

Erasmus MC
Universitair Medisch Centrum Rotterdam



Vulnerable Plaque, Vulnerable Neointima

Clinical Application of VH, OCT and NIR - Safety, Pitfalls and Future Direction -

**E. Regar
Thoraxcenter
Erasmus Medical Center
Rotterdam
The Netherlands**

**ANGIOPLASTY SUMMIT
TCTAP 2012**

TRANS-CATHETER CARDIOVASCULAR THERAPEUTICS ASIA-PACIFIC

17TH
APRIL 24-27, 2012, SEOUL, KOREA
SHERATON GRAND WALKERHILL HOTEL



Vulnerable Plaque, Vulnerable Neointima

Intravascular Ultrasound

IVUS VH

Near Infrared Spectroscopy

NIRS

Safety

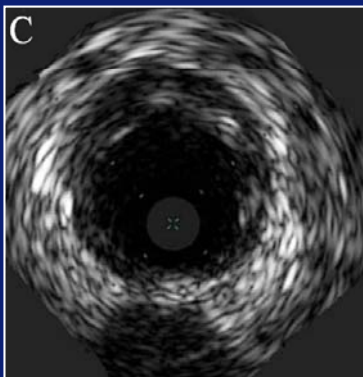


Optical Coherence Tomography

OCT

IVUS VH Safety

IVUS



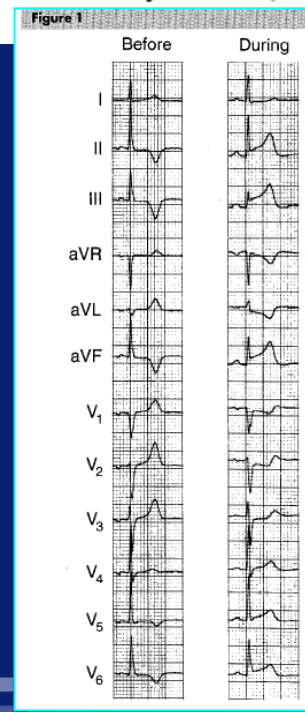
Frequency, duration, magnitude, and consequences of myocardial ischemia during intracoronary ultrasonography



Barbara J. Drew, RN, PhD,^a Mary G. Adams, RN, MS,^a Denise K. McEldowney, RN, MS,^a Kimberly Y. Lau, RN, MS,^a Shu-Fen Wung, RN, MS,^a Christopher L. Wolfe, MD,^b Thomas A. Ports, MD,^b and Tony M. Chou, MD^b *San Francisco, Calif.*

1997: N=27 pts, IVUS 3.2-4.3F

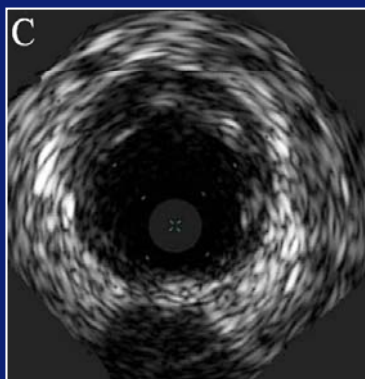
67% ischemia during IVUS imaging



IVUS VH Safety



IVUS



Journal of the American College of Cardiology
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Vol. 45, No. 4, 2005
ISSN 0735-1097/05/\$30.00
doi:10.1016/j.jacc.2004.10.063

Long-Term Safety of Intravascular Ultrasound in Nontransplant, Nonintervened, Atherosclerotic Coronary Arteries

Antoine Guédès, MD, Pierre-Frédéric Keller, MD, Philippe L. L'Allier, MD, Jacques Lespérance, MD,
Jean Grégoire, MD, Jean-Claude Tardif, MD

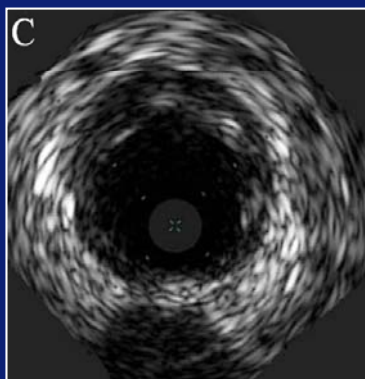
Montreal, Quebec, Canada

2005: N=525 pts, IVUS 2.9-3.2F

**is safe in nonintervened arteries and
does not accelerate coronary artery disease**

IVUS VH Safety

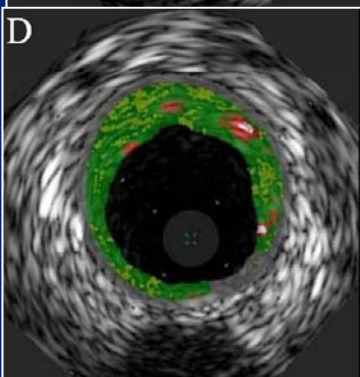
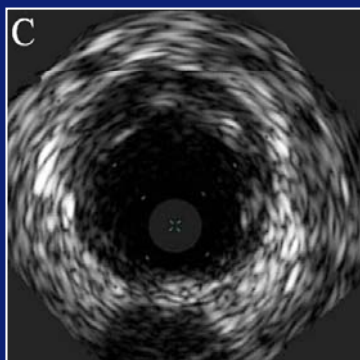
IVUS



■ Thermal injury	Temperature rise < 1K
■ Mechanical injury	Blood cells: None Endothelium: Minimal
■ Ischemia	67% ECG changes 22% Angina pectoris
■ Coronary spasm	0.6% - 3%
■ Dissection	0.1% - 0.3%
■ Abrupt vessel occlusion	0.2%
■ Thrombus formation	0.05%
■ Coronary embolism	0.05%
■ Myocardial infarction	0.01%

IVUS VH Safety

IVUS VH



The NEW ENGLAND JOURNAL of MEDICINE

ORIGINAL ARTICLE

A Prospective Natural-History Study of Coronary Atherosclerosis

Gregg W. Stone, M.D., Akiko Maehara, M.D., Alexandra J. Lansky, M.D.,
Bernard de Bruyne, M.D., Ecaterina Cristea, M.D., Gary S. Mintz, M.D.,
Roxana Mehran, M.D., John McPherson, M.D., Naim Farhat, M.D.,
Steven P. Marso, M.D., Helen Parise, Sc.D., Barry Templin, M.B.A.,
Roseann White, M.A., Zhen Zhang, Ph.D., and Patrick W. Serruys, M.D., Ph.D.,
for the PROSPECT Investigators*

Imaging Complications

- All 1.6%
- Myocardial infarction 0.5%



Vulnerable Plaque, Vulnerable Neointima

Intravascular Ultrasound

IVUS VH

Near Infrared Spectroscopy

NIRS

Optical Coherence Tomography

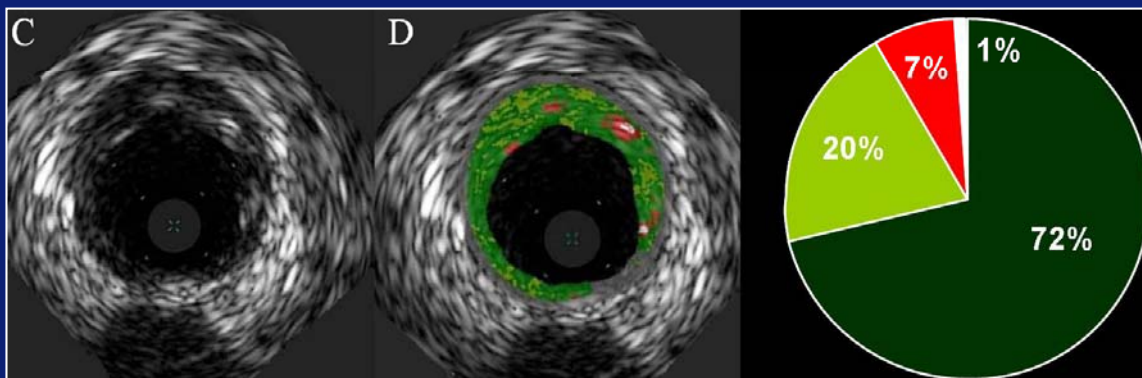
OCT

**Safety
Pitfalls**



IVUS VH

IVUS VH



VH	Color	Accuracy
Fibrous	Dark Green	87 %
Fibro-fatty	Light Green	87 %
Necrotic core	Red	88 %
Dense calcium	White	97 %

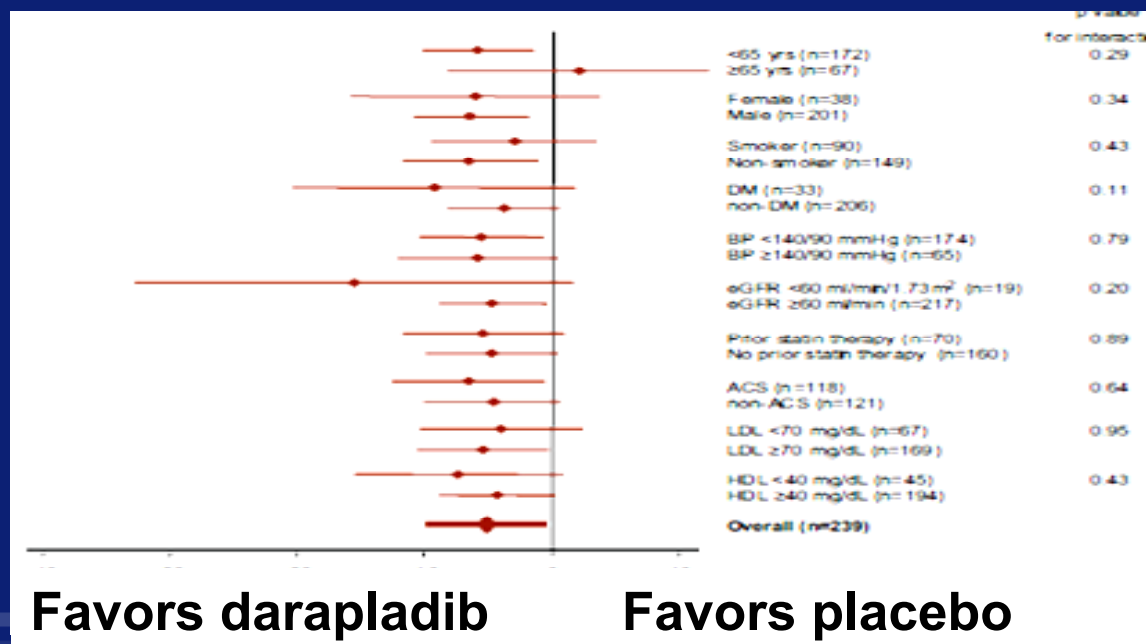
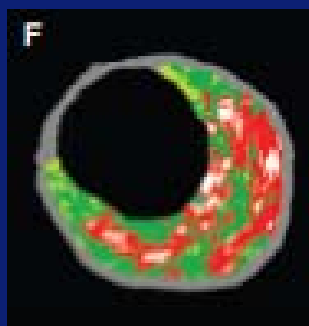


IVUS Tissue Characterization Clinical Trials: IBIS

IBIS 1
Observational, exploratory study

IBIS 2
Prospective, randomized, multicenter study

Difference in
**necrotic core
volume**



IVUS Tissue Characterization Clinical Trials: Atheroremo

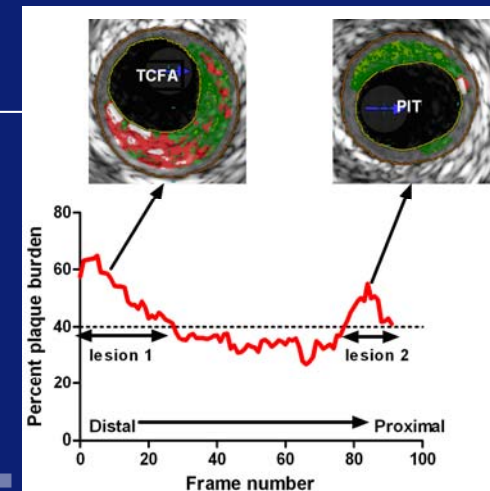


European Collaborative Project on Inflammation and Vascular Wall Remodeling in Atherosclerosis

Atheroremo - ongoing

Observational, exploratory study, n=850 pts

To assess the **interplay between the vulnerable plaque** as determined **by IVUS-VH and genetic profile, biomarkers of inflammation and vascular injury**





IVUS Tissue Characterization

Clinical Trials: PROSPECT

PROSPECT: Primary Endpoint

MACE attributable to rapid angiographic progression of a non-culprit lesion*

- Cardiac death
- Cardiac arrest
- Myocardial infarction
- Unstable angina
 - Requiring revascularization
 - Requiring rehospitalization
- Increasing angina
 - Requiring revascularization
 - Requiring rehospitalization

Most severe

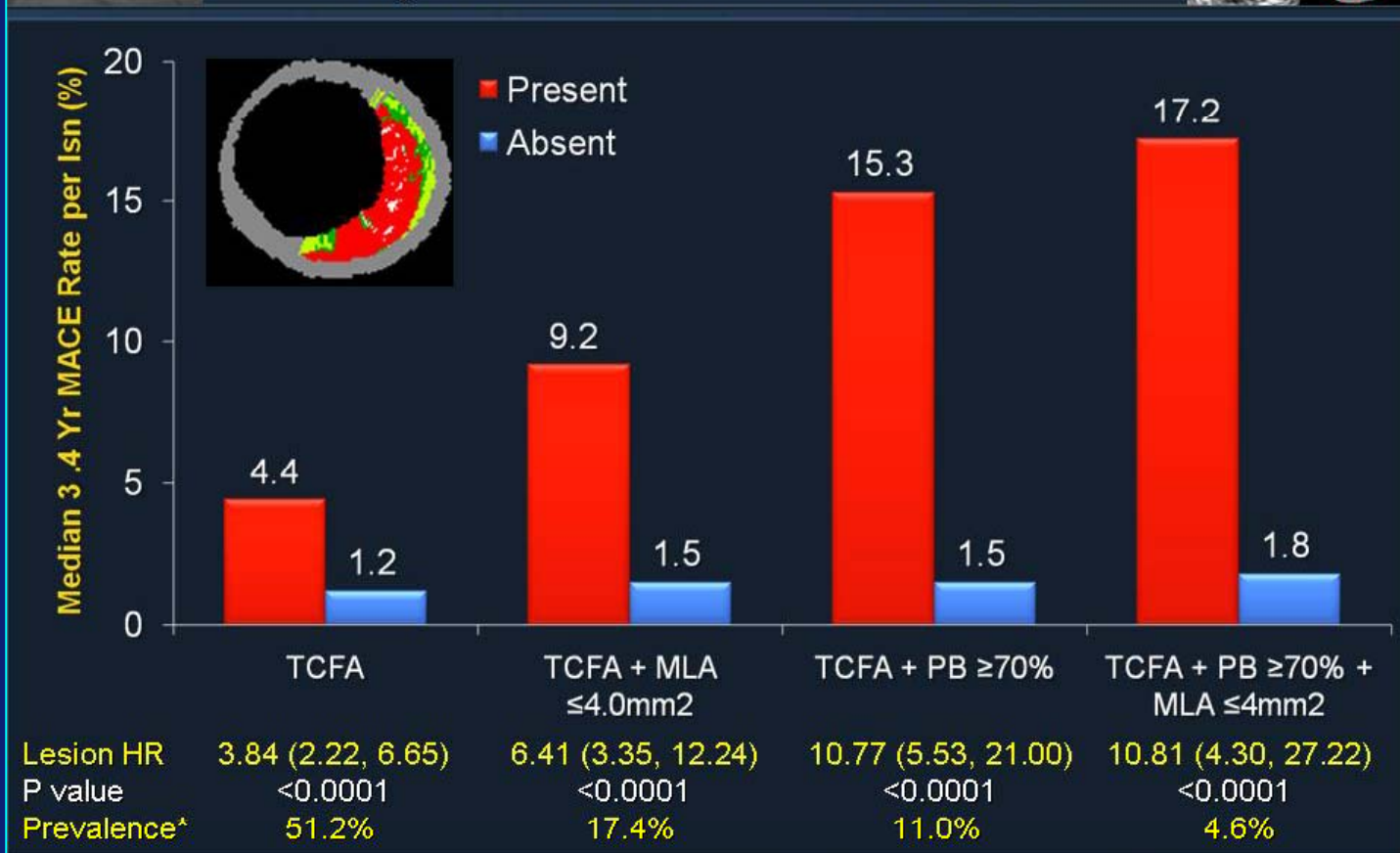
Hierarchical

Least severe

MACE during FU were adjudicated by the CEC as attributable to culprit lesions (those treated during or before the index hospitalization) or non culprit lesions (untreated areas of the coronary tree) based on angiography (+ECGs, etc.) at the time of the event; events occurring in pts without angiographic follow-up were considered indeterminate in origin. Rapid lesion progression = \uparrow in QCA DS by $>20\%$ from baseline to FU.

IVUS Tissue Characterization Clinical Trials: PROSPECT

PROSPECT: VH-TCFA and Non Culprit Lesion Related Events



Lesion HR	3.84 (2.22, 6.65)	6.41 (3.35, 12.24)	10.77 (5.53, 21.00)	10.81 (4.30, 27.22)
P value	<0.0001	<0.0001	<0.0001	<0.0001
Prevalence*	51.2%	17.4%	11.0%	4.6%

*Likelihood of one or more such lesions being present per patient. PB = plaque burden at the MLA



IVUS VH Pitfalls (1)

The NEW ENGLAND JOURNAL of MEDICINE

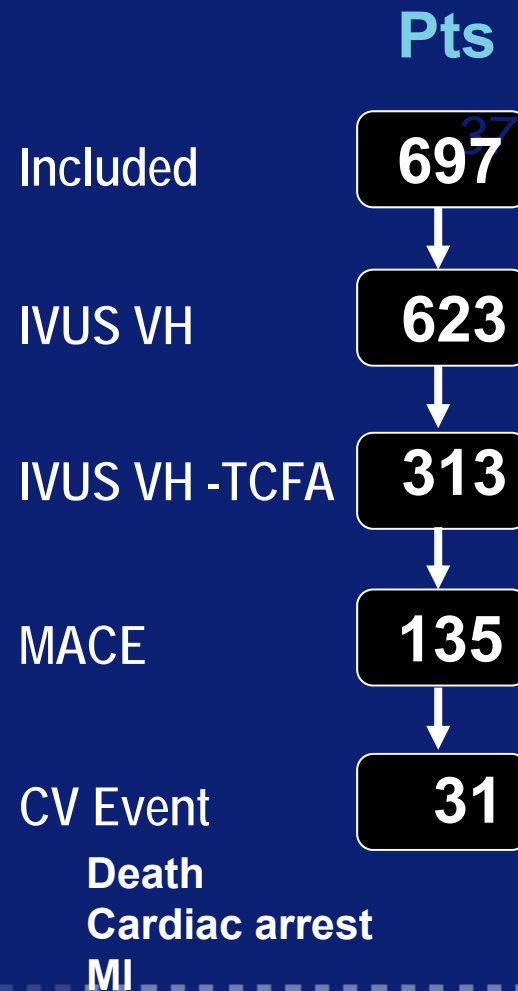
ORIGINAL ARTICLE

A Prospective Natural-History Study of Coronary Atherosclerosis

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for the PROSPECT Investigators*

Patients with ACS (NSTEMI & STEMI)
Medication use as to local standard!

FUP 3.4 years





IVUS VH Pitfalls (1)

The NEW ENGLAND JOURNAL of MEDICINE

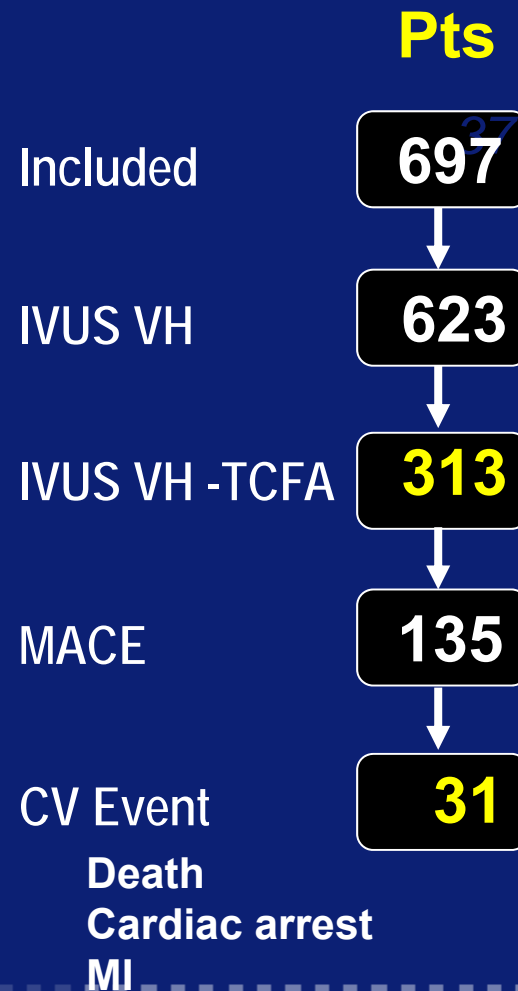
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IVUS VH Pitfalls (1)

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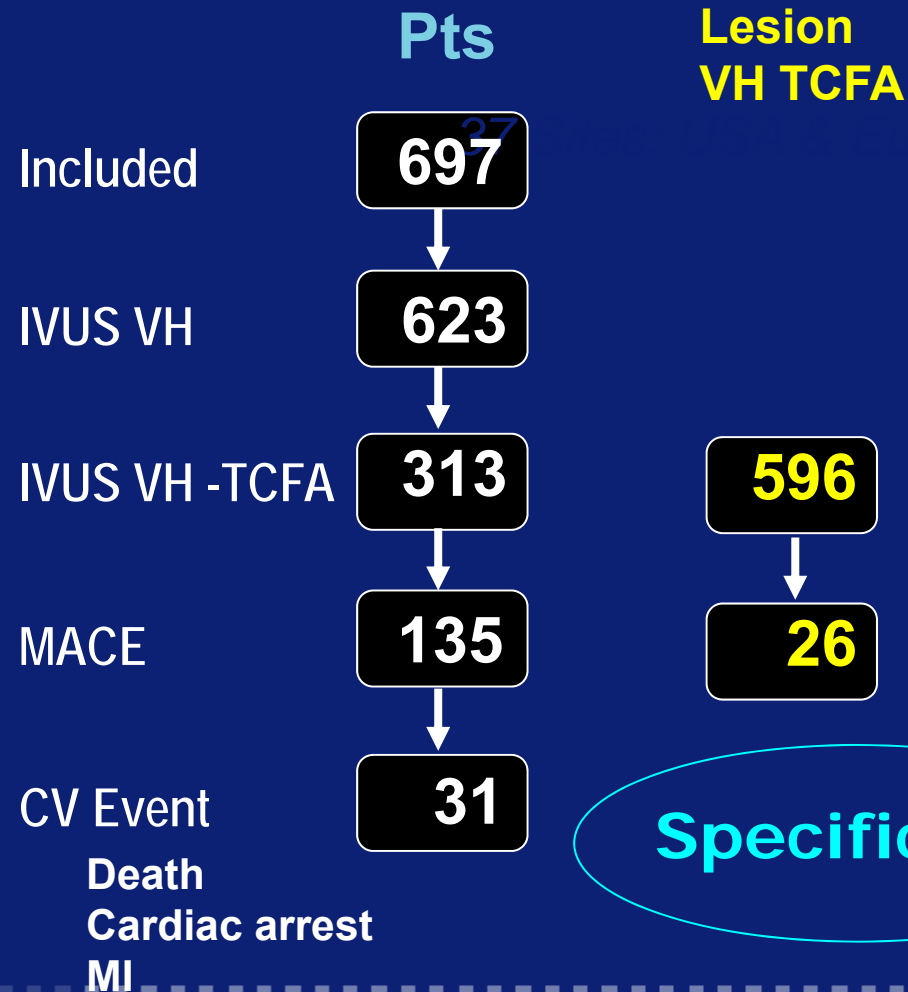
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Patients with ACS (NSTEMI & STEMI)
Medication use as to local standard!

FUP 3.4 years



Specificity?



IVUS VH Pitfalls (2)

Erasmus MC



Coronary Plaque Classification With Intravascular Ultrasound Radiofrequency Data Analysis

Anuja Nair, MS; Barry D. Kuban, BS; E. Murat Tuzcu, MD; Paul Schoenhagen, MD;
Steven E. Nissen, MD; D. Geoffrey Vince, PhD

Background—Atherosclerotic plaque stability is related to histological composition. However, current diagnostic tools do not allow adequate in vivo identification and characterization of plaques. Spectral analysis of backscattered intravascular ultrasound (IVUS) data has potential for real-time in vivo plaque classification.

Methods and Results—Eighty-eight plaques from 51 left anterior descending coronary arteries were imaged ex vivo at physiological pressure with the use of 30-MHz IVUS transducers. After IVUS imaging, the arteries were pressure-fixed and corresponding histology was collected in matched images. Regions of interest, selected from histology, were 101 fibrous, 56 fibrolipidic, 50 calcified, and 70 calcified-necrotic regions. Classification schemes for model building were computed for autoregressive and classic Fourier spectra by using 75% of the data. The remaining data were used for validation. Autoregressive classification schemes performed better than those from classic Fourier spectra with accuracies of 90.4% for fibrous, 92.8% for fibrolipidic, 90.9% for calcified, and 89.5% for calcified-necrotic regions in the training data set and 79.7%, 81.2%, 92.8%, and 85.5% in the test data, respectively. Tissue maps were reconstructed with the use of accurate predictions of plaque composition from the autoregressive classification scheme.

Conclusions—Coronary plaque composition can be predicted through the use of IVUS radiofrequency data analysis. Autoregressive classification schemes performed better than classic Fourier methods. These techniques allow real-time analysis of IVUS data, enabling in vivo plaque characterization. (*Circulation*. 2002;106:2200-2206.)

Key Words: atherosclerosis ■ coronary disease ■ Fourier analysis ■ plaque ■ ultrasonics

No validation
in stented segments

-Plaque behind stent

-Tissue coverage at fup



Vulnerable Plaque, Vulnerable Neointima

Intravascular Ultrasound

IVUS VH

Near Infrared Spectroscopy

NIRS

Optical Coherence Tomography

OCT

Near Infrared Spectroscopy (NIRS)

Unique Aspects:

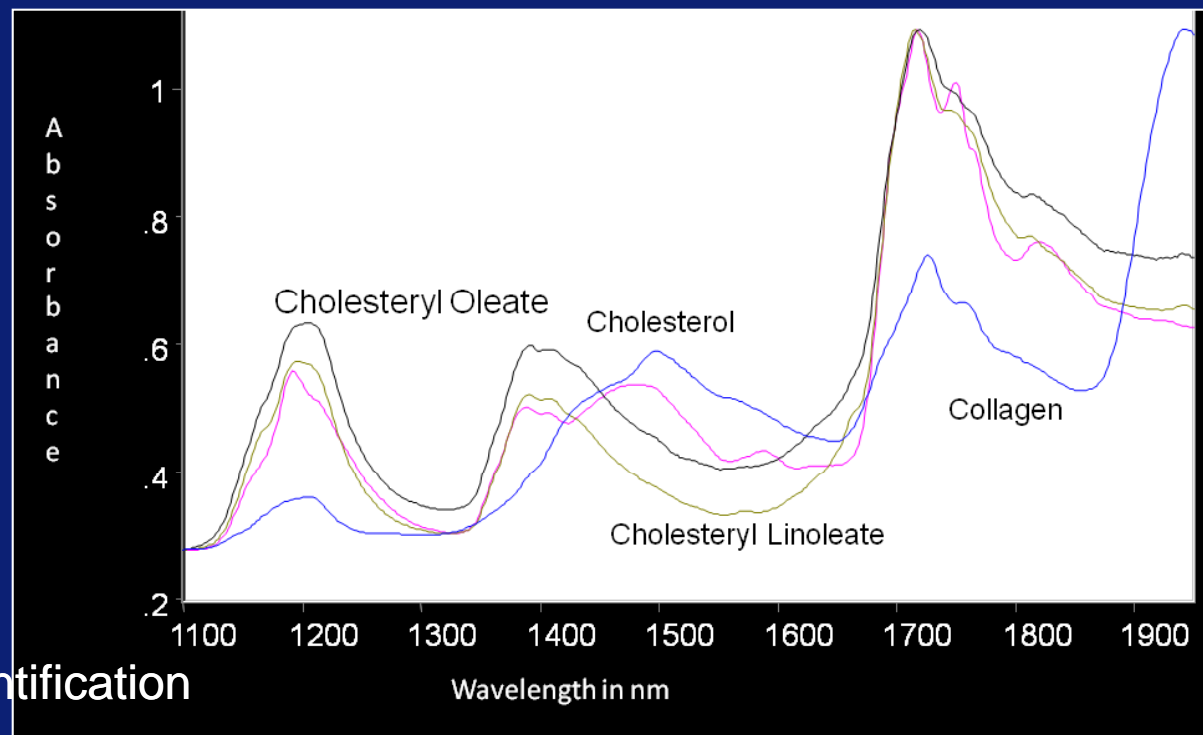
NIR Spectra can uniquely identify organic chemicals.
NIR Spectra are chemical finger prints.

Industry:

- Pharmaceutical;
- Food;
- Agriculture;
- Petrochemical;
- Medical.

Techniques:

- Process control
- Unknown substance identification



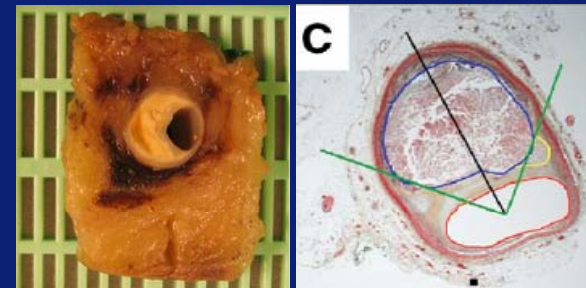
Intracoronary Near Infrared Spectroscopy (NIRS) Lipid Core Plaque (LCP) Algorithm



- Intracoronary catheter: 3.2F fibre optic catheter
- Spectra processed by algorithm and displayed to user as a chemical image of lipid rich plaque probability (“Chemogram”)

Algorithm Calibration

- 4.2 meters of artery from 33 autopsy hearts.
- **Lipid Core Plaque (LCP)** defined as:
 - Fibroatheroma > 200 μm thick
 - > 60 deg angular extent
 - Cap < 450 μm thick



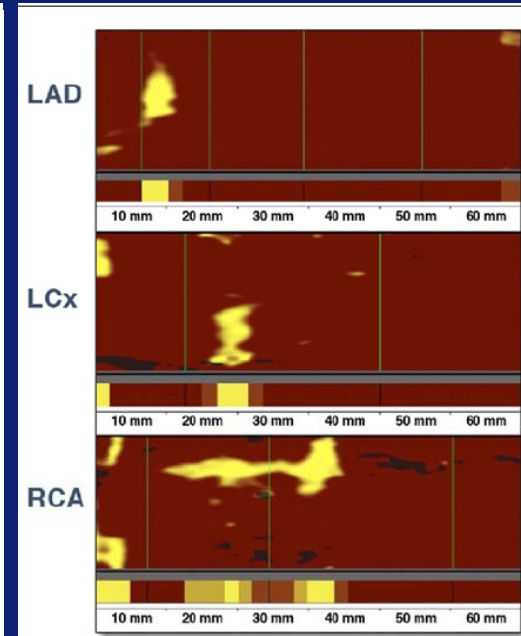
NIRS: Distance From the Ostium A Predictor of Lipid Core Plaque ?

BRIEF REPORT

Distance of Lipid Core–Rich Plaques From the Ostium by NIRS in Nonculprit Coronary Arteries

Salvatore Brugaletta, MD,*† Hector M. Garcia-Garcia, MD, PhD,*†
Patrick W. Serruys, MD, PhD,* Josep Gomez-Lara, MD,* Sanneke de Boer, MD,*
Jurgen Ligthart, BSc,* Karen Witberg, RN,* Cihan Simsek, MD,*
Robert-Jan van Geuns, MD, PhD,* Carl Schultz, MD, PhD,*
Henricus J. Duckers, MD, PhD,* Nicolas van Mieghem, MD,* Peter de Jaegere, MD, PhD,*
Sean P. Madden, PhD,§ James E. Muller, MD,§ Antonius F. W. van der Steen, PhD,*
Eric Boersma, PhD,* Wim J. van der Giessen, MD, PhD,* Felix Zijlstra, MD, PhD,*
Evelyn Regar, MD, PhD*

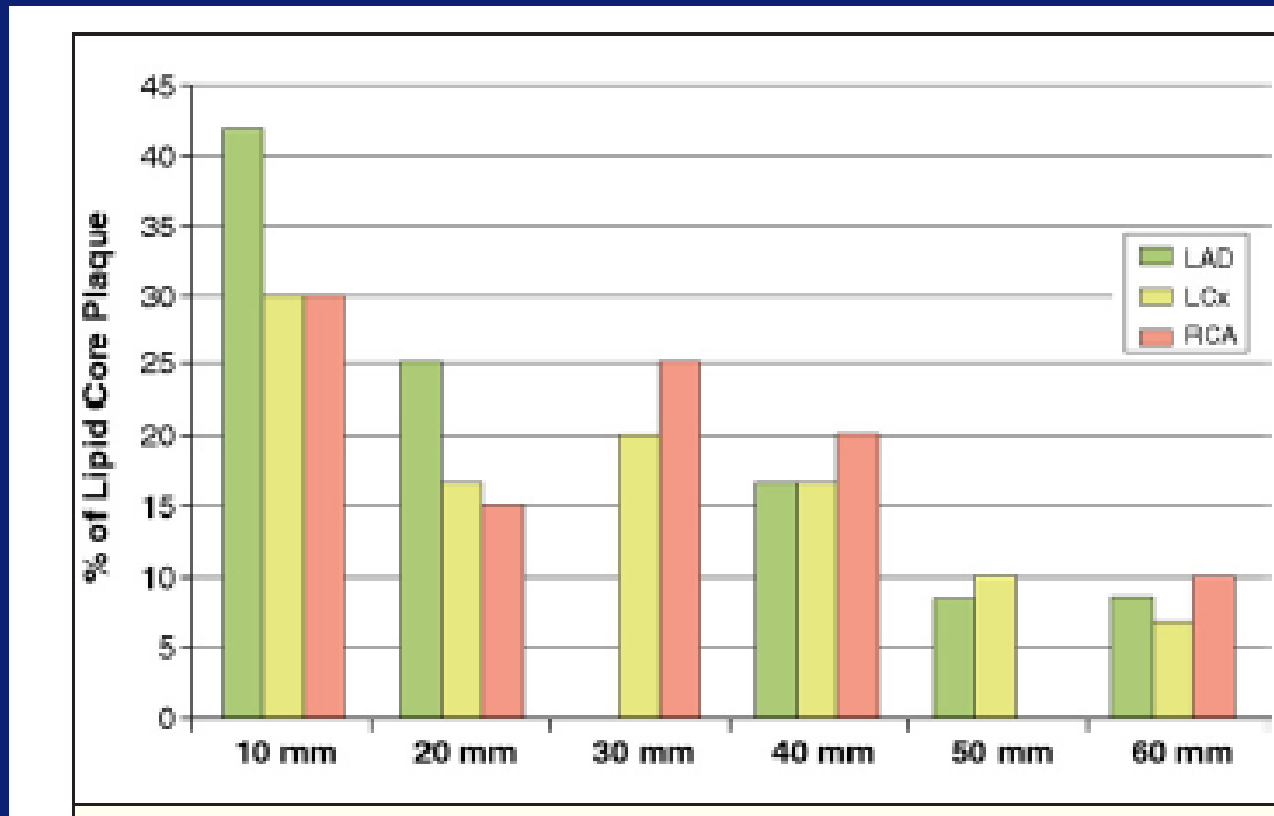
Rotterdam, the Netherlands; Barcelona, Spain; and Burlington, Massachusetts



Single center,
observational study
N=68 Pts
Non culprit arteries
ROI 58 ± 4.3 mm

NIRS: Distance From the Ostium A Predictor of Lipid Core Plaque ?

*Distance from the ostium
is an independent predictor of LCP: OR 0.37 ; CI 0.20-0.69*



Single center,
observational study
N=68 Pts
Non culprit arteries
ROI 58 ± 4.3 mm



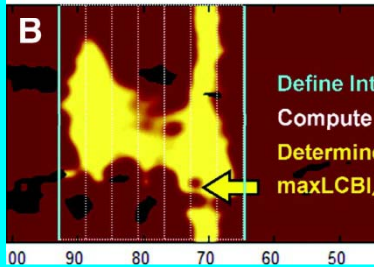
Immediate Stent Complication: Distal Embolization - NIRS Plaque Evaluation

Detection of Lipid-Core Plaques by Intracoronary Near-Infrared Spectroscopy Identifies High Risk of Periprocedural Myocardial Infarction

James A. Goldstein, MD; Brijeshwar Maini, MD; Simon R. Dixon, MBChB;
Emmanouil S. Brilakis, MD, PhD; Cindy L. Grines, MD; David G. Rizik, MD; Eric R. Powers, MD;
Daniel H. Steinberg, MD; Kendrick A. Shunk, MD, PhD; Giora Weisz, MD; Pedro R. Moreno, MD;
Annapoorna Kini, MD; Samin K. Sharma, MD; Michael J. Hendricks, BS; Steve T. Sum, PhD;
Sean P. Madden, PhD; James E. Muller, MD; Gregg W. Stone, MD; Morton J. Kern, MD

Chemogram intervention zones n=62

Maximum 4-mm subsegment lipid-core burden index



Parameter*	Threshold†	Relative risk of periprocedural MI		
		Relative risk of peri-procedural MI (95% CI)	p‡	
maxLCBI _{4mm}	≥500	12 (3.3 to 48)	0.0002	
LDL – mg/dL	>100	5.4 (1.4 to 23)	0.03 ^s	
Complex Plaque	Y	3.5 (0.91 to 14)	0.15	
Degree Stenosis – %	>75	3.1 (0.92 to 11)	0.14 ^{**}	



Vulnerable Plaque, Vulnerable Neointima

Intravascular Ultrasound

IVUS VH

Near Infrared Spectroscopy

NIRS

Optical Coherence Tomography

OCT

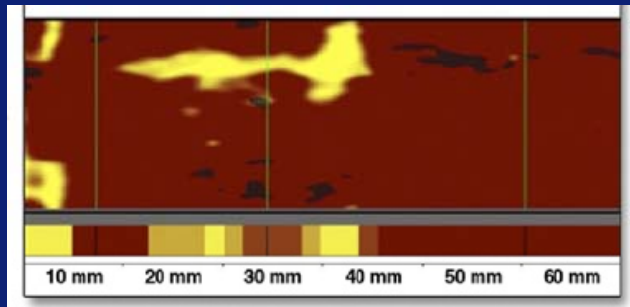
Pitfalls





NIRS Pitfalls (1)

Chemogram



- Poor orientation within the artery
- No anatomic structures
- No information on the extent of plaque



NIRS Pitfalls -> Solution

- Catheter: 3.2Fr, 6Fr compatible, 0.014" guidewire
- NIRS: Same as LipiScan™, cleared by FDA Apr '08
- Ultrasound: 40MHz, 16 fps
- Pullback speed: 0.5mm/sec
- **Single catheter & pullback, thru blood**
→ simultaneous, co-registered NIR & IVUS data

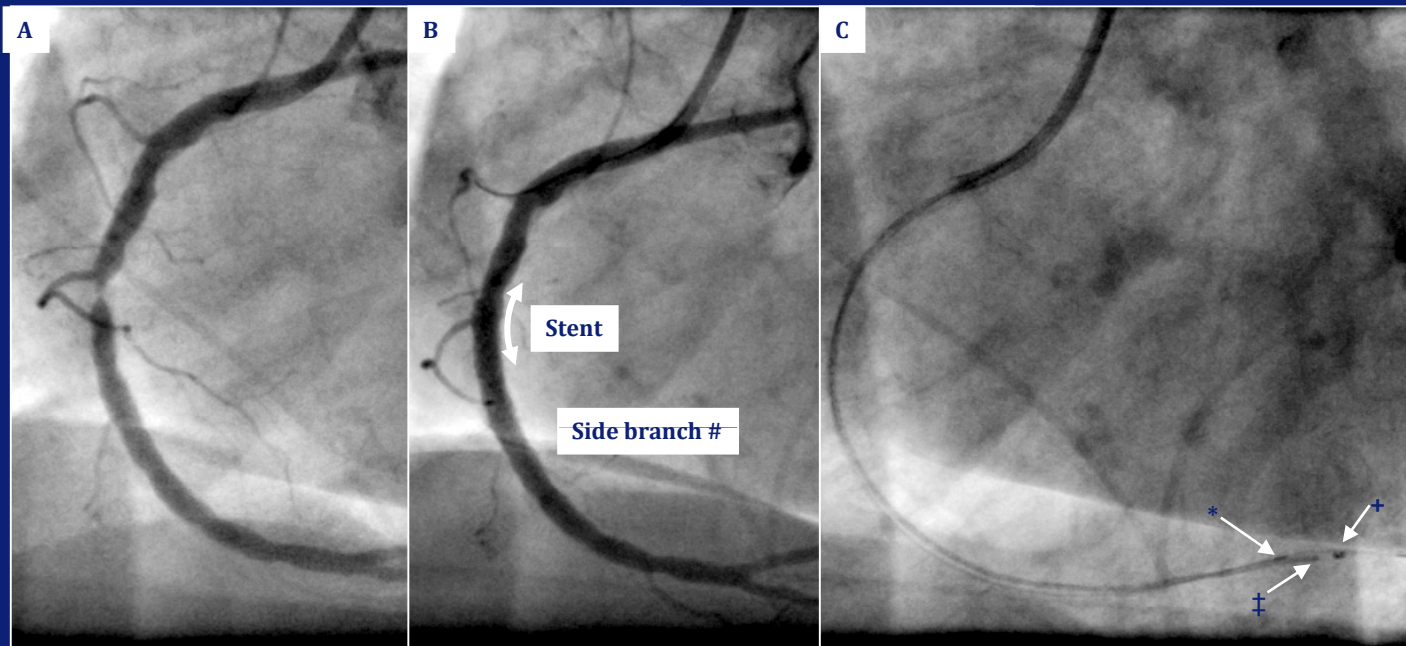


Savoir Trial

First in Man Evaluation of a Combined Optical/Ultrasound Catheter

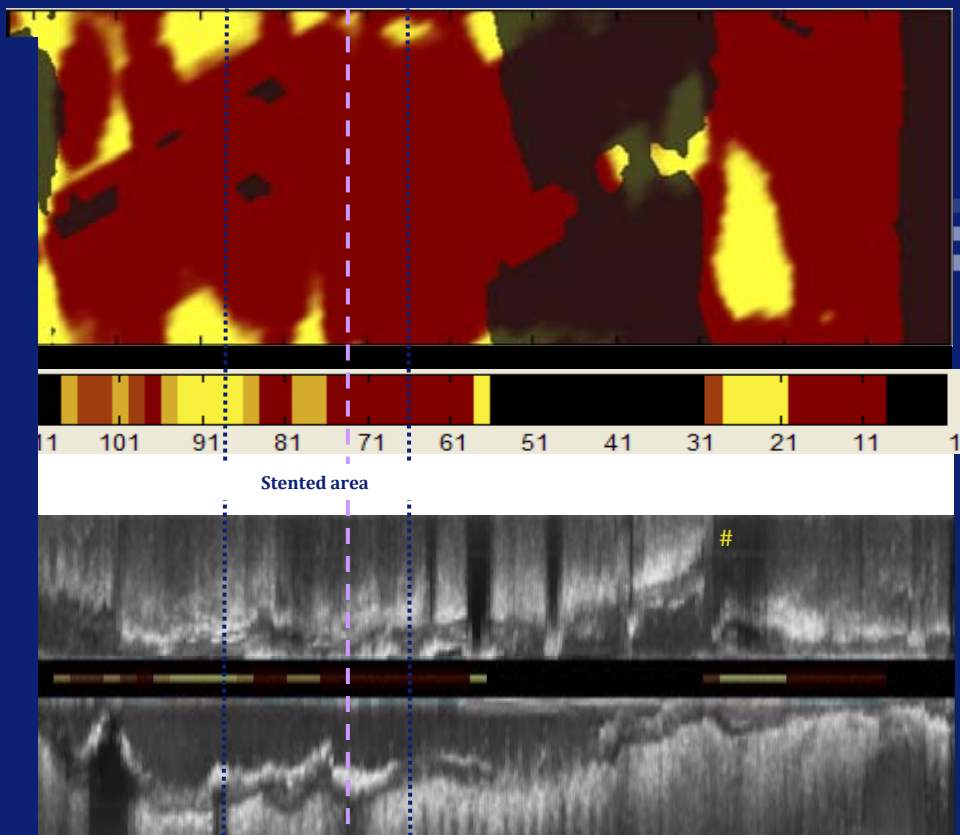


Simultaneous Acquisition of Intravascular Ultrasound and Near Infrared Spectroscopy Data in the Coronary Artery Study





Chemogram



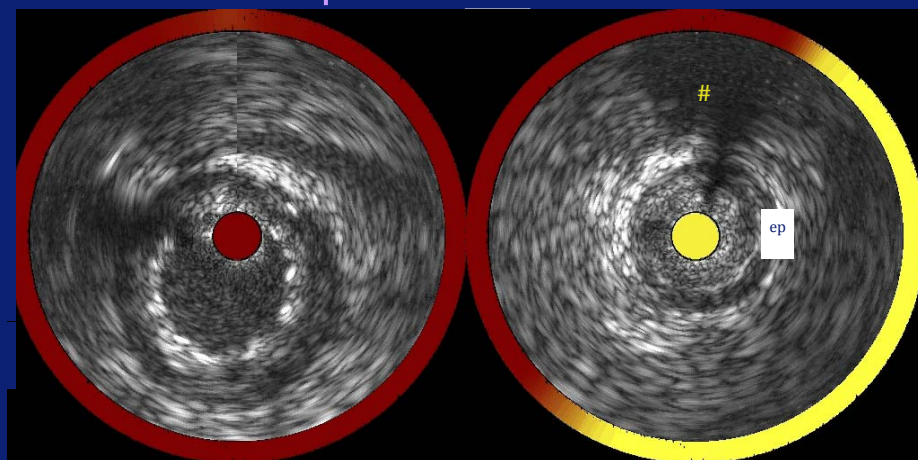
Block chemogram

Automated Detection
of Lipid-core Plaques

Longitudinal IVUS

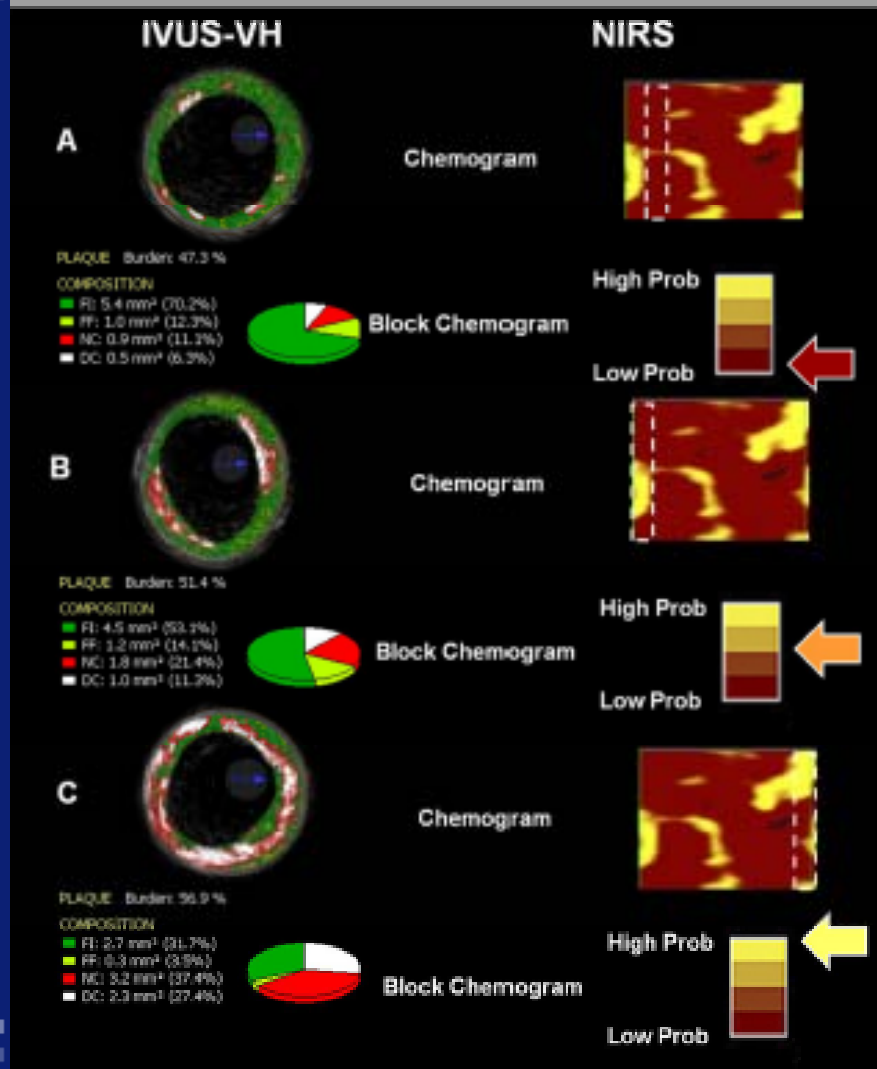
Cross sectional IVUS

- Lumen Dimension
- Plaque Size
- Stent Expansion





NIRS Pitfalls (2)



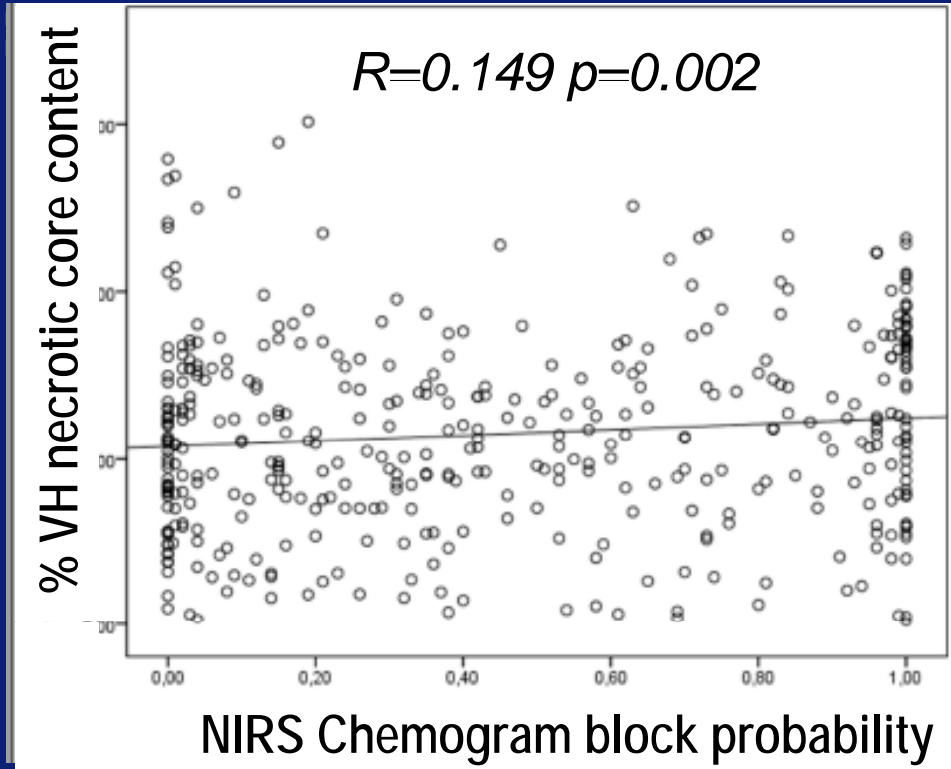
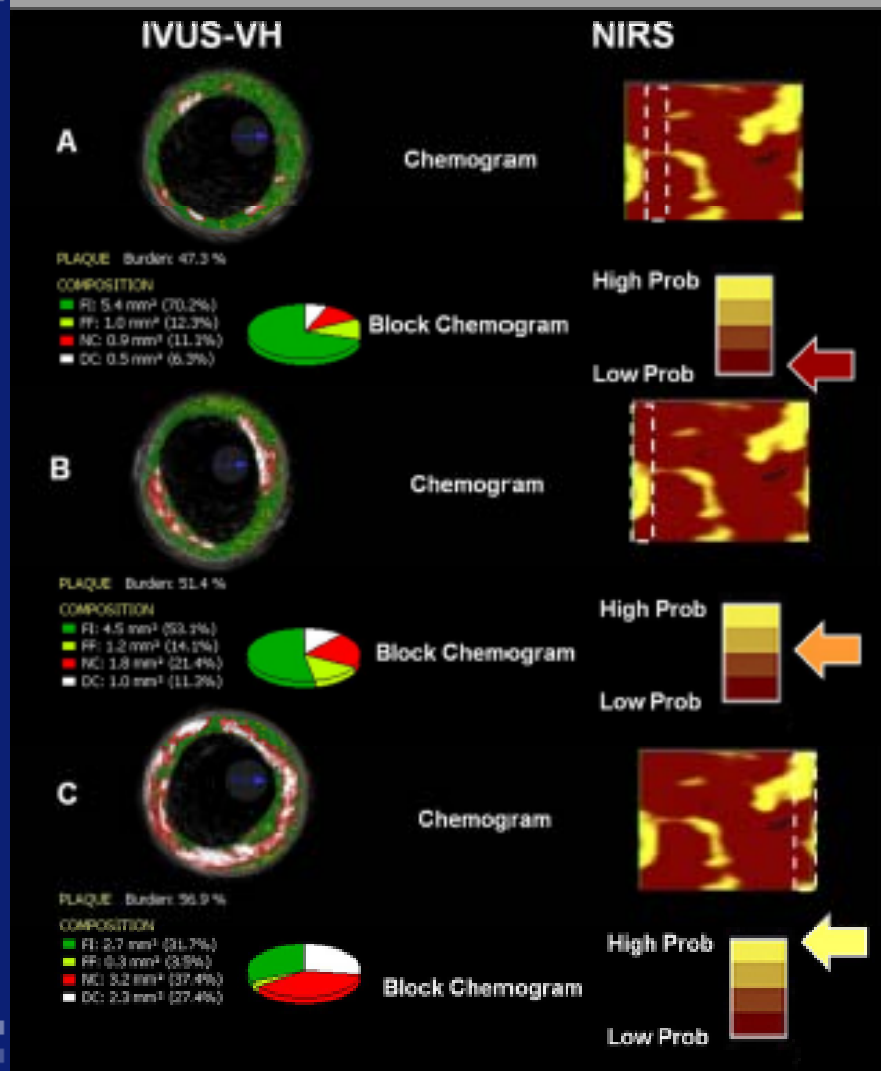
NIRS and IVUS for Characterization of Atherosclerosis in Patients Undergoing Coronary Angiography

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 Patrick W. Serruys, MD, PhD,* Sanneke de Boer, MD,* Jurgen Ligthart, BSC,*
 Josep Gomez-Lara, MD,* Karen Witberg, RN,* Roberto Diletti, MD,*
 Joanna Wykrzykowska, MD,*|| Robert-Jan van Geuns, MD, PhD,*
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 Wim J. van der Giessen, MD, PhD,* Eric Boersma, PhD*
 Rotterdam and Amsterdam, the Netherlands; Barcelona, Spain; and Burlington, Massachusetts

Does
 “lipid-core plaque” by NIRS &
 “necrotic core” by VH
 refer to the same anatomical substrate?



NIRS Pitfalls (2)



Does
“lipid-core plaque” by NIRS &
“necrotic core” by VH
refer to the same anatomical substrate?



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Intravascular Ultrasound

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Near Infrared Spectroscopy

NIRS

Safety



Optical Coherence Tomography

OCT

OCT Safety: 2nd Generation, Fourier Domain OCT



Safety and feasibility of frequency domain optical coherence tomography to guide decision making in percutaneous coronary intervention

Fabrizio Imola^{1,2}, MD; Maria Teresa Mallus¹, MD, PhD; Vito Ramazzotti¹, MD; Alessandro Manzoli¹, MD, PhD; Alessandro Pappalardo¹, MD; Alessandro Di Giorgio², MD; Mario Albertucci², MD; Francesco Prati^{1,2*}, MD

1. Interventional Cardiology, San Giovanni Hospital, Rome, Italy; 2. CLI Foundation, Rome, Italy

First-in-man evaluation of intravascular optical frequency domain imaging (OFDI) of Terumo: a comparison with intravascular ultrasound and quantitative coronary angiography

Takayuki Okamura¹, MD, PhD; Yoshinobu Onuma¹, MD; Héctor M. Garcia-Garcia², MD, PhD; Robert-Jan M van Geuns¹, MD, PhD; Joanna J. Wykrzykowska¹, MD; Carl Schultz¹, MD, PhD; Willem J van der Giessen¹, MD, PhD; Jurgen Ligthart¹, BSc; Evelyn Regar¹, MD, PhD; Patrick W Semaya^{1*}, MD, PhD

1. Thoraxcenter, Erasmus MC, Rotterdam, The Netherlands; 2. Cardology BV, Rotterdam, The Netherlands

Single center, n=90 pts

Imaging success 99.1%

X-ray contrast for flush 49.4 ± 19.0 ml

Serum creatinin pre 1.17 ± 0.12

Serum creatinin post 1.21 ± 0.19

Coronary spasm 1 pt

ECG changes 0 pt

Ventricular ectopic beats 3 pts

MACE 0 pt

Single center, n=19 pts

X-ray contrast for flush 15.4 ml

MACE 0 pt

How does the flushing procedure affect Renal function ?



Circulation Journal
Official Journal of the Japanese Circulation Society
<http://www.j-circ.or.jp>

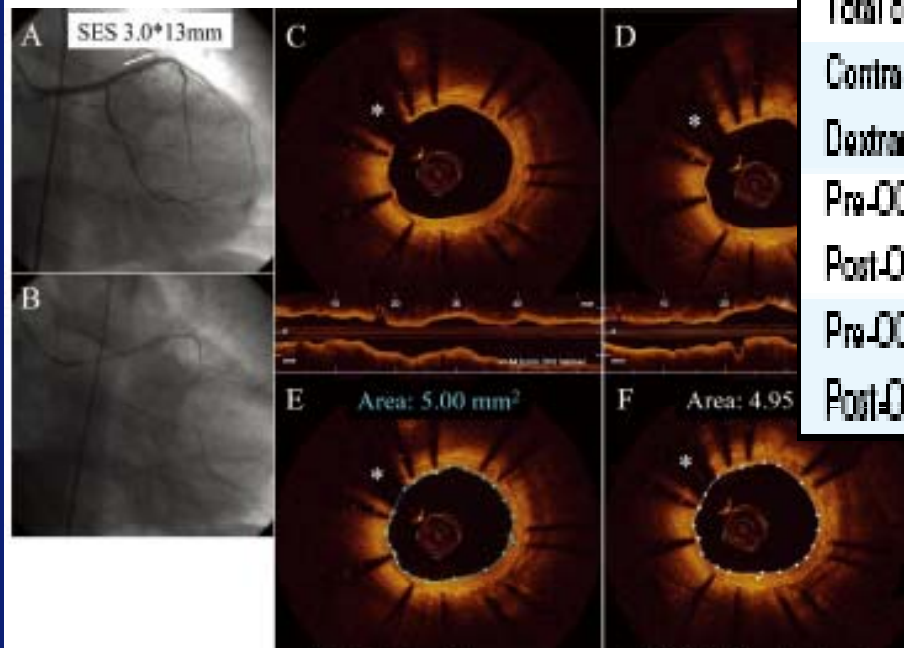
ORIGINAL ARTICLE
Imaging

Comparison of Contrast Media and Low-Molecular-Weight Dextran for Frequency-Domain Optical Coherence Tomography

Yuichi Ozaki, MD; Hironori Kitabata, MD, PhD; Hiroto Tsujioka, MD, PhD; Seiki Hosono, MD; Manabu Kashiwagi, MD; Kohei Ishibashi, MD; Kenichi Komukai, MD; Takashi Tanimoto, MD; Yasushi Ino, MD; Shigeho Takarada, MD, PhD; Takashi Kubo, MD, PhD; Keizo Kimura, MD; Atsushi Tanaka, MD, PhD; Kumiko Hirata, MD, PhD; Masato Mizukoshi, MD, PhD; Toshio Imanishi, MD, PhD; Takashi Akasaka, MD, PhD

Table 3. Contrast/dextran Volume and Renal Function

Total contrast media including that for OCT image (ml)	183±43
Total contrast media excluding that for OCT image (ml)	166±44
Contrast for OCT (ml)	16.8±1.7
Dextran for OCT (ml)	18.4±4.2
Pre-OCT Cr (mg/dl)	0.83±0.24
Post-OCT Cr (mg/dl)	0.82±0.24
Pre-OCT eGFR (ml·min ⁻¹ ·1.73m ⁻²)	60.9±17.9
Post-OCT eGFR (ml·min ⁻¹ ·1.73m ⁻²)	60.9±16.7



FD-OCT X-ray contrast

dextran L

2nd Generation OCT at Thoraxcenter Patient Population (n=838)



Age (Years)	61 ± 10	
Male	628	(75%)
Risk factors		
Hypertension	439	(52%)
Diabetes	142	(18%)
Dyslipidemia	483	(58%)
Smoking	380	(45%)
Family history CAD	377	(45%)
Prior MI	267	(32%)
Prior CABG	49	(6%)
Prior PCI	411	(49%)
Clinical presentation		
Stable angina	299	(36%)
Unstable angina	178	(21%)
AMI	208	(25%)
Previous PCI/Fup	144	(18%)

2nd Generation OCT at Thoraxcenter Patient Population (n=838)



Major complications during or within 24 hour after the procedure

Death	0
Cerebral infarction	0
TIA	0
Myocardial infarction	0
Emergency CABG	0

Adverse events during or within 24 hour after the procedure*

ECG changes	0
Arrhythmia	3
VF	0
Vasospasm	2

* Non self-limiting



Vulnerable Plaque, Vulnerable Neointima

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IVUS VH

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Optical Coherence Tomography

OCT

Pitfalls





OCT Plaque Characterization In Vivo Coronary Arteries

Fibroatheroma (A)

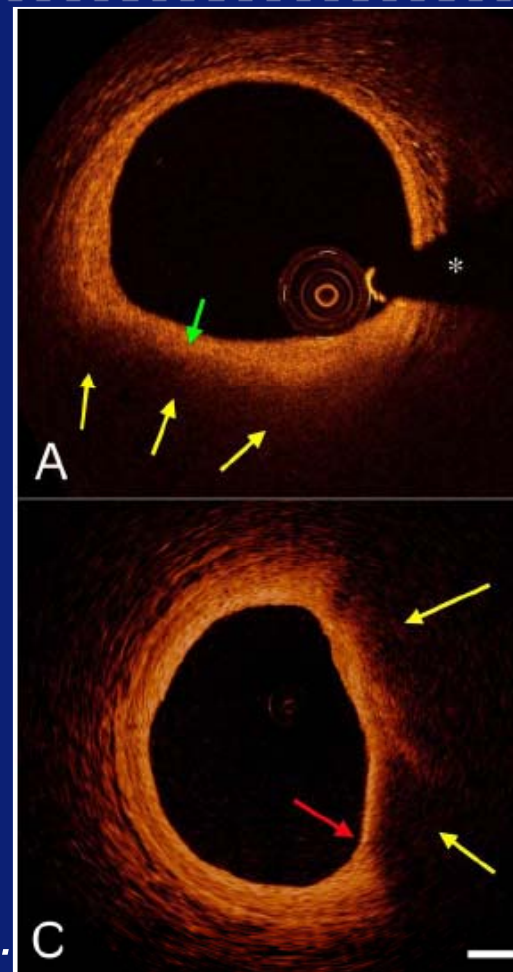
lesion with an OCT-delineated fibrous cap and a lipid pool

OCT thin cap fibroatheroma (C)

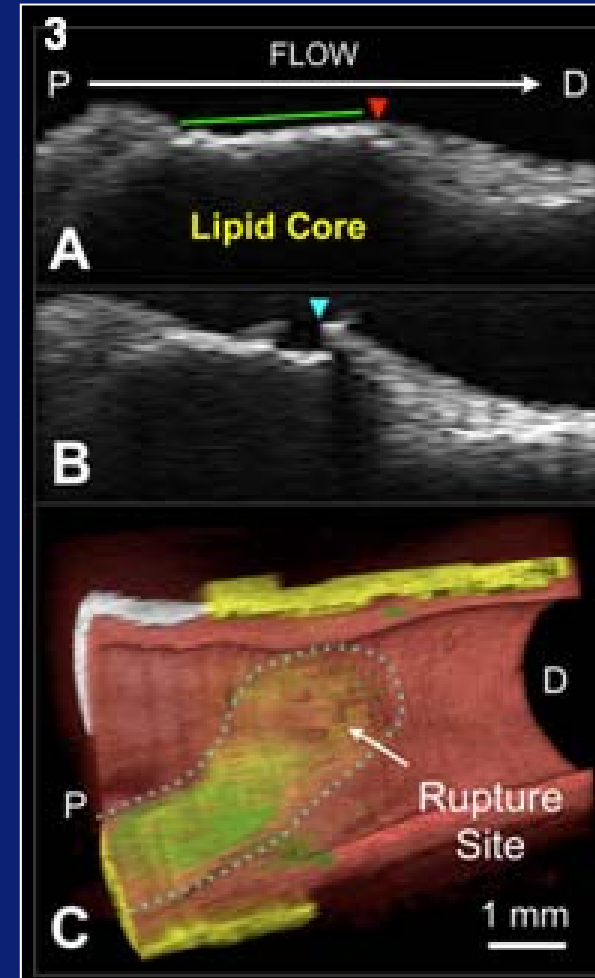
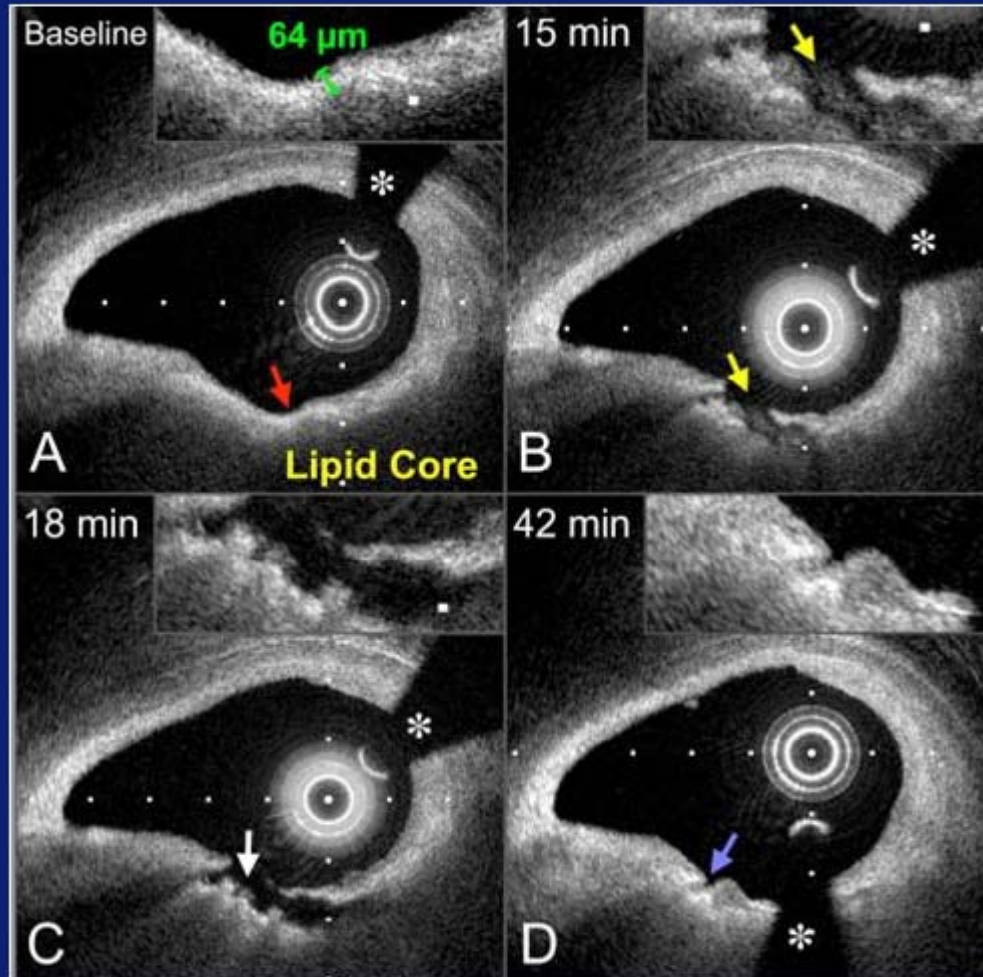
an OCT-delineated necrotic core with an overlying fibrous cap where the min. thickness is less than a predetermined threshold

Fibrous cap

is a tissue layer, which is often signal-rich, overlying a lipid pool, necrotic core, or calcium.



OCT: Witnessed Plaque Rupture





OCT Pitfalls (1)

OCT TCFA - Comparison to Histologic Classification



OCT	Fibrous tissue area		
	Thick <i>160-910 μm</i>	Medium-thin <i>90-140 μm</i>	Thin <i>30-60 μm</i>
	38	9	13
Histo	25 <i>Thick fibrous cap</i> 8 <i>Fibro-calcific</i> 5 <i>Fibrous</i>		11 <i>Thin fibrous cap</i> 11 <i>Fibro-calcific</i>

to 2 main limitations of OCT imaging. First, the penetration depth of OCT is limited to 1 to 2 mm, which does not allow the accurate detection of signal-poor areas possibly representing lipid pools or calcium behind fibrous tissue. This may generate false-positive fibrous plaques, false-negative fibrocalcific plaques, and false-negative thick-cap fibroatheromas. Second, OCT analysis often confuses the presence of lipid pools with that of calcium deposits, or vice versa. As



OCT Pitfalls (1)

Confusion of Lipid with Calcium

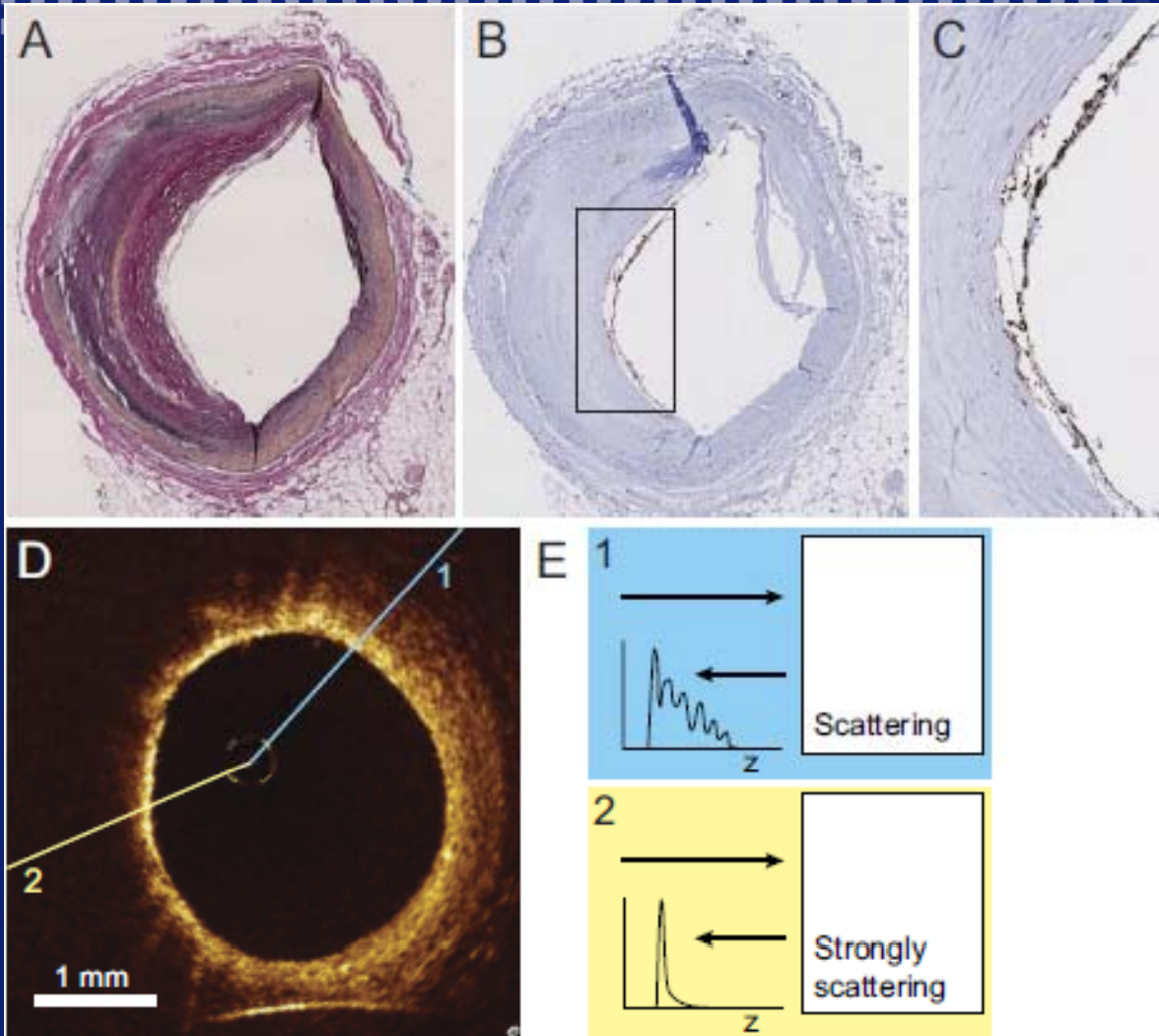
OCT	Calcified lesion	Lipid-rich lesion	Thin 30-60 μm
Histo			13
	<i>Sharply delineated borders</i>	<i>Diffuse borders</i>	thin fibrous cap pro-calcific

ing. First, the penetration
 nm, which does not allow
 poor areas possibly repre-
 behind fibrous tissue. This
 us plaques, false-negative
 negative thick-cap fibroathe-
 romas. Second, OCT analysis often confuses the presence of
 lipid pools with that of calcium deposits, or vice versa. As



OCT Pitfalls (2)

Artefacts: Macrophage scattering



The region of thickened intima appears as a TCFA due to strong scattering & shadowing by macrophages.



OCT Pifalls (2)

Artefacts cause misclassification!

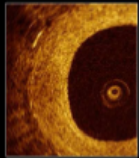
Incidence of artefacts in clinical setting

Category	# observations		
	Pullbacks	Sections	Frames
	Total 37		Total 4597
1: Superficial attenuation	16	26	94
2: Tangential signal dropout	15	27	145
3: Catheter shadowing	12	21	35
4: Axial PSF tail	0	0	0
5: Proximity brightening	12	17	313

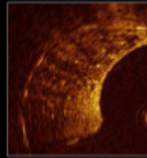


OCT Pifalls (3) Validation

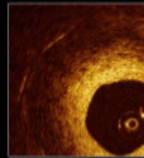
Restenotic tissue structure



Homogeneous: restenotic tissue has uniform optical properties and does not show focal variations in backscattering pattern.



Heterogeneous: restenotic tissue has focally changing optical properties and shows various backscattering patterns



Layered: restenotic tissue consists of concentric layers with different optical properties: an abluminal high scattering layer and an abluminal low scattering layer

Restenotic tissue backscatter

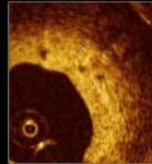


High: the majority of the tissue shows high backscatter and appears bright

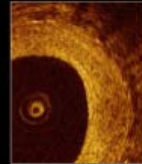


Low: the majority of the tissue shows low backscatter and appears dark or black

Microvessels visible

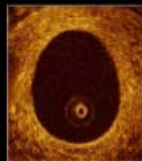


Yes: microvessels appear as well delineated low backscattering structures less than 200 micron in diameter that show a trajectory within the vessel



No

Lumen shape



Regular: lumen border is sharply delineated, smooth and circular

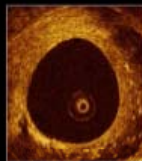


Irregular: lumen border is irregular with tissue protrusions from the vessel wall into the lumen

Presence of intraluminal material



Yes: there is visible material inside the vessel lumen.



No

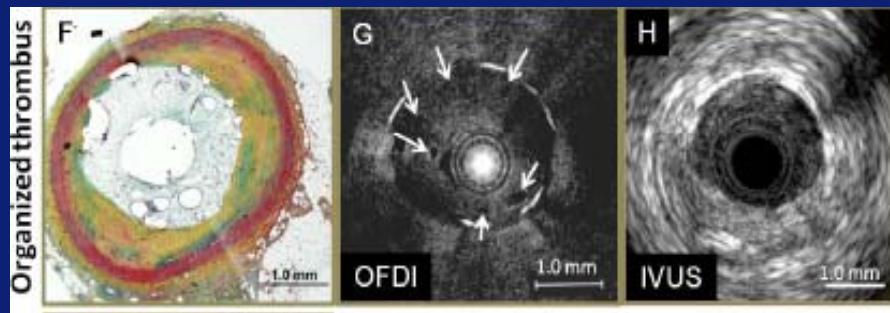
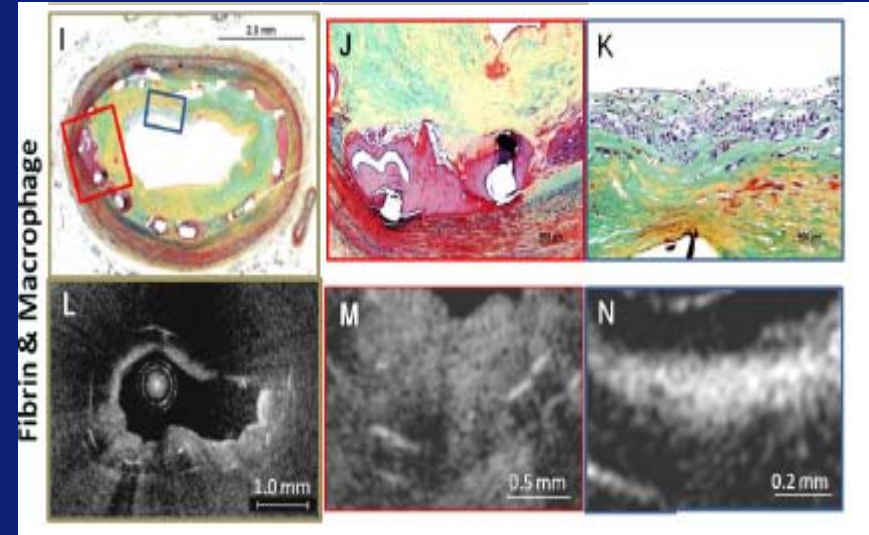
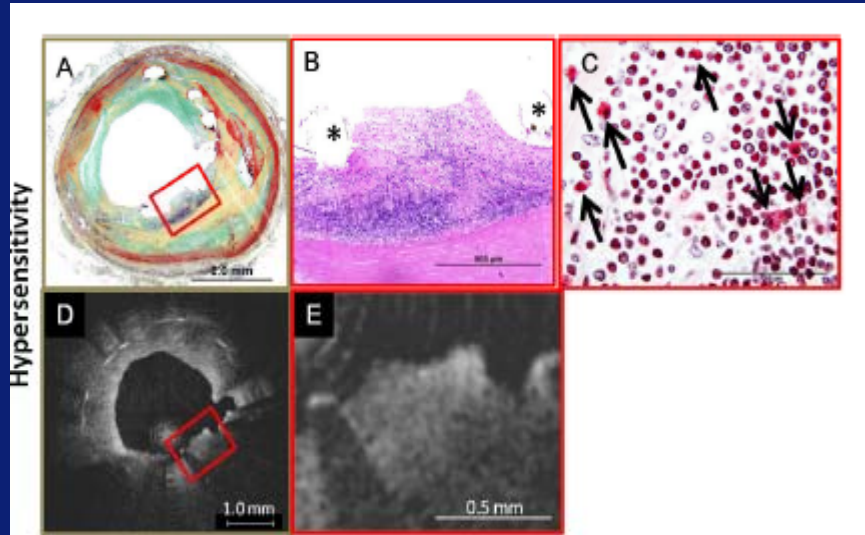
OCT Assessment of Strut Coverage Qualitative Parameters

Parameter	K
Restenotic tissue structure	0.92
Restenotic tissue backscatter	0.57
Lumen shape	0.85
Intraluminal material	0.83
Microvessels	0.79

Interobserver reproducibility



OCT Pifalls (3) Validation





Vulnerable Plaque, Vulnerable Neointima

Intravascular Ultrasound

IVUS VH

Near Infrared Spectroscopy

NIRS

Optical Coherence Tomography

OCT

**Safety
Pitfalls**



Future Directions



Vulnerable Plaque, Vulnerable Neointima

Technology

-Tissue characterization

IVUS VH

-Co- registration with the angiogram

NIRS

-3D rendering (real time)

OCT

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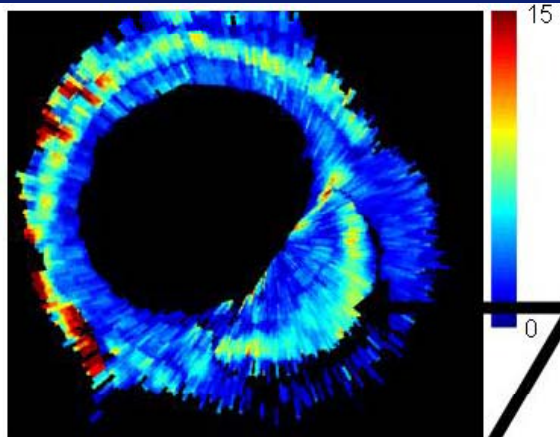
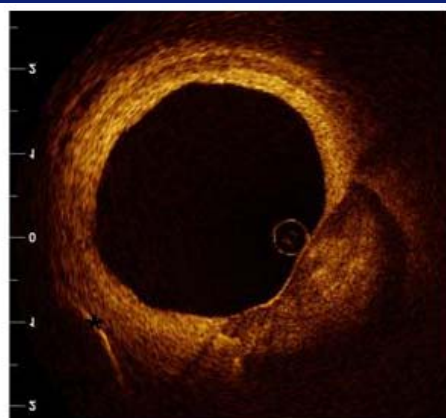
OCT

Future Directions

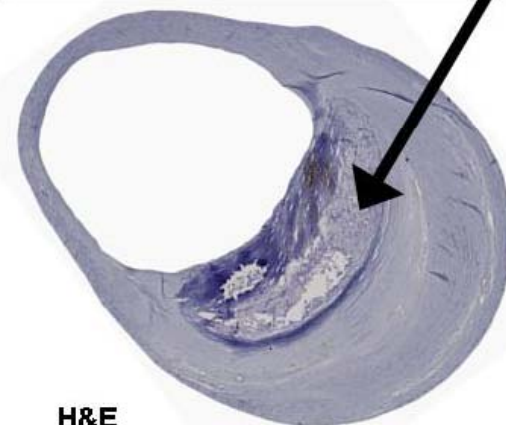
OCT Tissue Characterization

Optical Attenuation Imaging: *Ex-Vivo*

High attenuation is associated with markers of plaque vulnerability



Quantified optical attenuation in OCT image and correlated with tissue type in histology



H&E

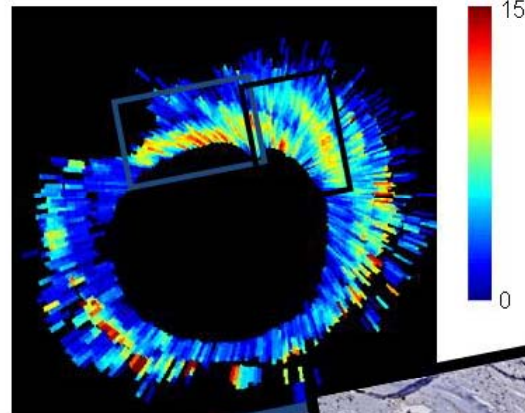
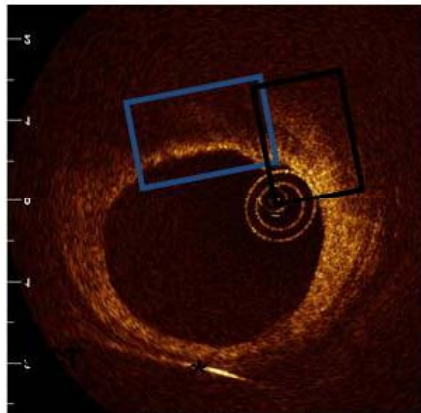
Necrotic Core

Fibrous	2 – 5 mm ⁻¹
Calcium	0 – 5 mm ⁻¹
Necrotic core	≥ 10 mm ⁻¹
Macrophages	> 12 mm ⁻¹

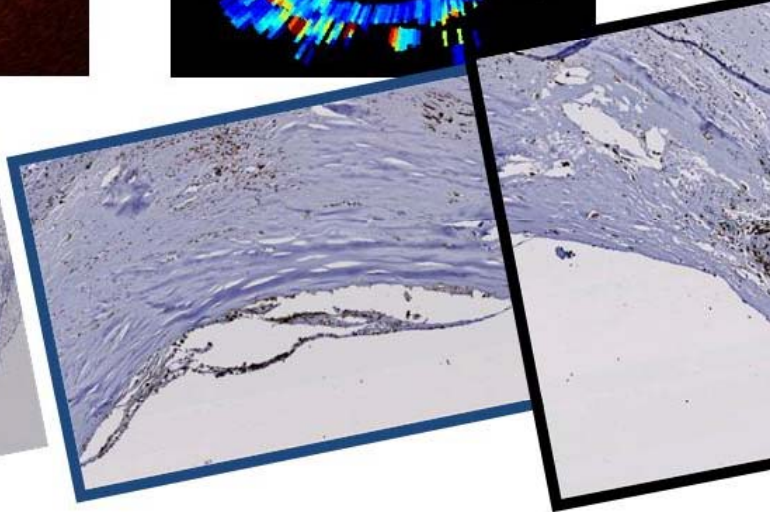
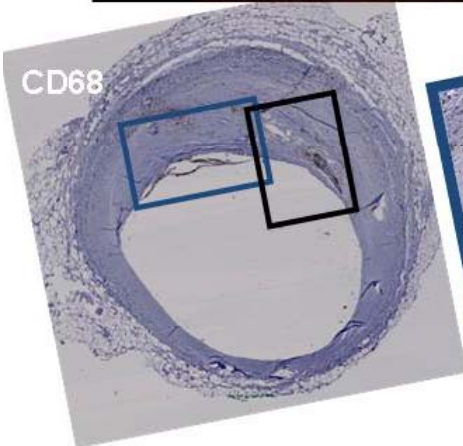
OCT Tissue Characterization

Optical Attenuation Imaging: *Ex-Vivo*

High attenuation is associated with markers of plaque vulnerability



Macrophages



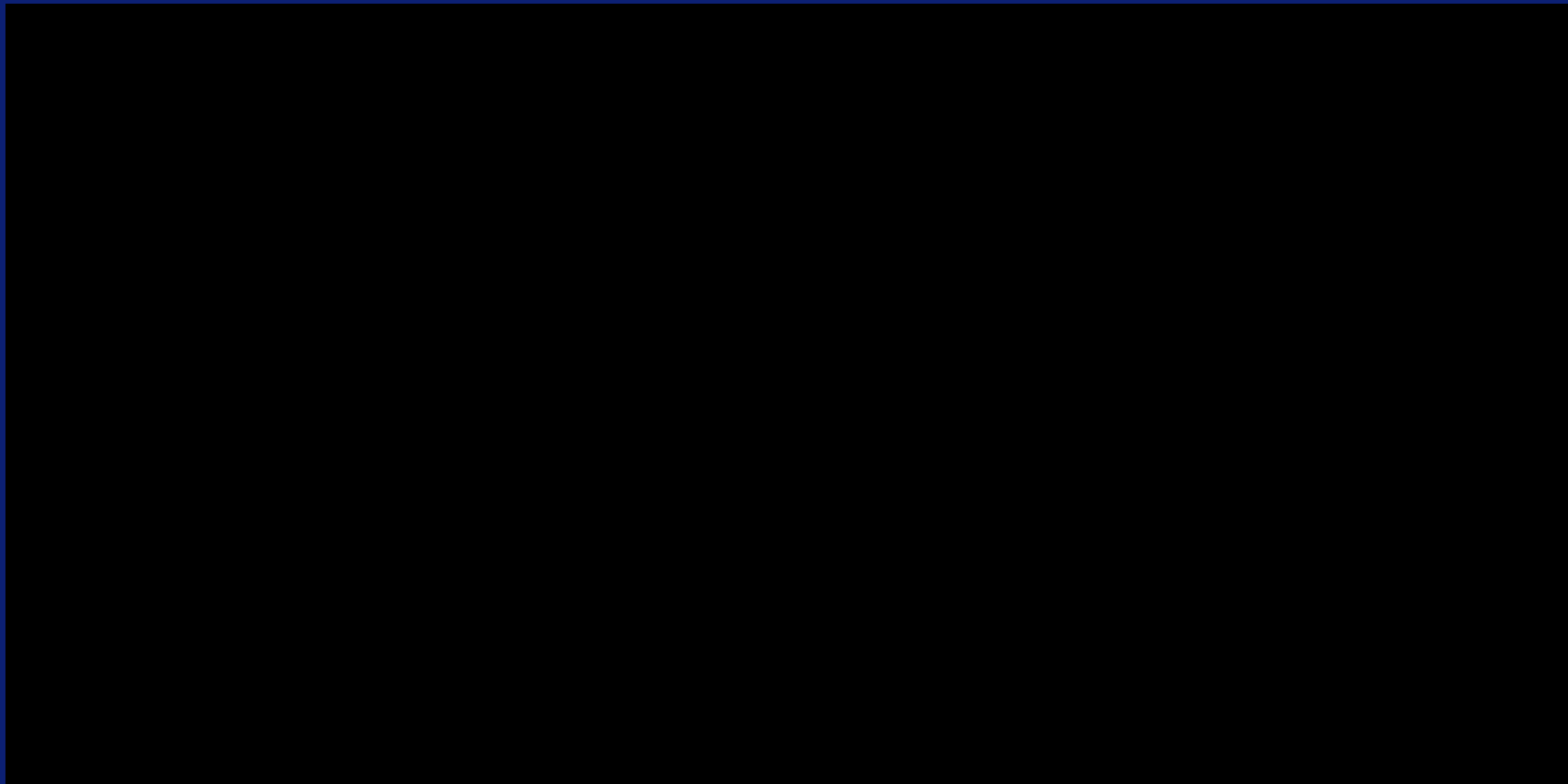
Fibrous	$2 - 5 \text{ mm}^{-1}$
Calcium	$0 - 5 \text{ mm}^{-1}$
Necrotic core	$\geq 10 \text{ mm}^{-1}$
Macrophages	$> 12 \text{ mm}^{-1}$

OCT Tissue Characterization

Optical Attenuation Imaging: *In-Vivo*

Erasmus MC

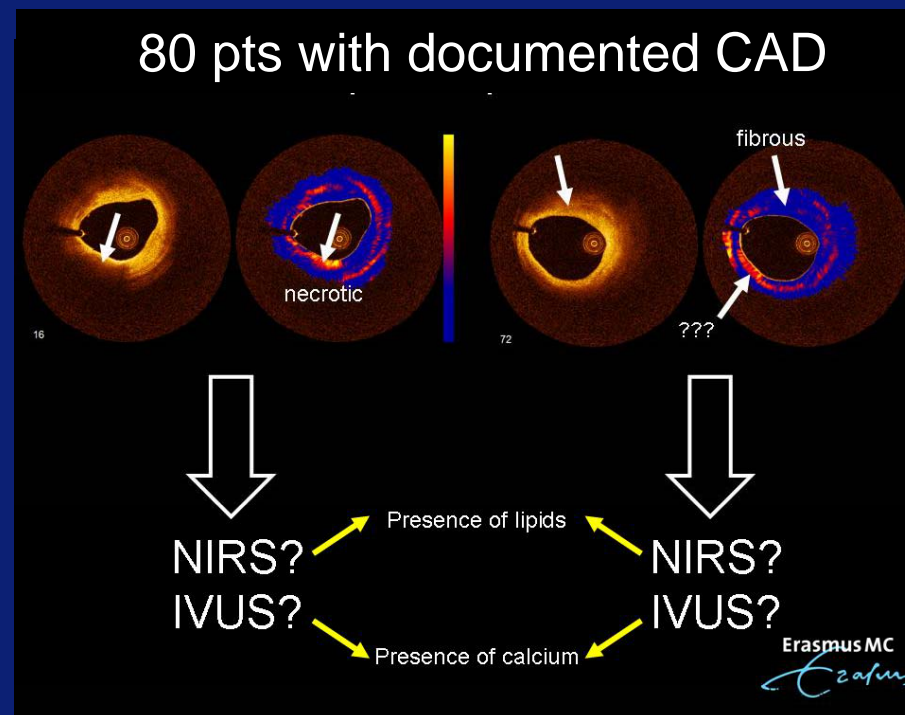
Erasmus



OCT tissue type Imaging Validation by Lipiscan-IVUS: OC3T Study

Objective: Validation of OCT-derived tissue optical properties in vivo

Design: Single-center, prospective, observational, cross-sectional





Vulnerable Plaque, Vulnerable Neointima

Technology

-Tissue characterization

IVUS VH

-Co- registration with the angiogram

NIRS

-3D rendering (real time)

OCT

Future Directions

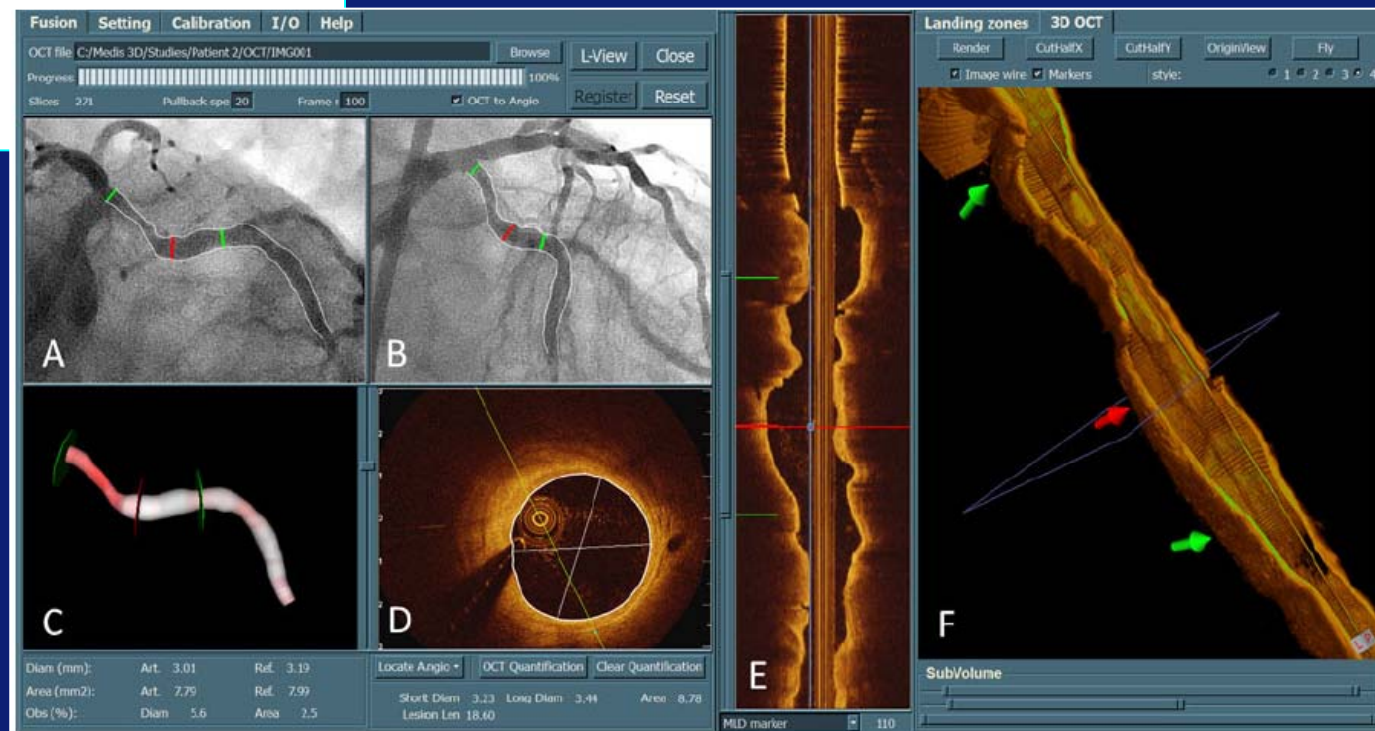
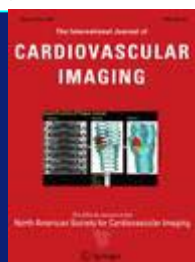
OCT – Angiography Co-Registration

Int J Cardiovasc Imaging
DOI 10.1007/s10554-012-0016-6

ORIGINAL PAPER

In vivo comparison of arterial lumen dimensions assessed by co-registered three-dimensional (3D) quantitative coronary angiography, intravascular ultrasound and optical coherence tomography

Shengxian Tu · Liang Xu · Jurgen Ligthart · Bo Xu · Karen Witberg · Zhongwei Sun · Gerhard Koning · Johan H. C. Reiber · Evelyn Regar



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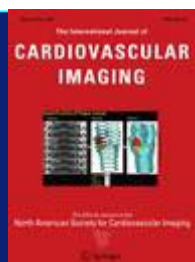


Table 3 Comparison between 3D QCA and OCT in assessing lumen size

	OCT	3D QCA	Difference (95% CI)	Intra-observer variability ^a	Inter-observer variability ^a
Positions, n = 541					
Short diameter (mm)	2.70 ± 0.65	2.57 ± 0.61	0.14(0.11–0.16) [†]	0.000 ± 0.013	0.003 ± 0.029
Long diameter (mm)	3.11 ± 0.72	2.80 ± 0.62	0.30 (0.27–0.33) [†]	0.003 ± 0.024	0.006 ± 0.035
Lumen area (mm ²)	7.01 ± 3.28	5.93 ± 2.66	1.07 (0.95–1.20) [†]	0.002 ± 0.039	0.021 ± 0.059
Vessels, n = 40					
Short diameter (mm)	2.71 ± 0.46	2.57 ± 0.43	0.14 (0.09–0.19) [†]	–	–
Long diameter (mm)	3.11 ± 0.52	2.81 ± 0.45	0.30 (0.24–0.37) [†]	–	–
Lumen area (mm ²)	7.02 ± 2.34	5.94 ± 1.91	1.08 (0.80–1.37) [†]	–	–

^a Observer variability was calculated from 165 positions from the first 10 vessels. *CI* Confidence interval; [†] *P* < 0.001

OCT – Angiography Co-Registration

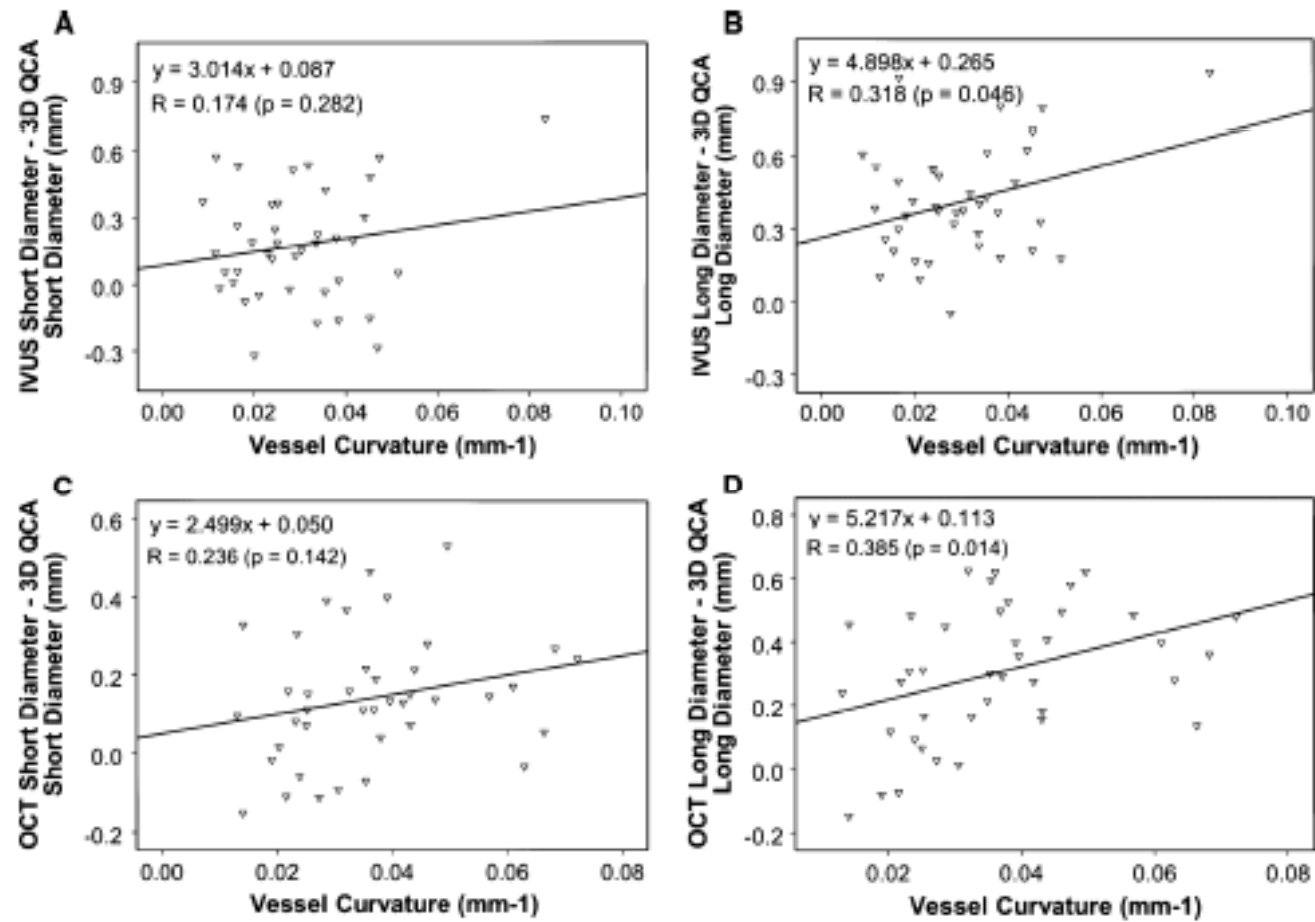
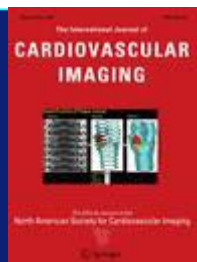


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Vulnerable Plaque, Vulnerable Neointima

Technology

-Tissue characterization

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-Co- registration with the angiogram

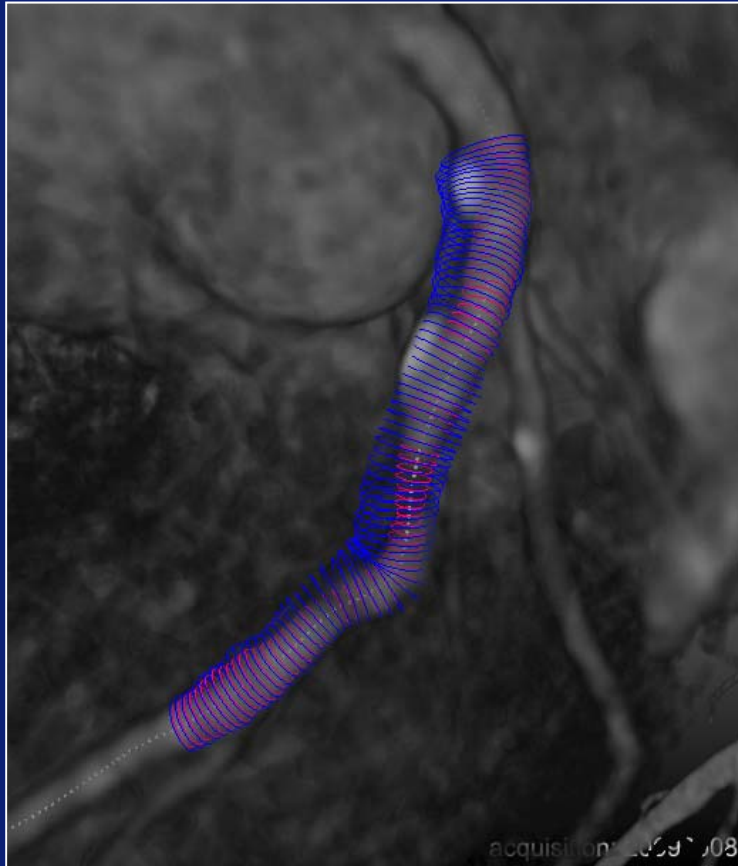
NIRS

-3D rendering (real time)

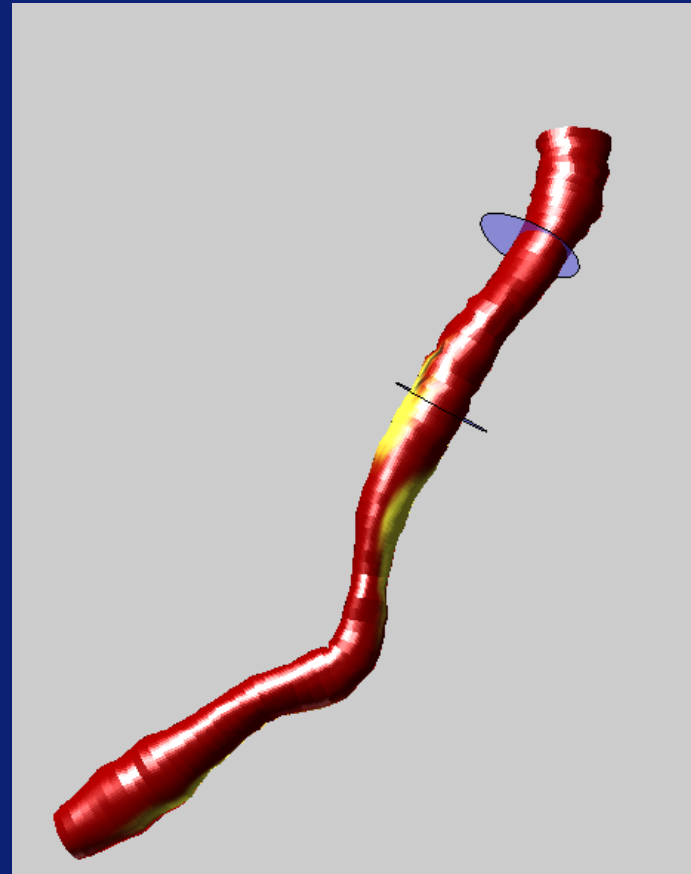
OCT

Future Directions

3D Representation of the Lipid Distribution in a Living Patient



Fusion of LipiScan -IVUS and MSCT

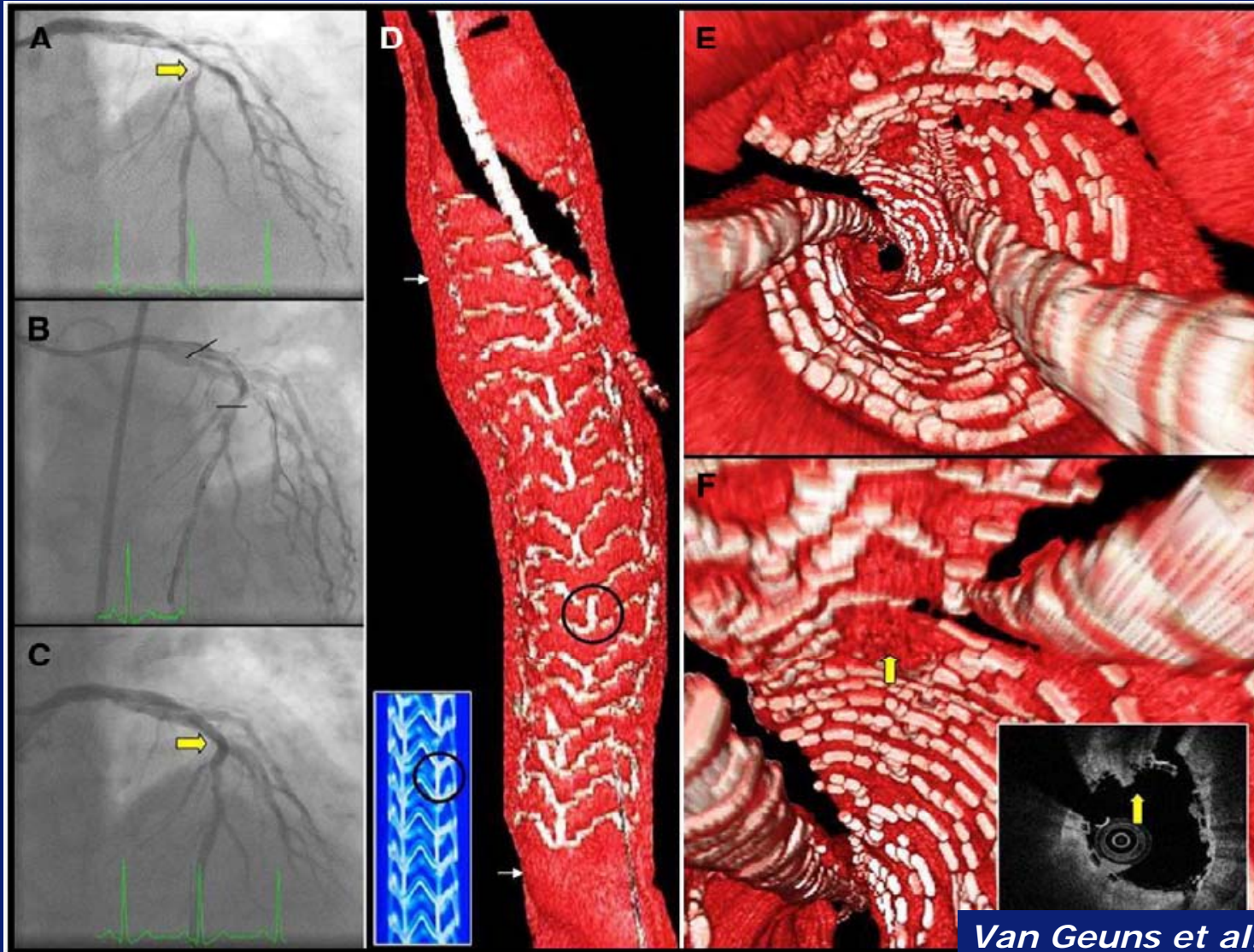


NIR in 3D

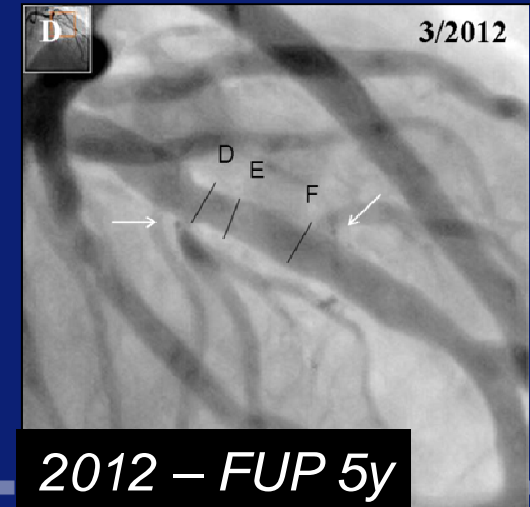
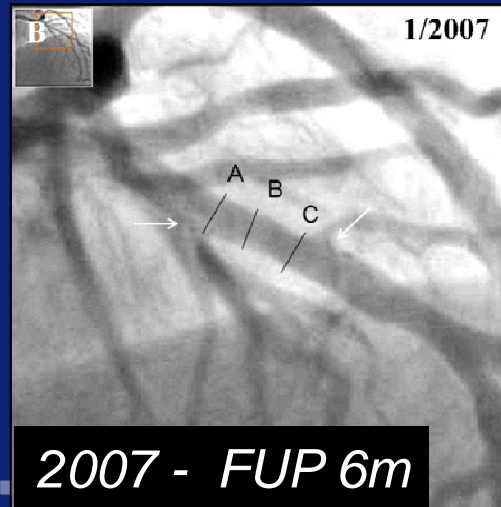
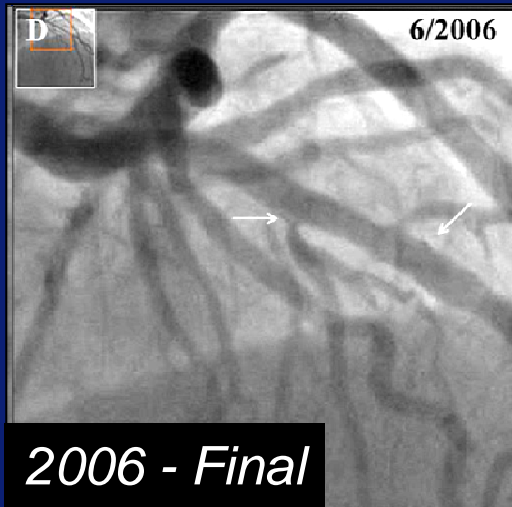
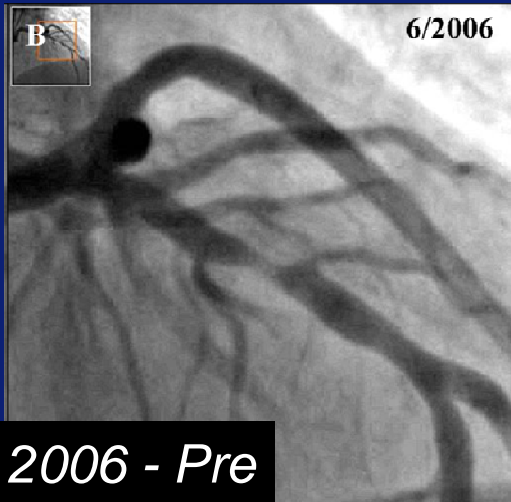
based on fusion of Lipiscan-IVUS and MSCT

Wentzel et al. Circulation, 2011.

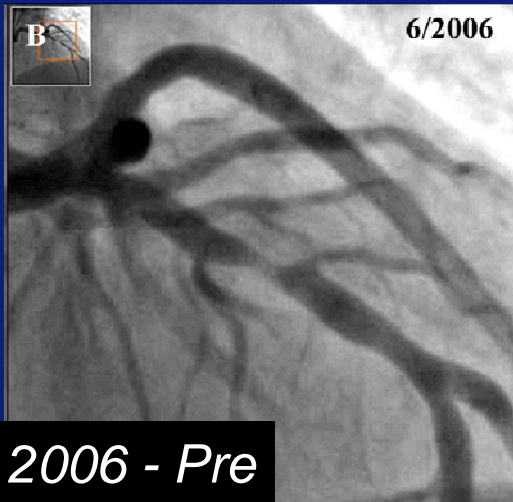
FD OCT- 3D Rendering Lesion Treated With BVS: Baseline



FD OCT- 3D Rendering BVS: 5Y FUP

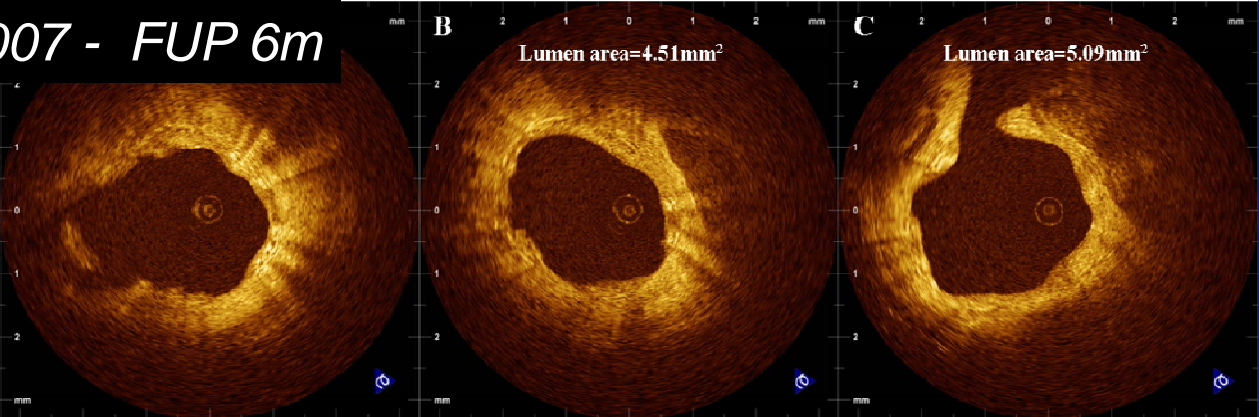


FD OCT- 3D Ren BVS: 5Y FUP



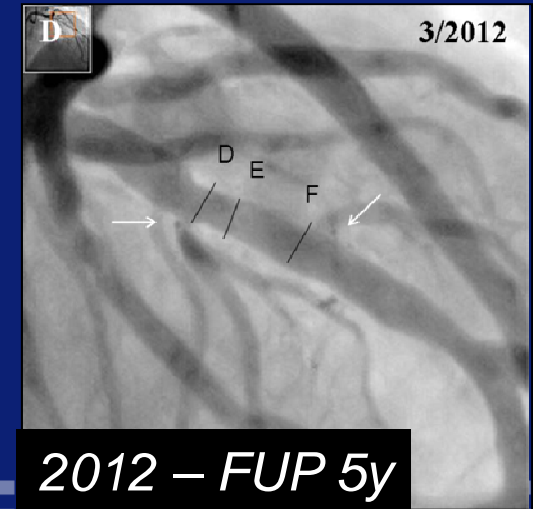
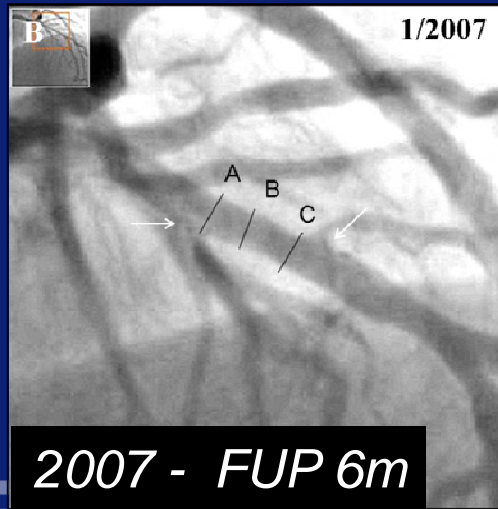
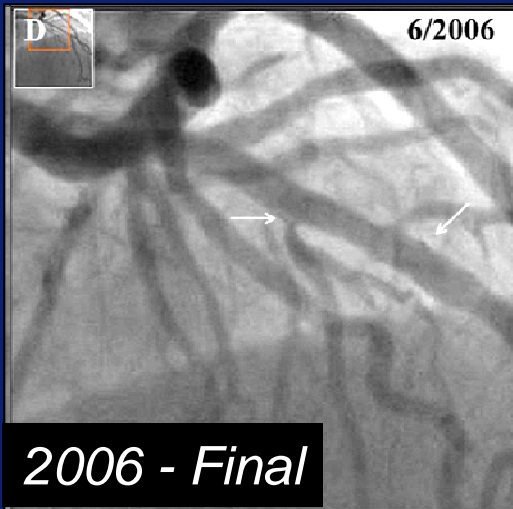
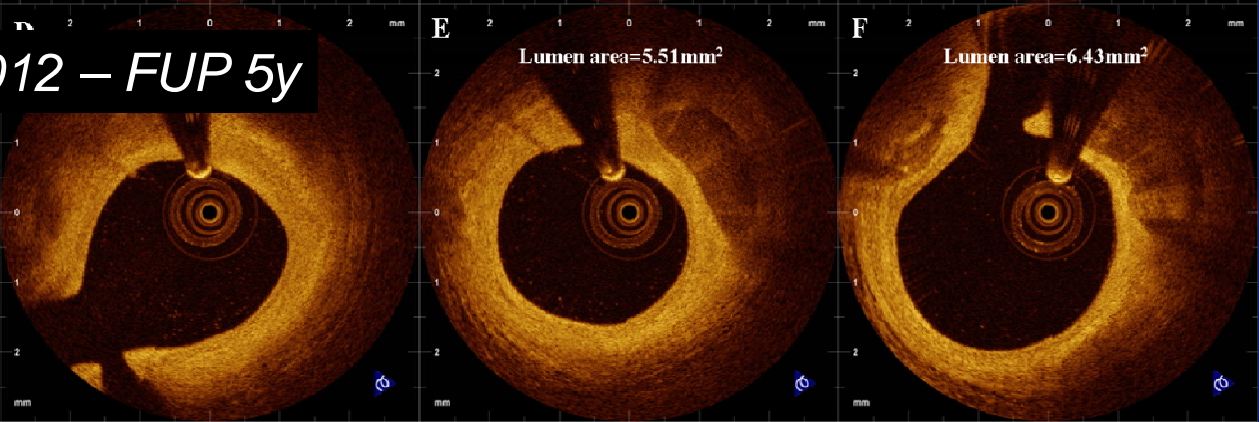
2007 - FUP 6m

6 months

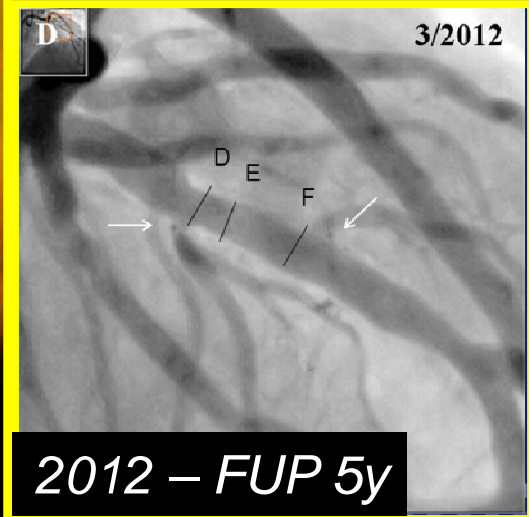
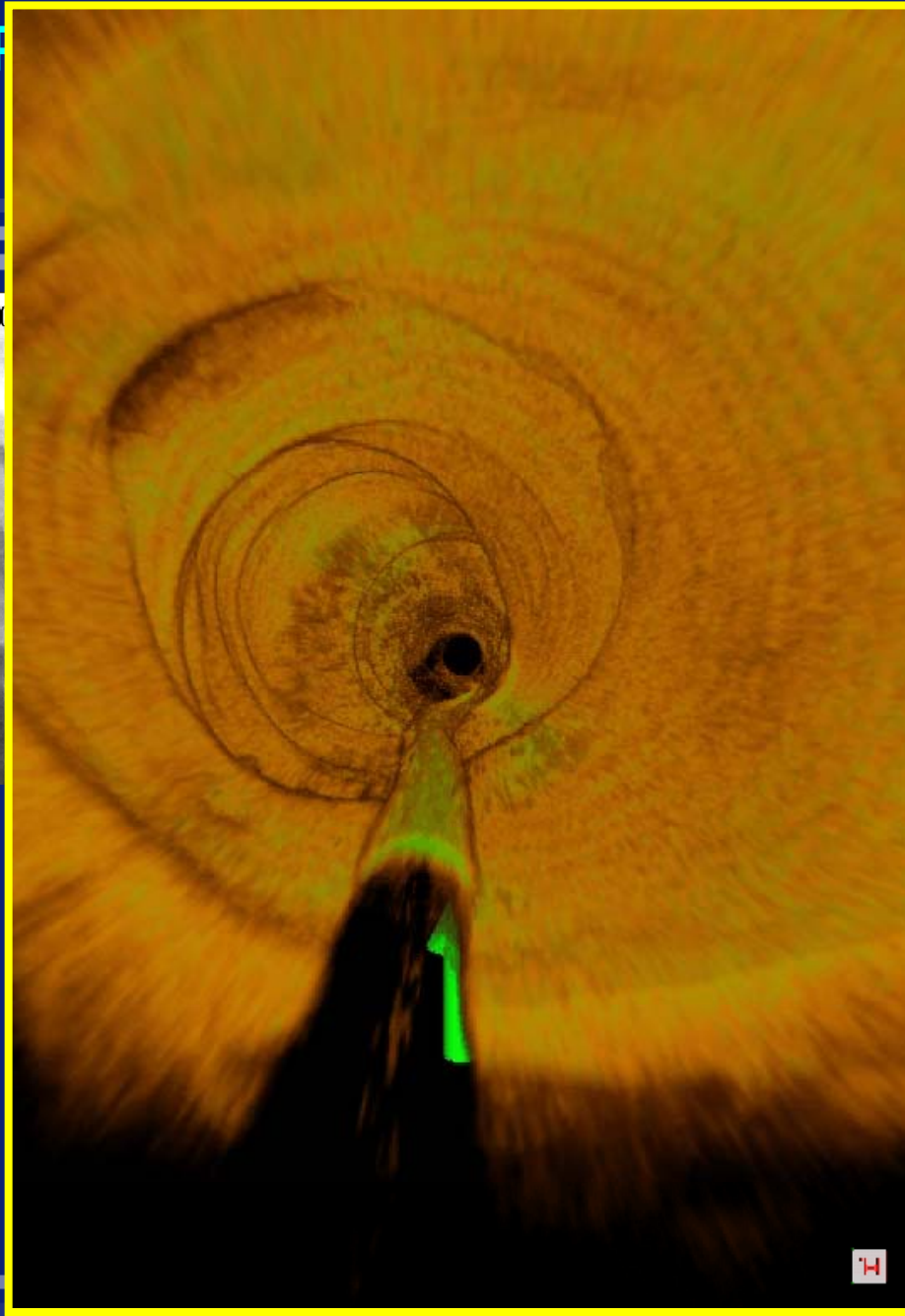


2012 - FUP 5y

5 years



FD OCT- 3D F BVS: 5Y FUP



Thank you for your attention!

PhD students interventional cardiology

A. Karanasos

N. van Ditzhuisen

M. Magro

Interventional Cardiology

R.J. van Geuns

C. Schultz

P. de Jaegere

J. Ligthart

N. van Mieghem

E. Duckers

P.W. Serruys

F. Zijlstra

Experimental Cardiology

H. van Beusekom

W. van der Giessen

Hemodynamics Laboratory

J. Wentzel

F. Gijsen

Bioengineering

G. van Soest

A.F.W. van der Steen

Imaging Group

N. Bruining

S. de Winter

K. Sihan