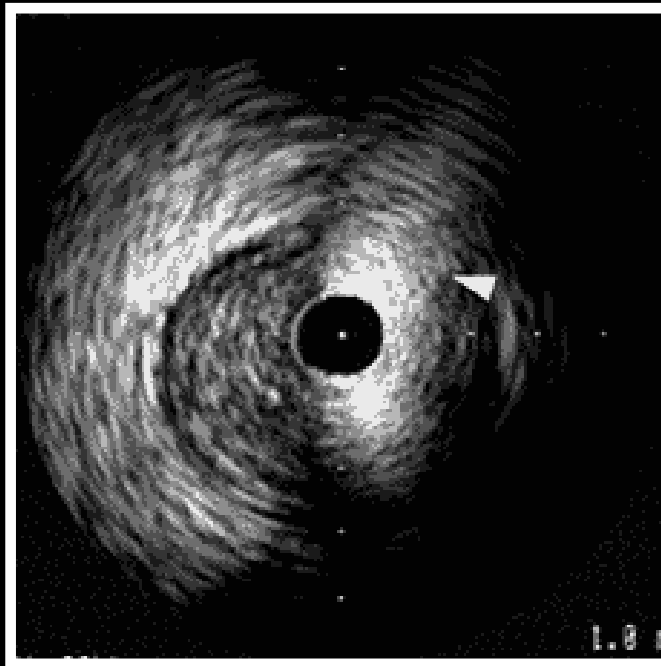
Full sector NURD



Isolated sector NURD

IVUS artifacts

air bubble

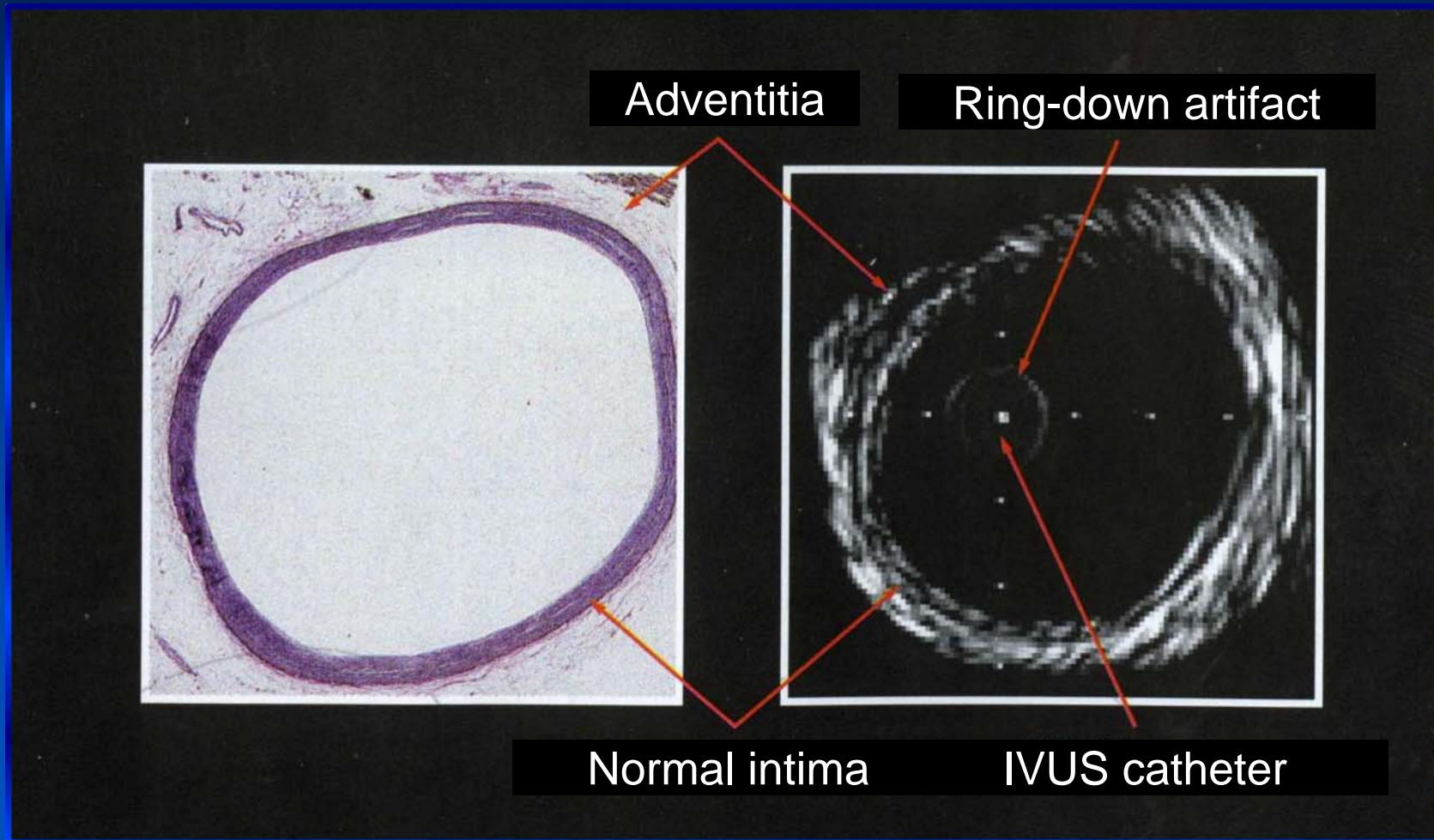


Contents

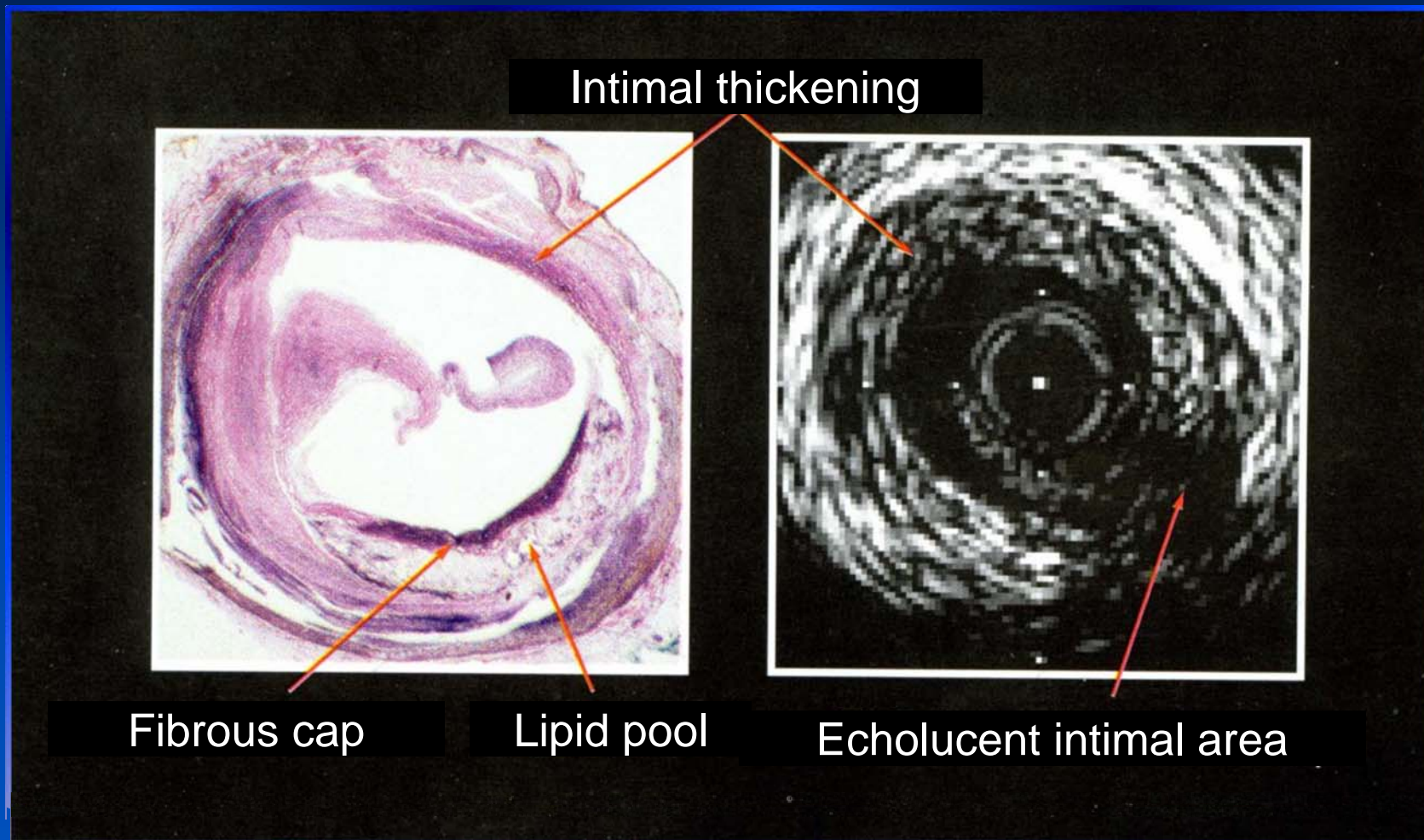
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Histology and IVUS



Histology and IVUS



Fibrous cap

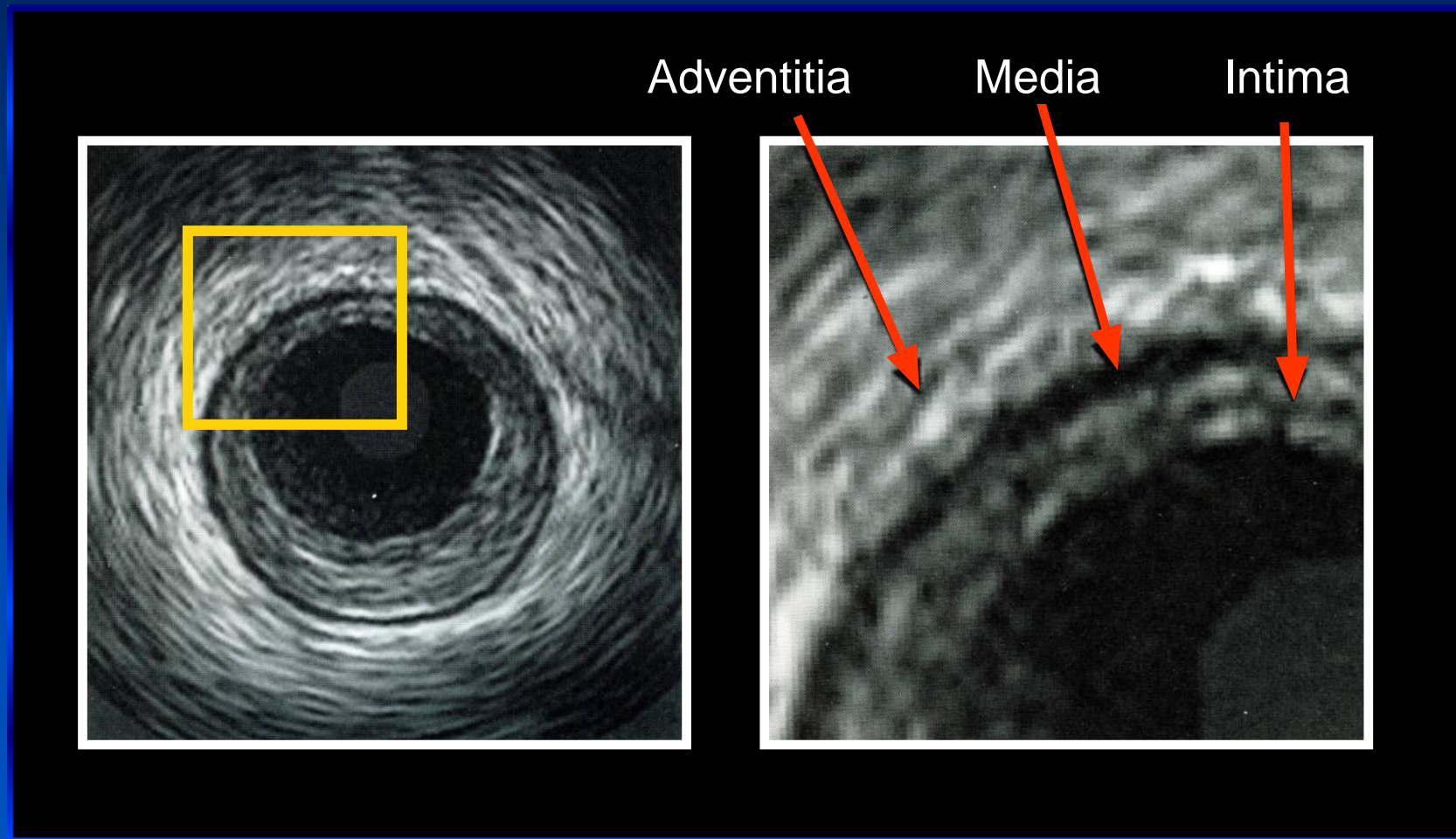
Lipid pool

Echolucent intimal area



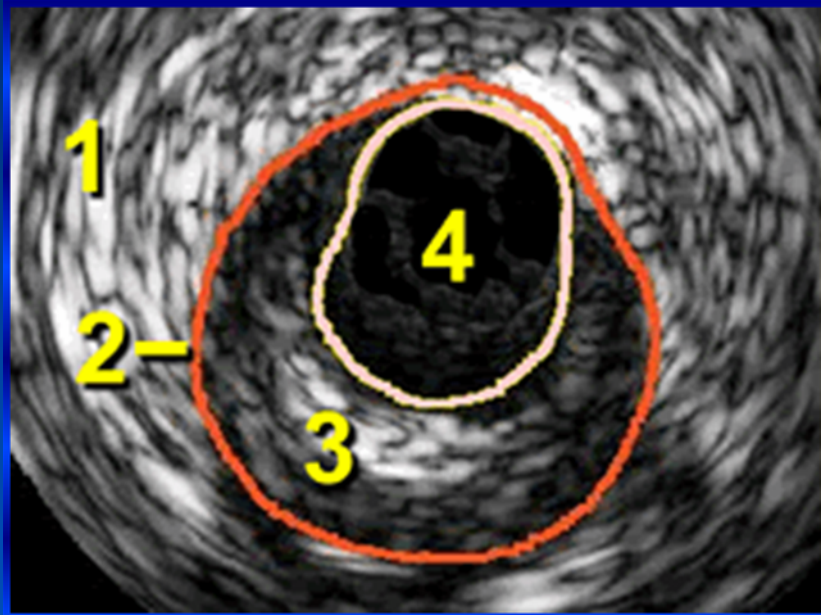
The Three-Layered Appearance

border identification



The Three-Layered Appearance

border identification



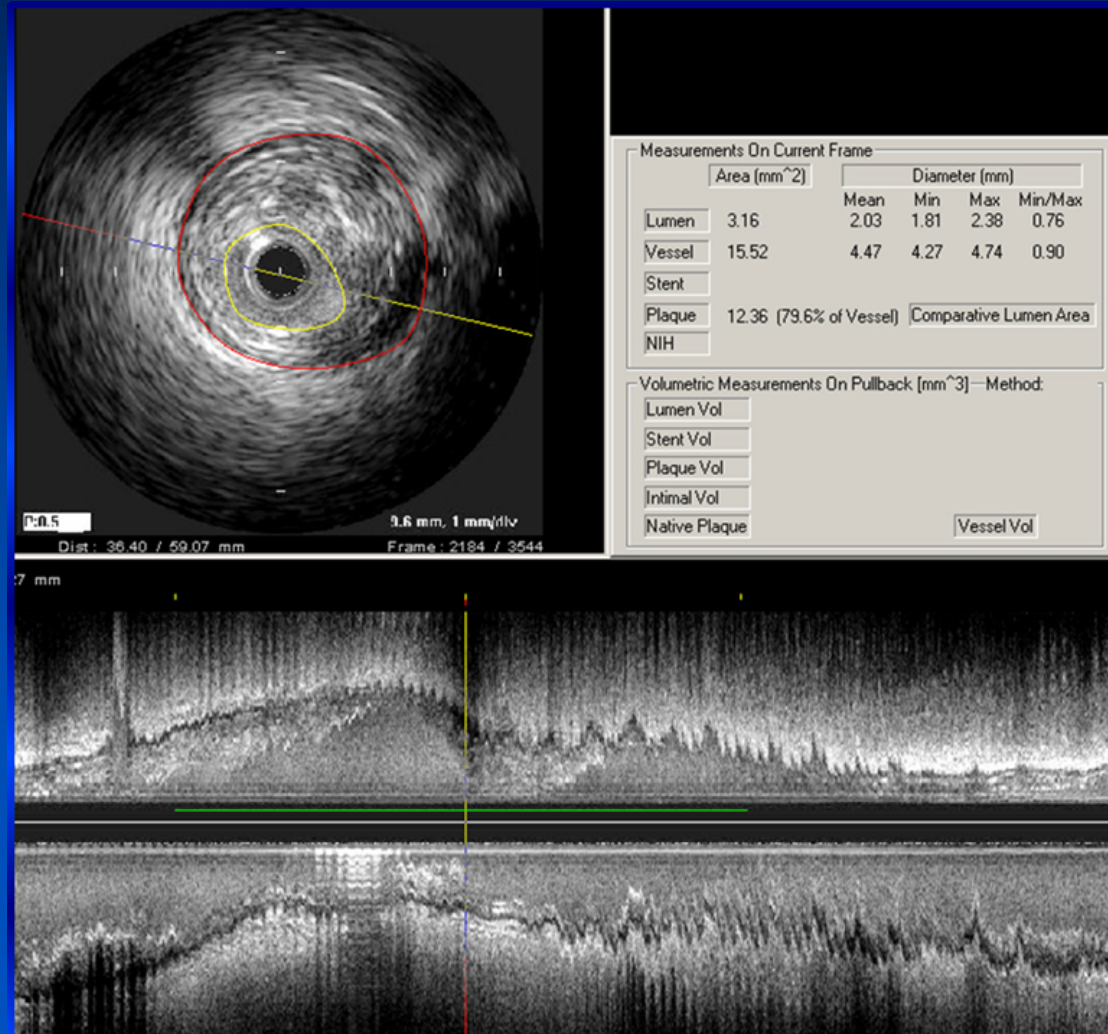
- 1. Adventitia** : the outer covering of the artery
- 2. Media** : the actual wall of the artery
- 3. Intima** : a layer of endothelial and other cells that make direct contact with the blood inside the artery
- 4. Lumen** : the actual open channel of the artery through which the blood flows.

Contents

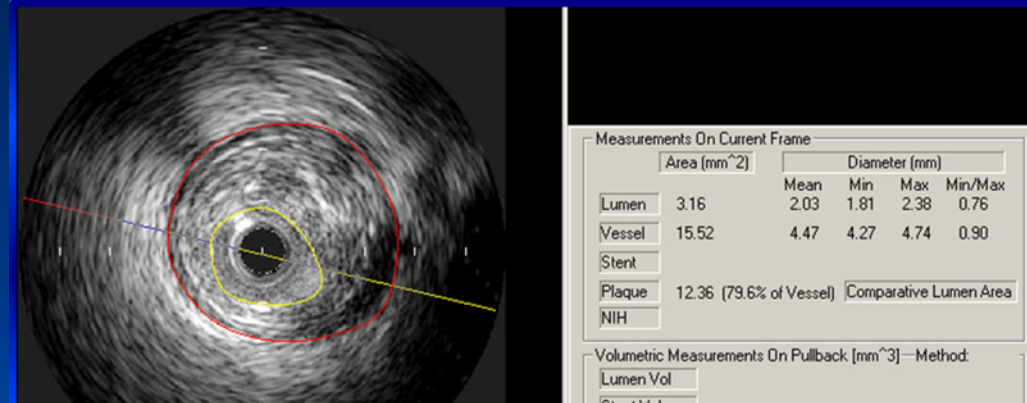
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Quantitative measurement lumen measurements



Quantitative measurement lumen measurements

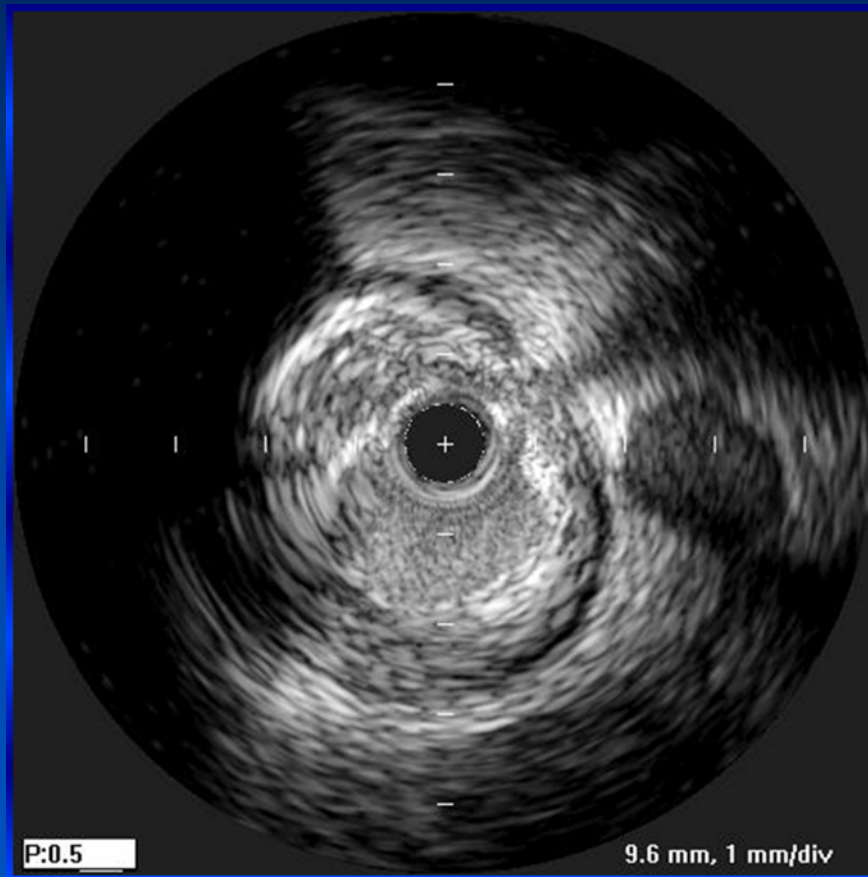


Measurements On Current Frame

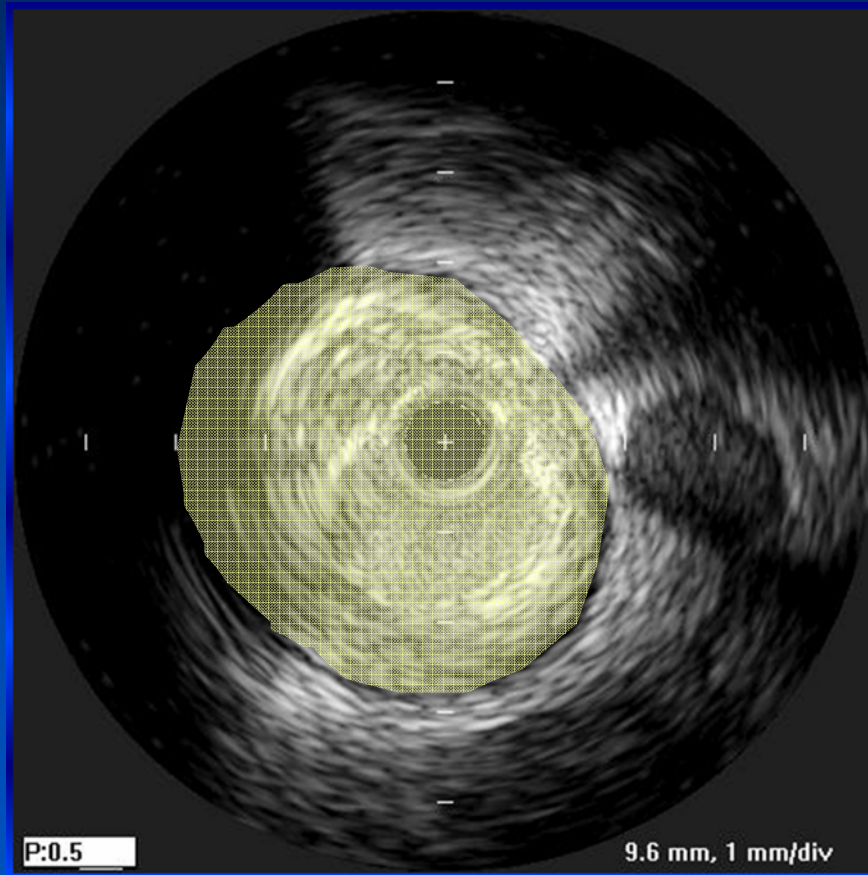
	Area (mm ²)	Diameter (mm)			
		Mean	Min	Max	Min/Max
Lumen	3.16	2.03	1.81	2.38	0.76
Vessel	15.52	4.47	4.27	4.74	0.90
Stent					
Plaque	12.36 (79.6% of Vessel)	Comparative Lumen Area			
NIH					



Quantitative measurement atheroma measurements



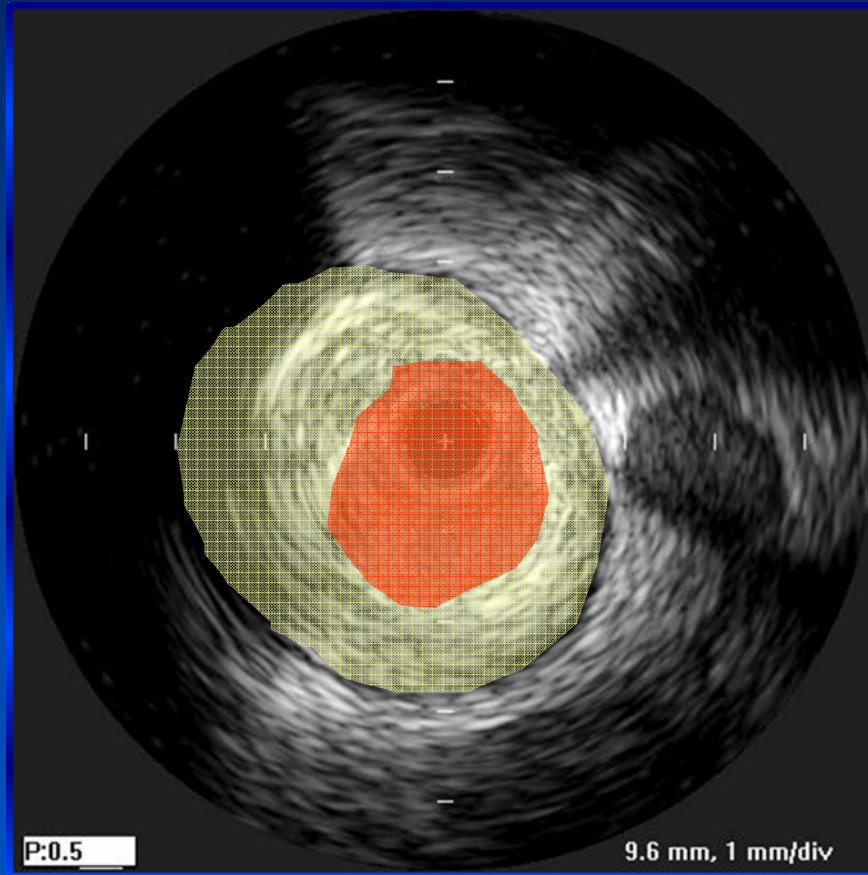
Quantitative measurement atheroma measurements



Atheroma

= **EEM**

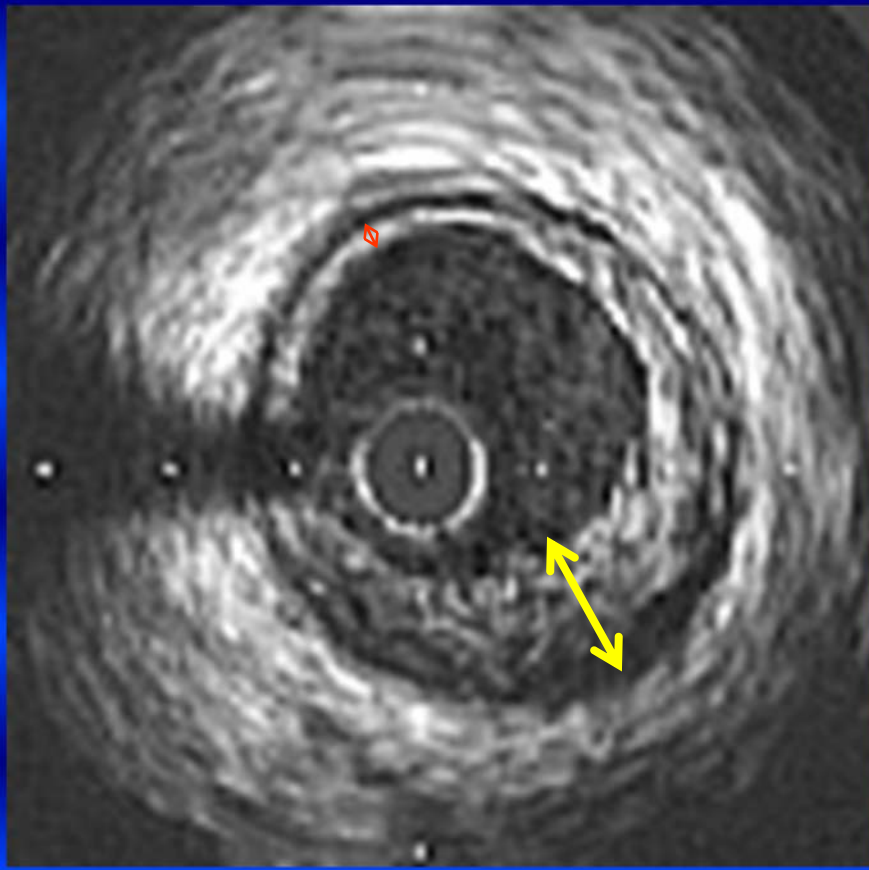
Quantitative measurement atheroma measurements



Atheroma

= **EEM** - **Lumen**

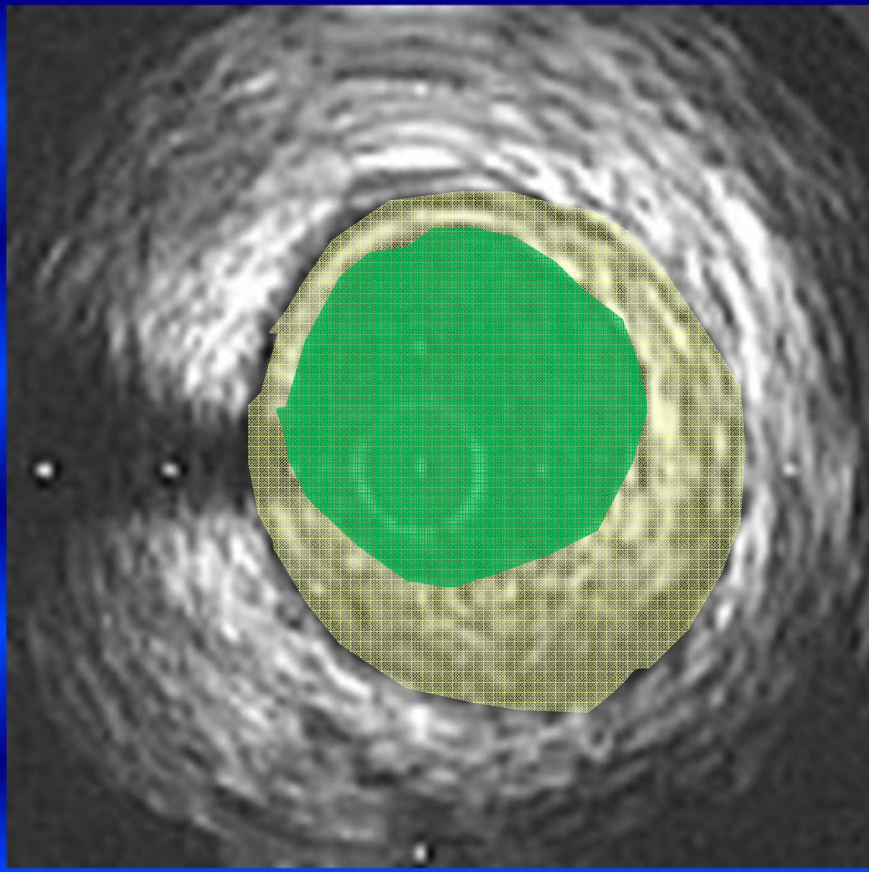
Quantitative measurement atheroma measurements



Atheroma eccentricity

$$= \frac{A - B}{A}$$

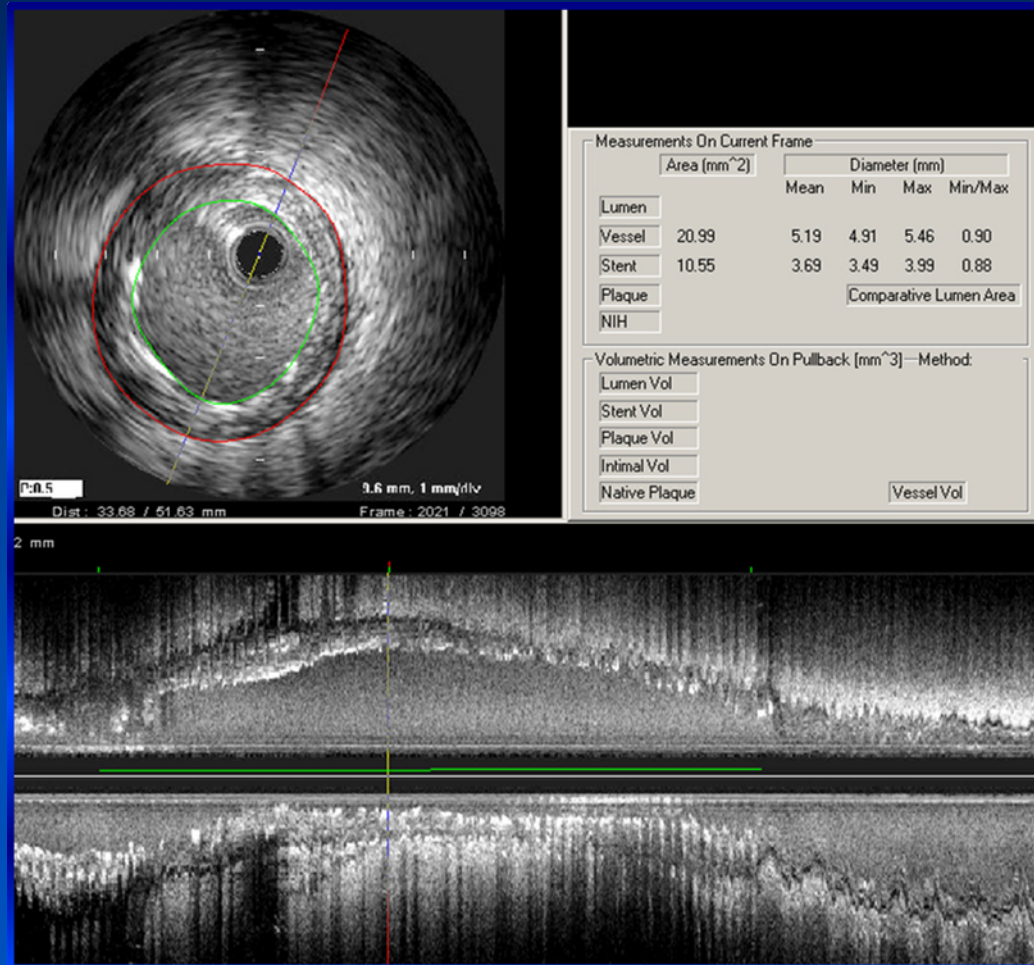
Quantitative measurement atheroma measurements



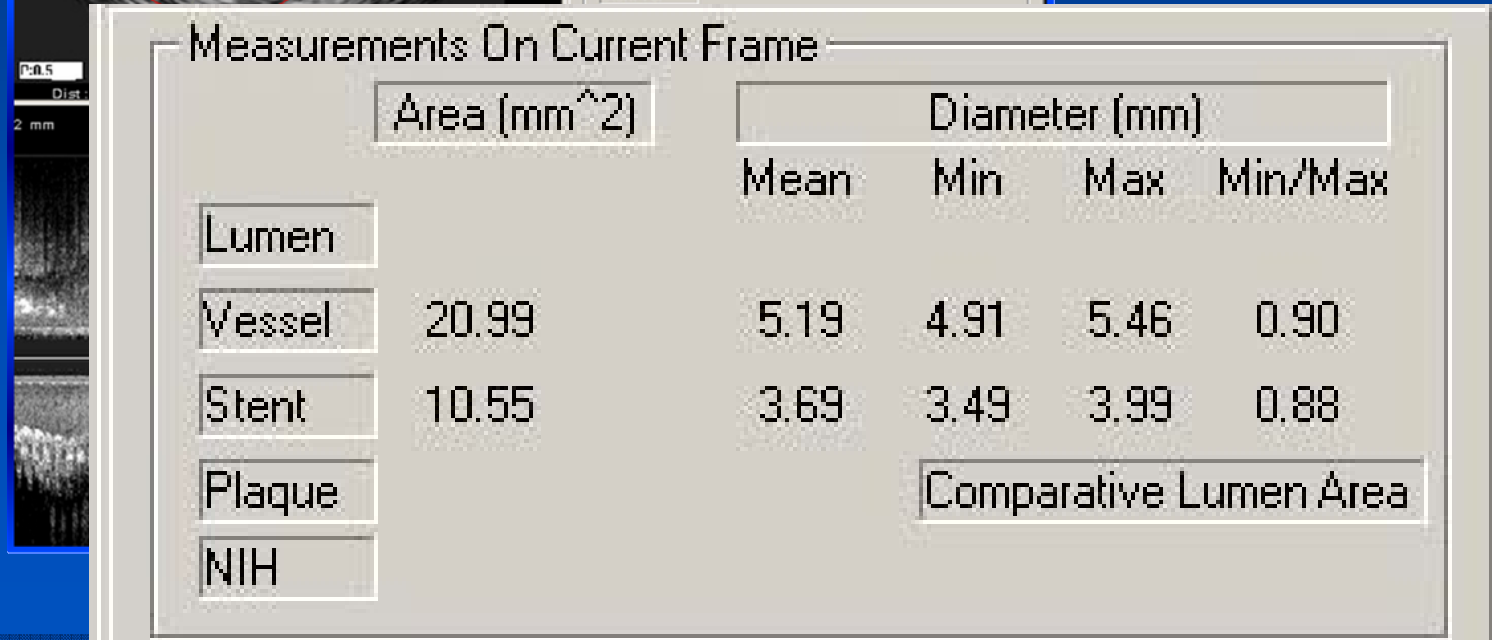
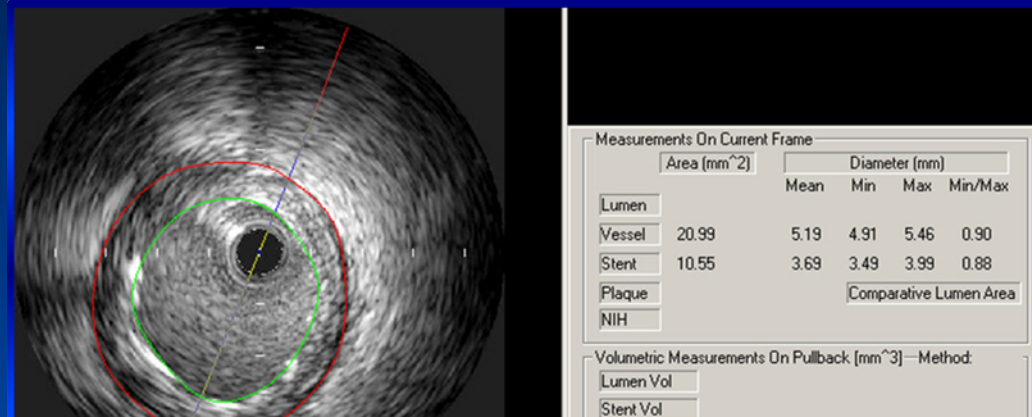
Atheroma burden

$$= C - D / C$$

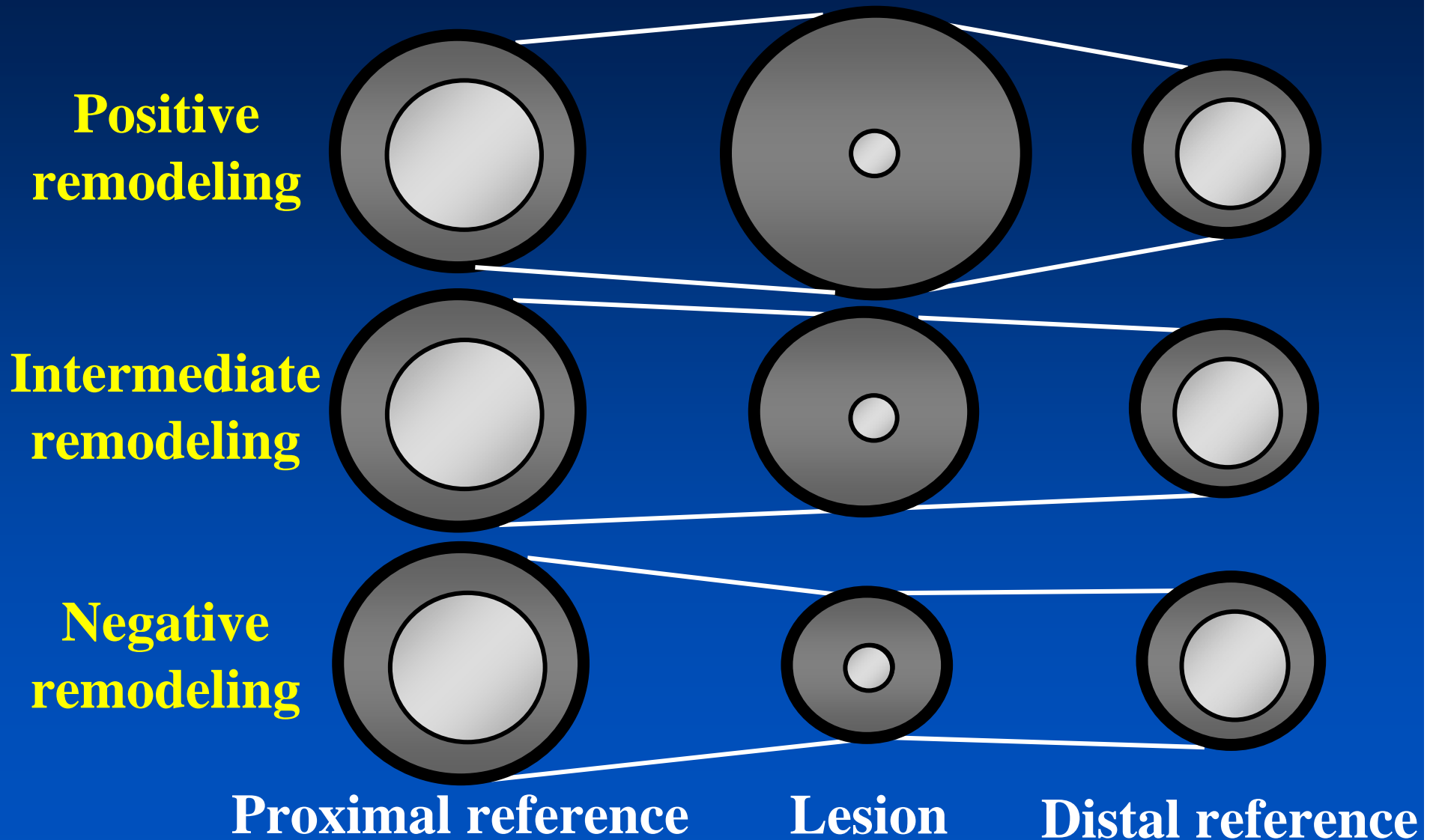
Quantitative measurement stent measurements



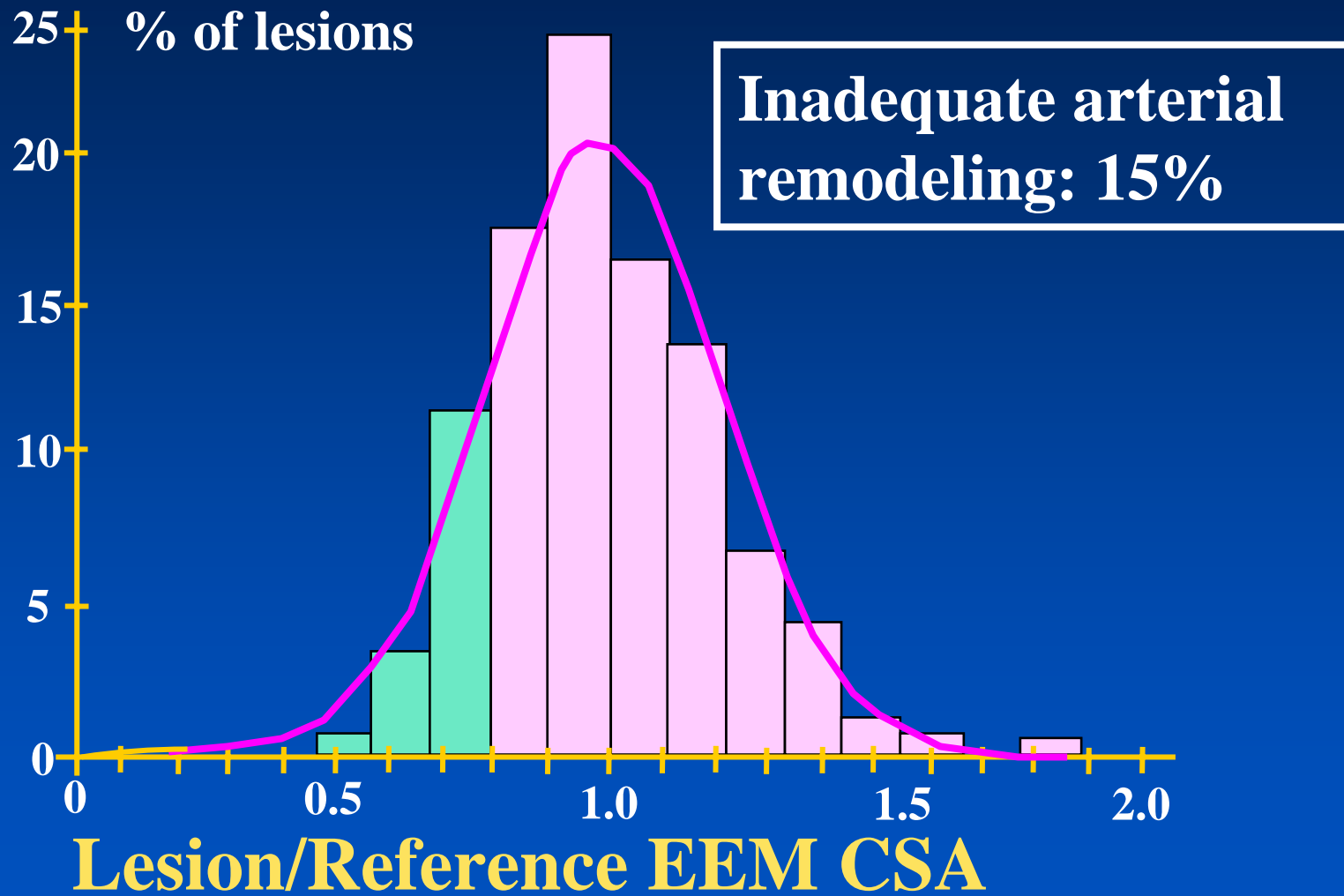
Quantitative measurement stent measurements



Dicotomous Classification of Remodeling



Contribution of inadequate arterial remodeling to the development of focal coronary artery stenoses: an IVUS study

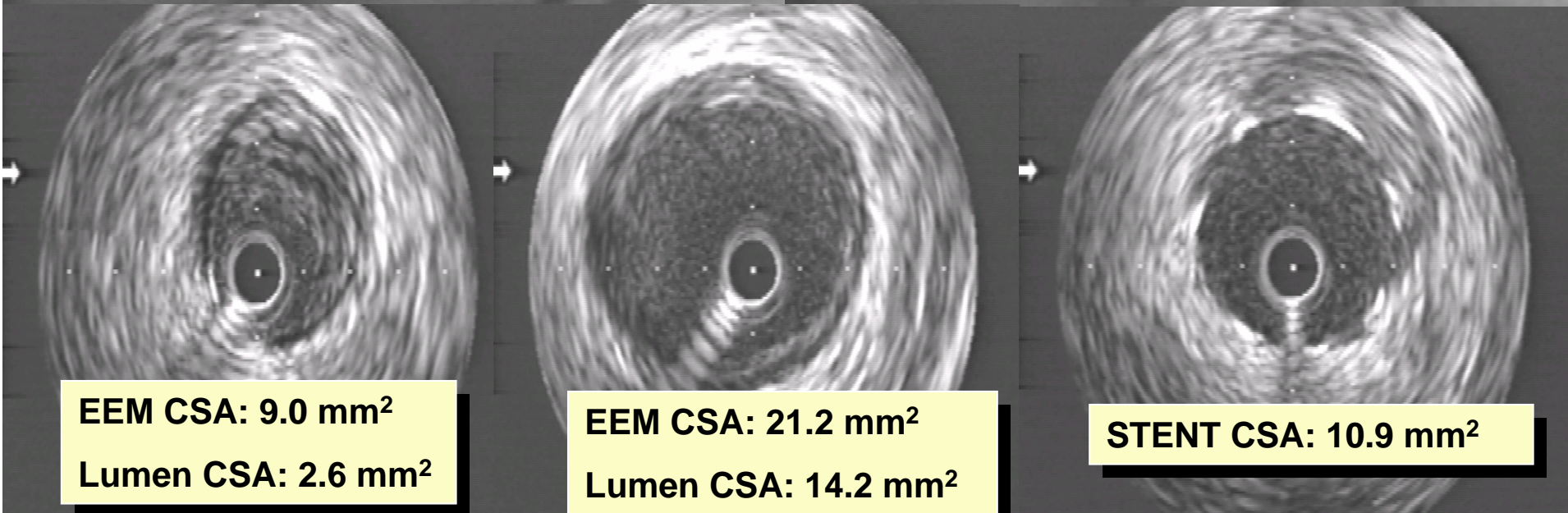
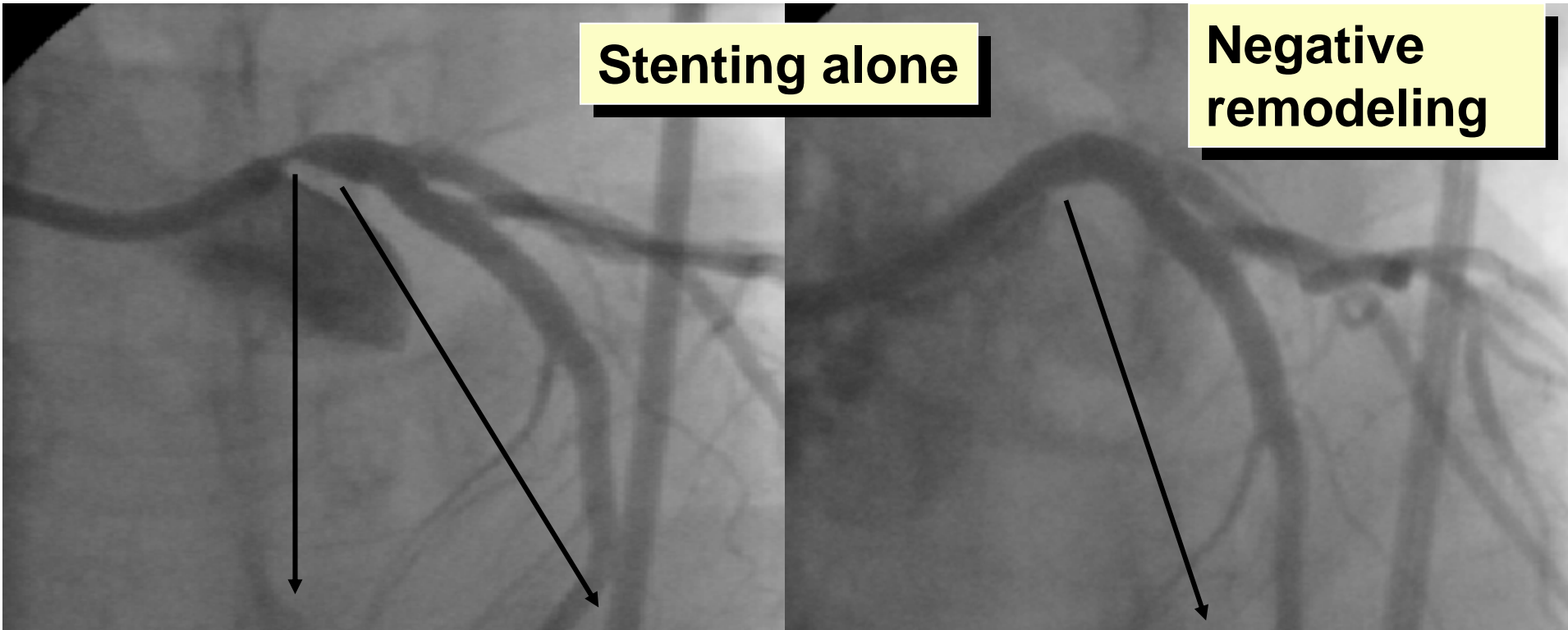


Mintz GS, et al. *Circulation* 1997;95: 1791-98



Stenting alone

Negative remodeling



EEM CSA: 9.0 mm²
Lumen CSA: 2.6 mm²

EEM CSA: 21.2 mm²
Lumen CSA: 14.2 mm²

STENT CSA: 10.9 mm²

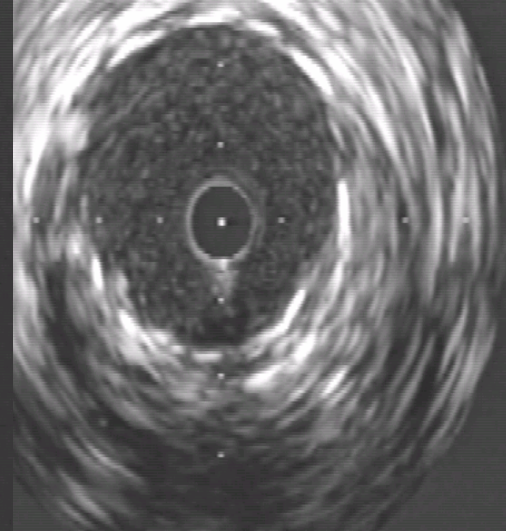
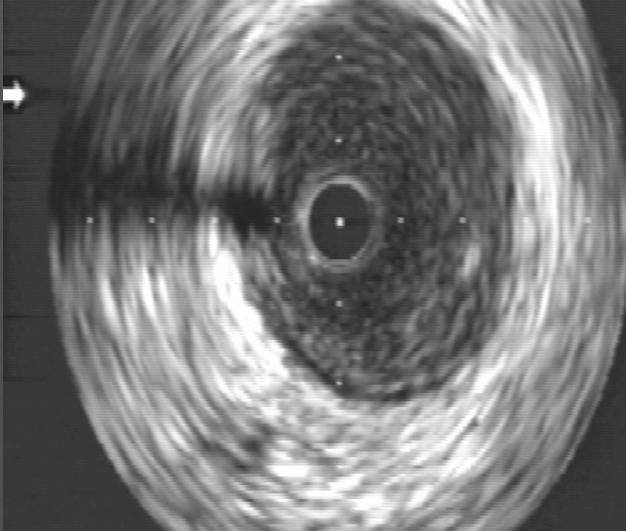
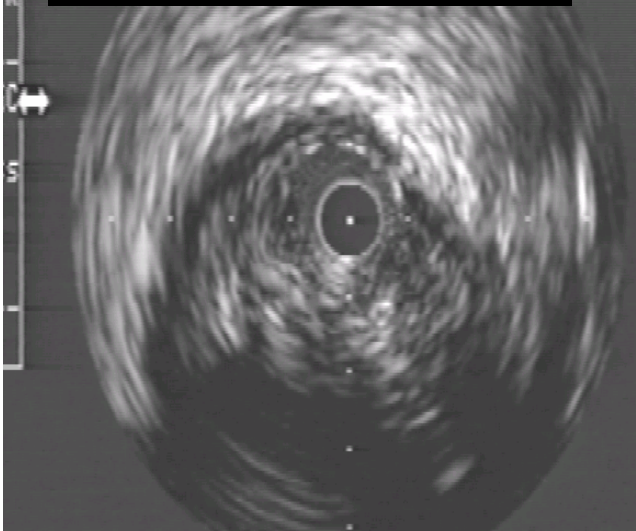
**Stenting
After DCA**

**Positive
remodeling**

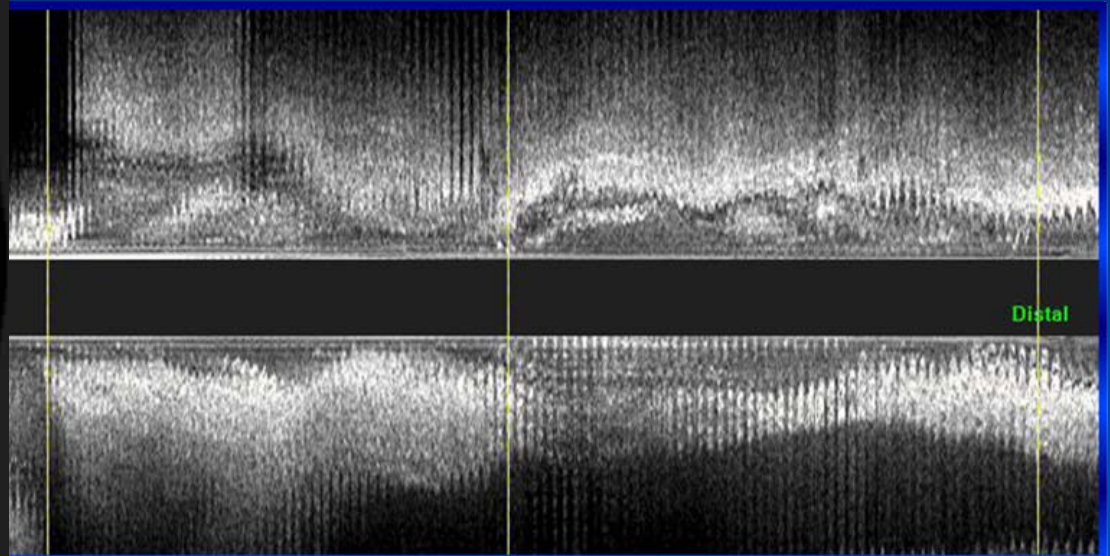
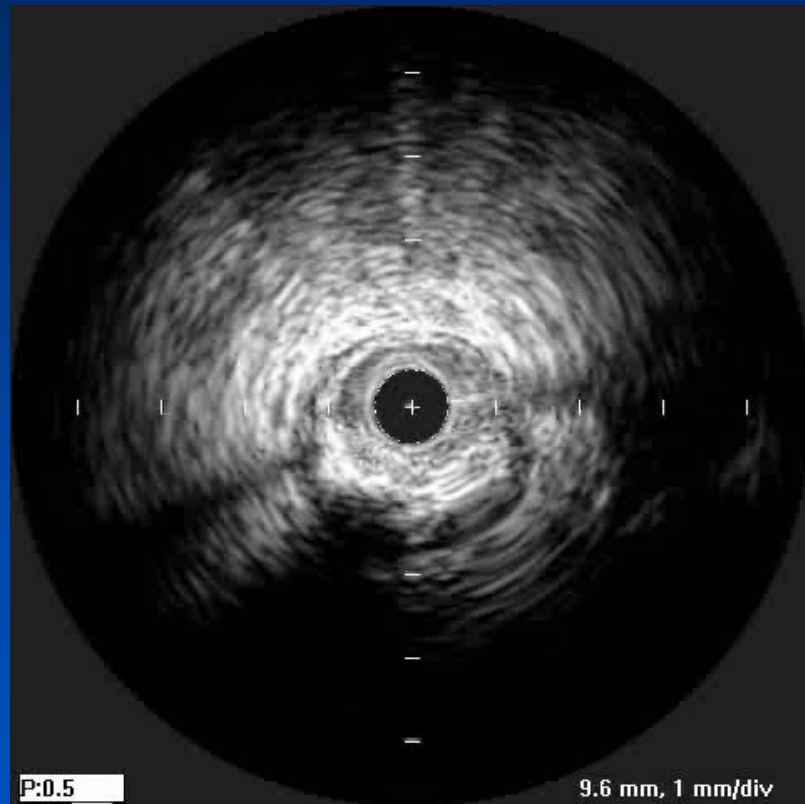
**EEM CSA: 23.9 mm²
Lumen CSA: 2.3 mm²**

**EEM CSA: 18.6 mm²
Lumen CSA: 10.3 mm²**

STENT CSA 15.4 mm²

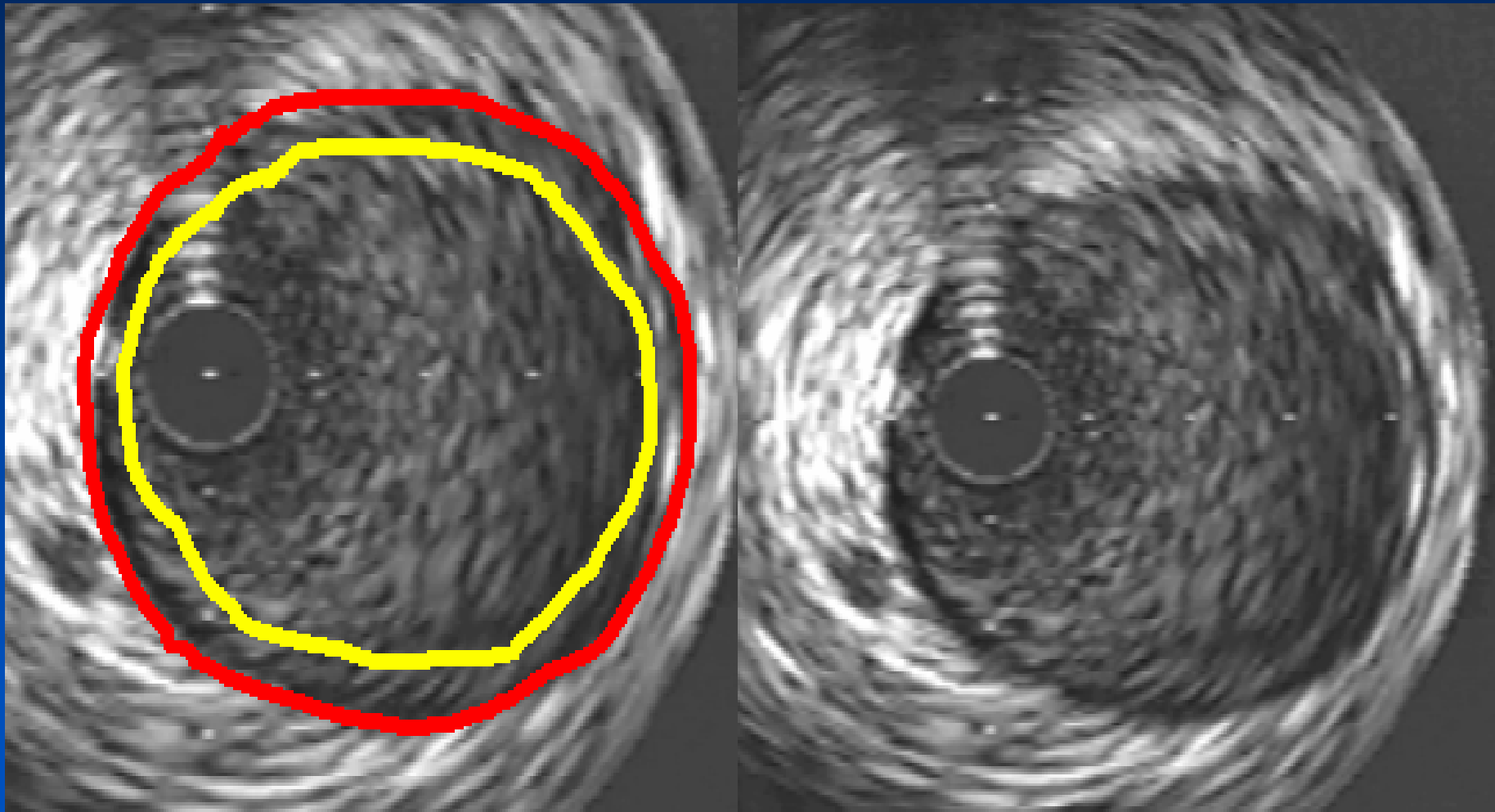


Quantitative measurement negative remodeling



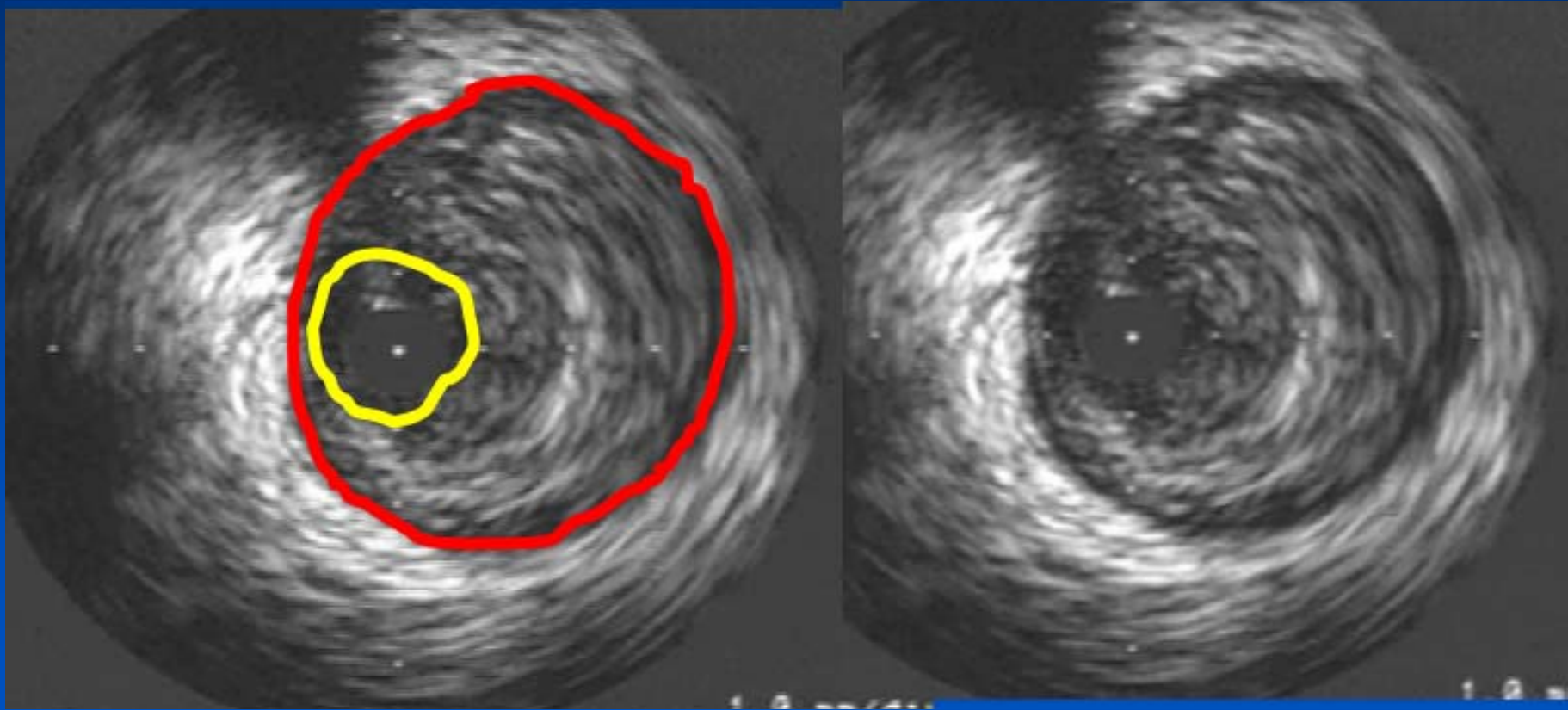
Atheroma Morphology

Normal



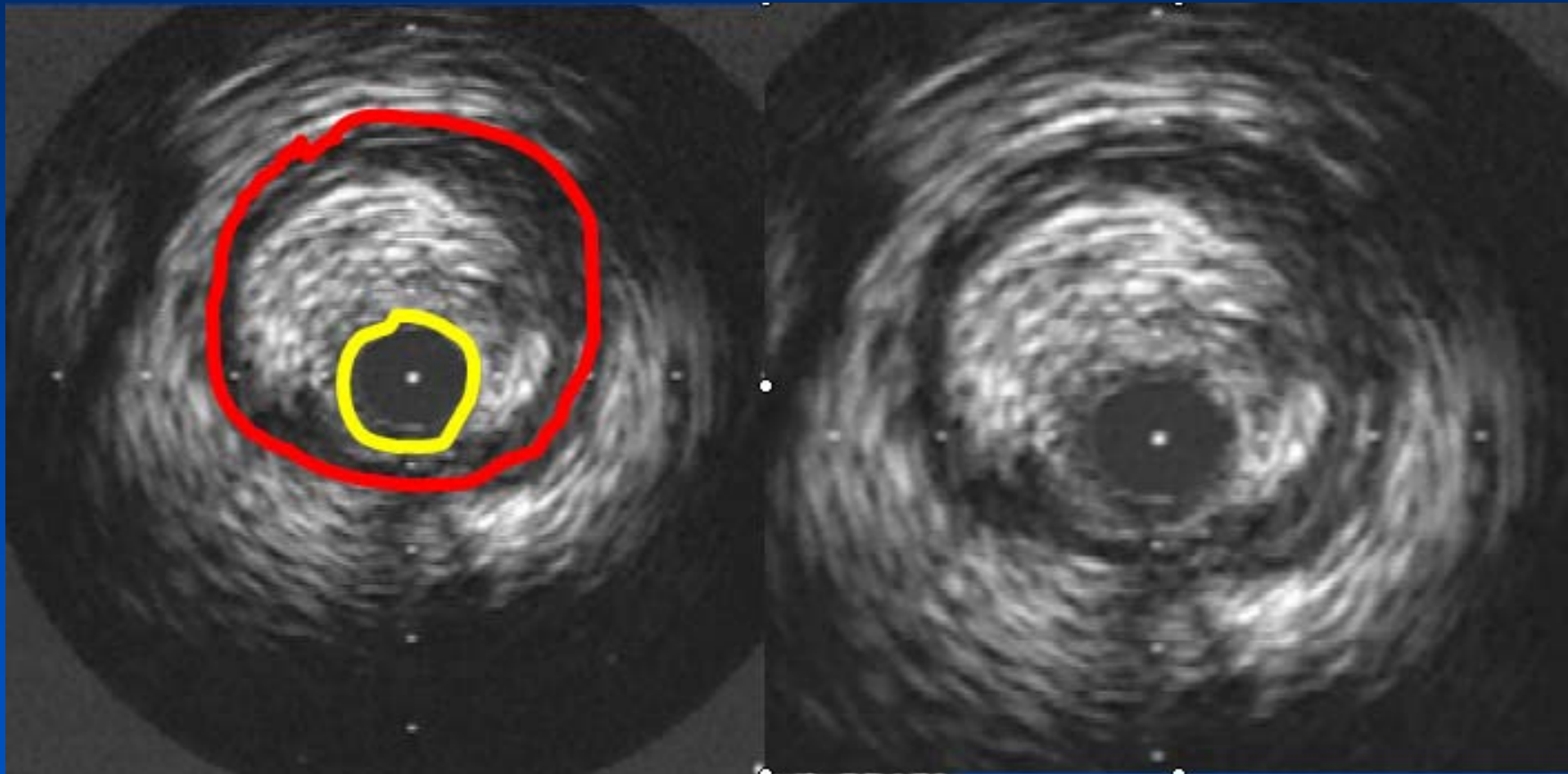
Atheroma Morphology

Soft plaque



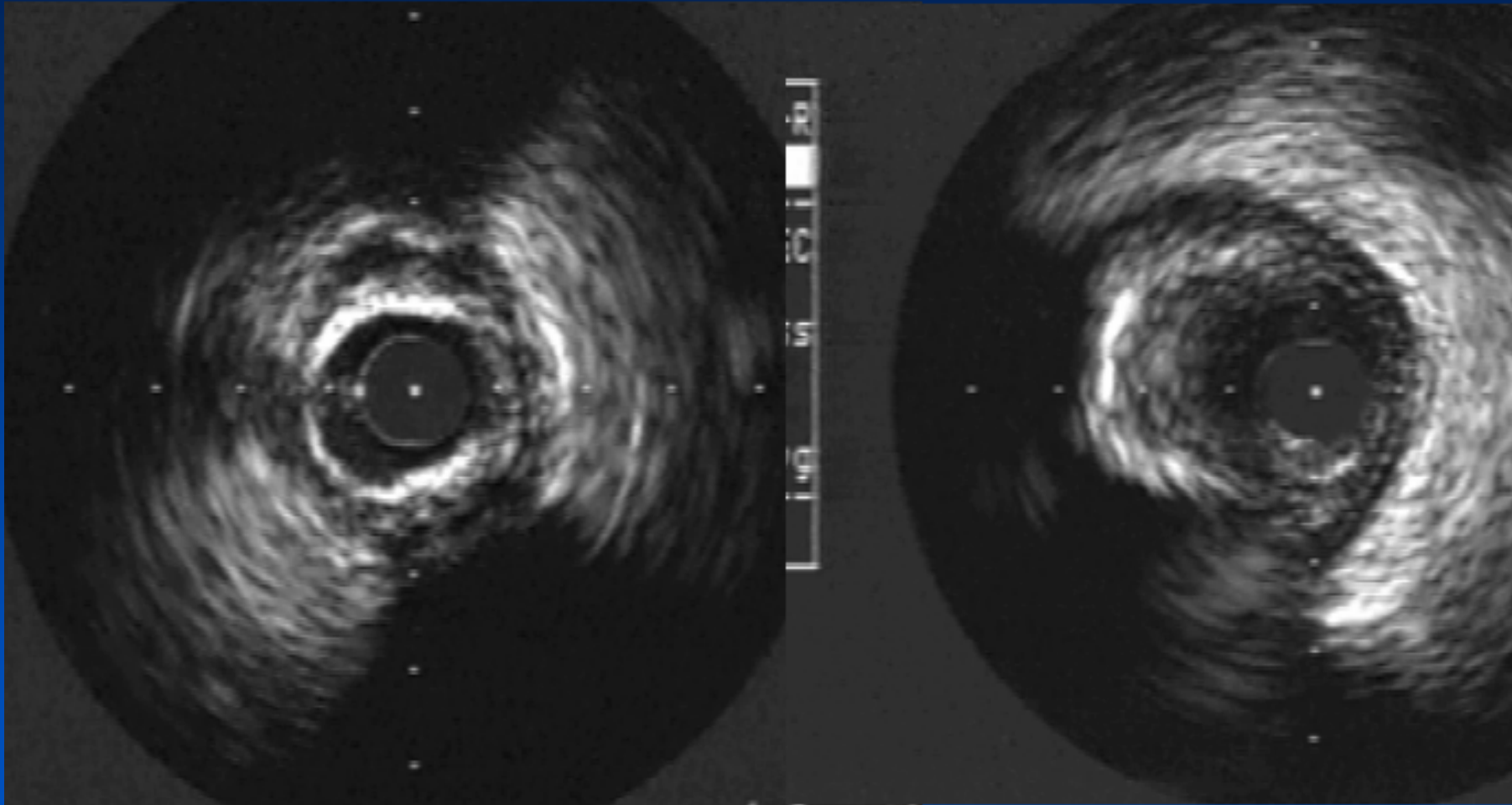
Atheroma Morphology

fibrotic plaque



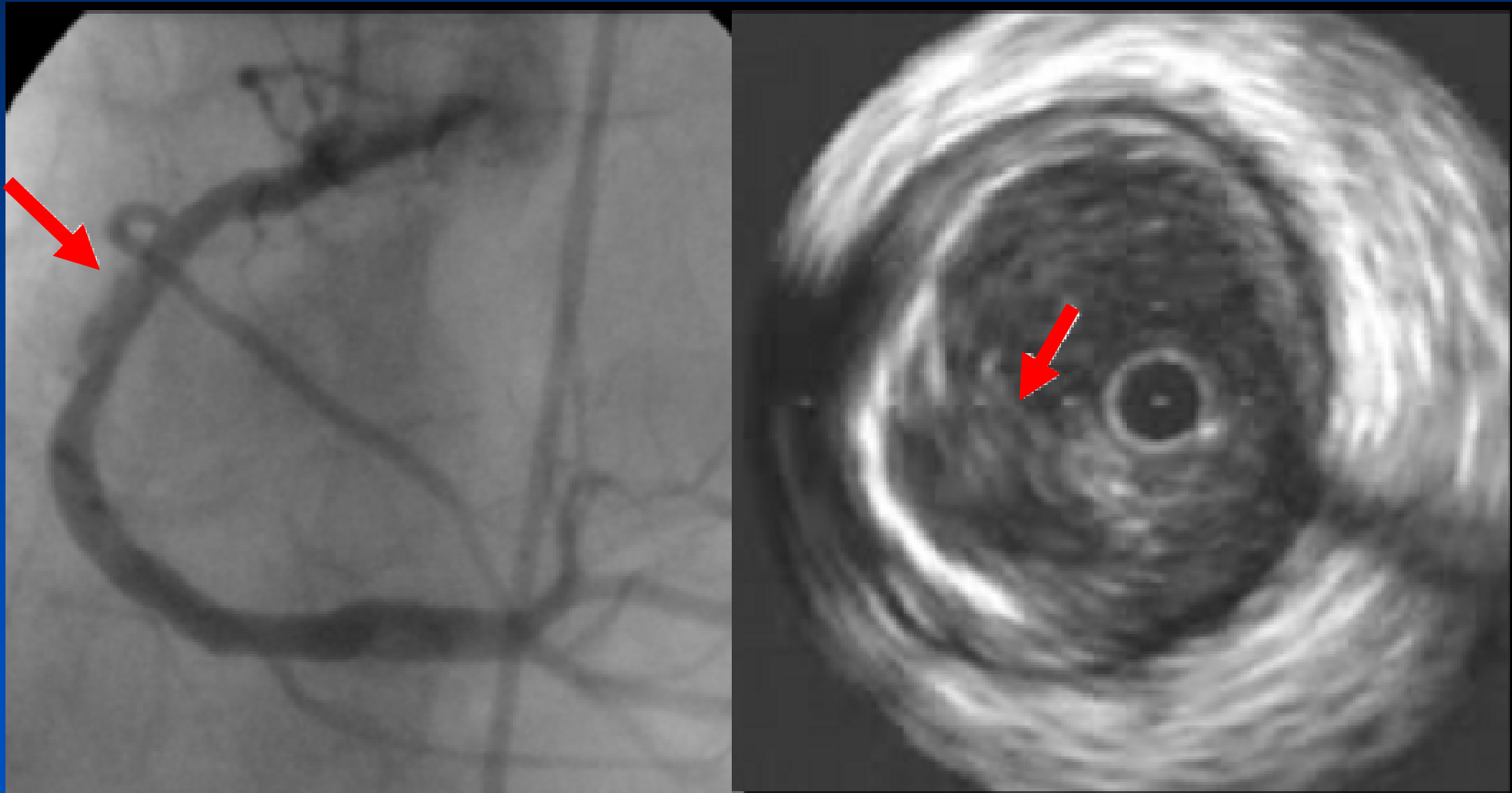
Atheroma Morphology

Calcium



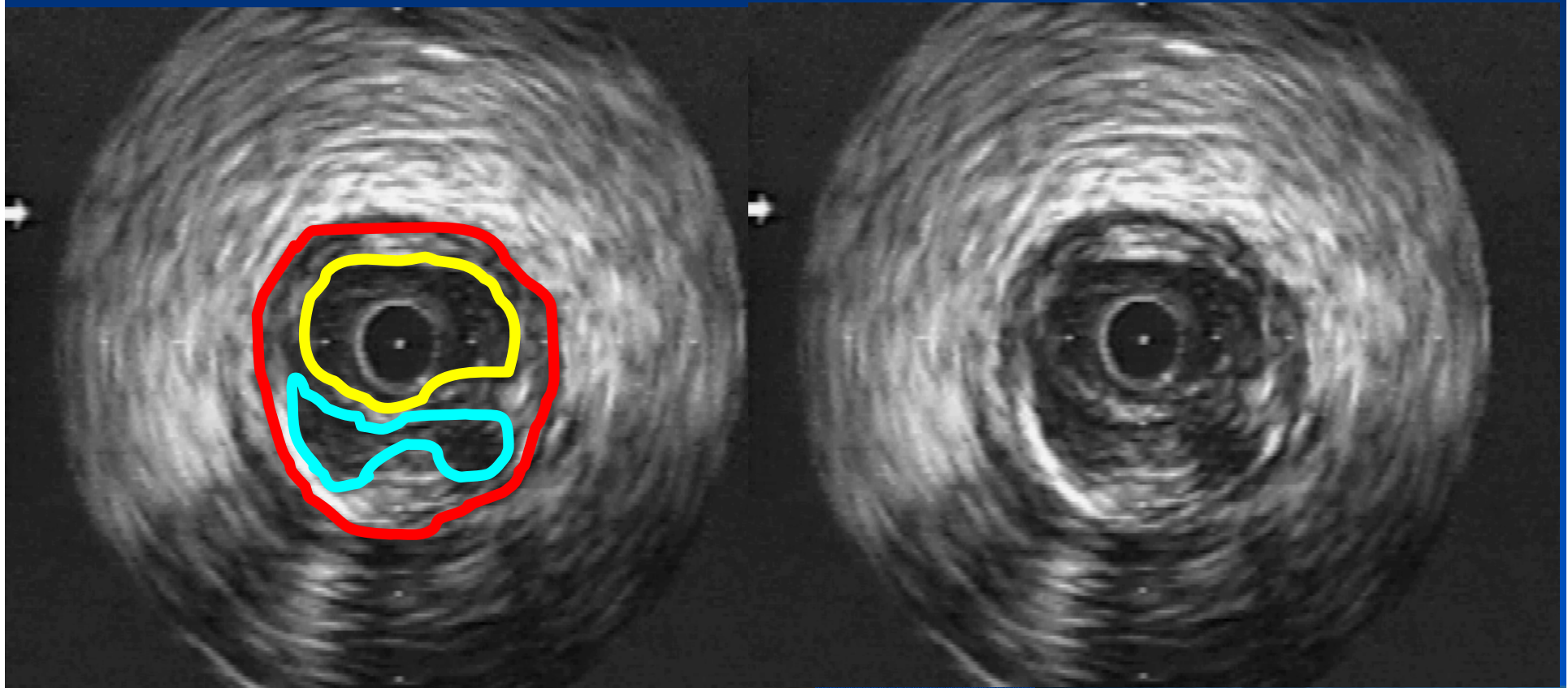
Atheroma Morphology

rupture



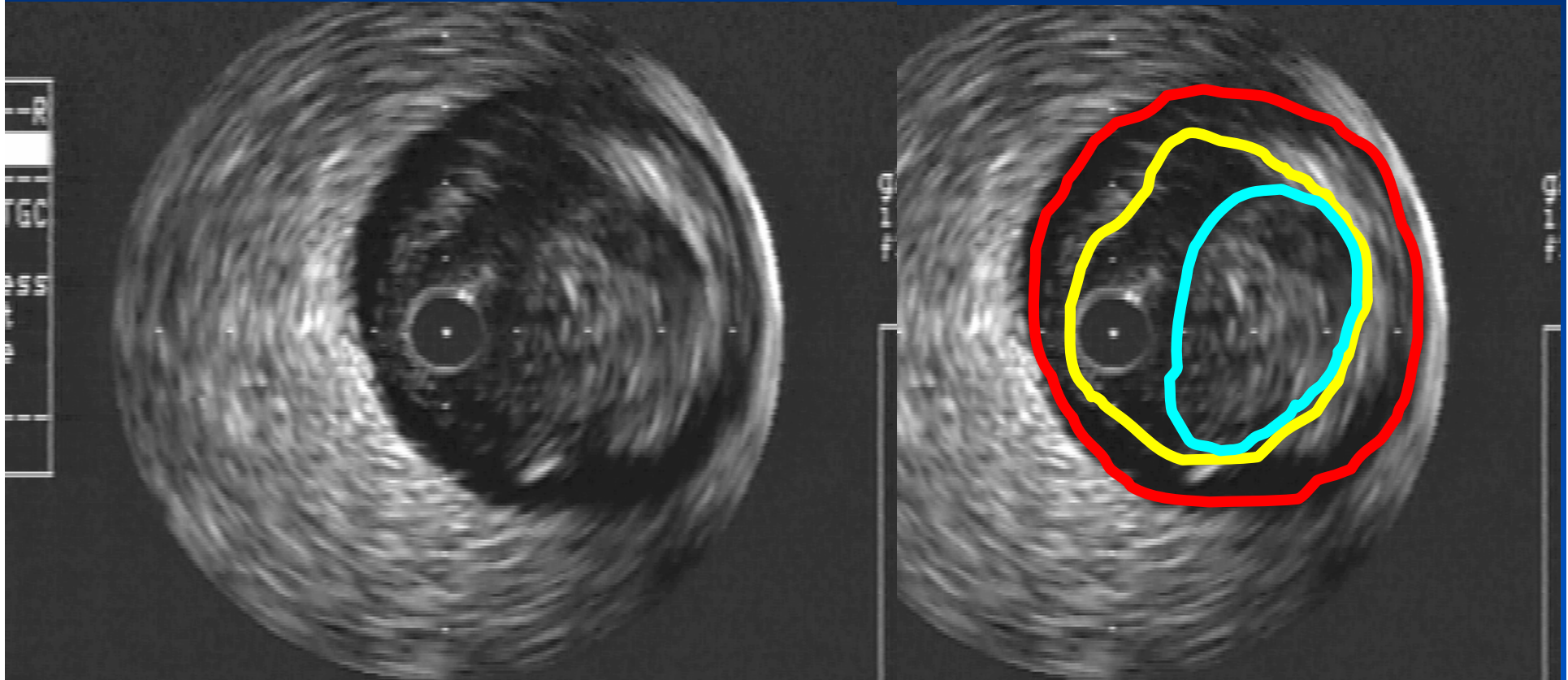
Atheroma Morphology

lipid core



Atheroma Morphology

thrombus



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Reporting of IVUS results

- ✓ Appropriate patient demographic information and date
- ✓ Indication and brief description of procedure
- ✓ Basic findings : MLD, minimum stent area, or plaque burden...
- ✓ Plaque features : dissection, calcium, or thrombus...
- ✓ Changes of therapy by IVUS
- ✓ IVUS-related complications and any consequent therapy.

ACC Clinical Expert Consensus. *J Am Coll Cardiol.* 2001



In my opinion

When you meet the complex cases, IVUS will help you at any time and answer you clearly about difficult questions



Image quality

- Contrast resolution
 - the distribution of the gray scale of the reflected signal and is often referred to as dynamic range

