

A Reason Why Visual-Functional Mismatch Happens: Insights from Mathematical Models

Imaging & Physiology Summit 2015

Naritatsu Saito, MD

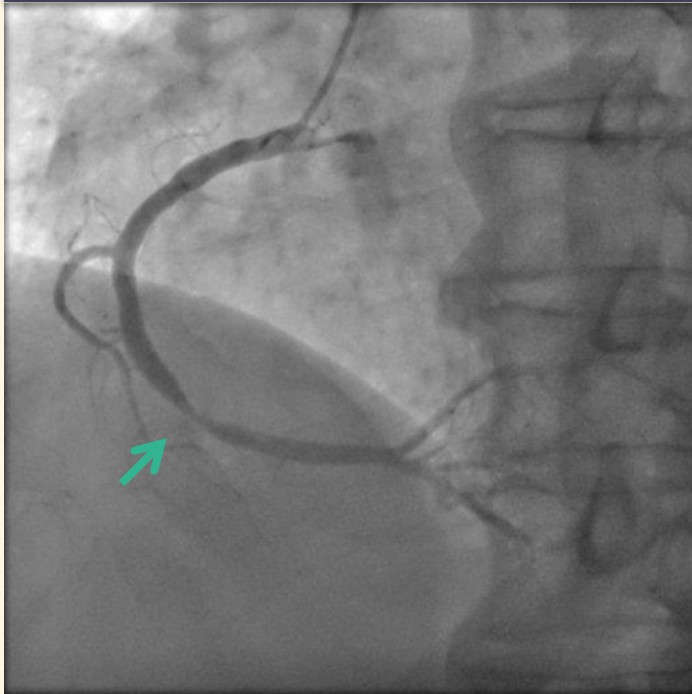
Department of Cardiology, Kyoto University, Japan

Imaging and Physiology Sometimes Do Not Agree

- Visual-Functional Mismatch
- Reverse Mismatch

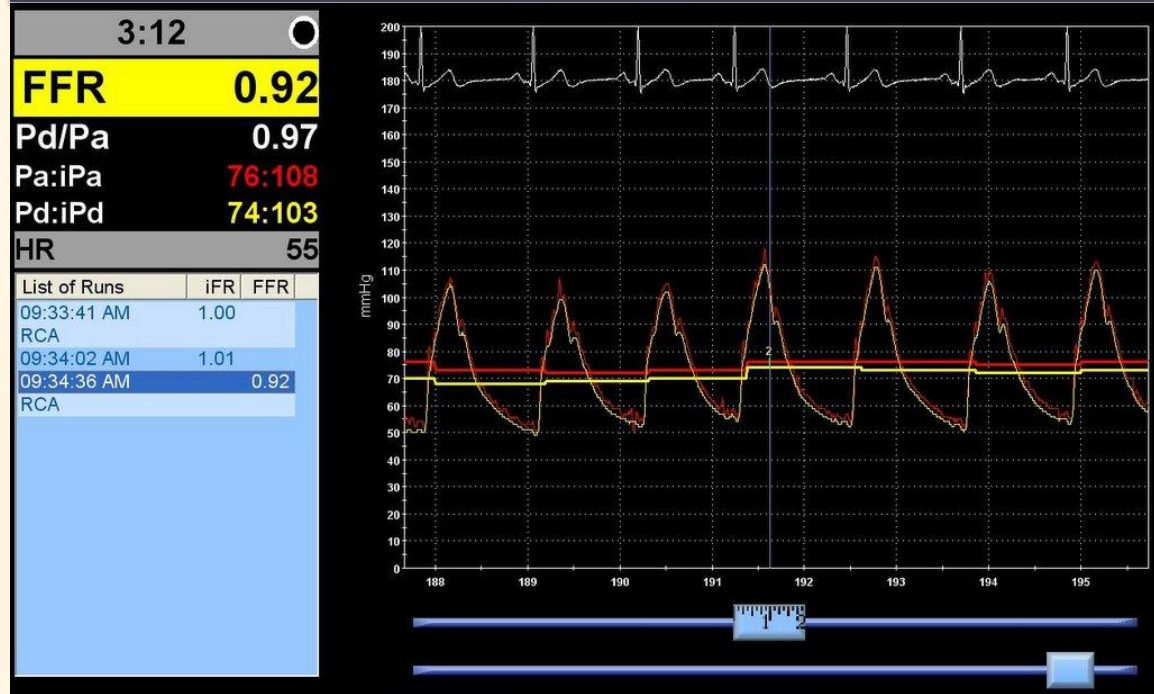
Visual-Functional Mismatch

Imaging



Visual Estimation: 90%

Physiology

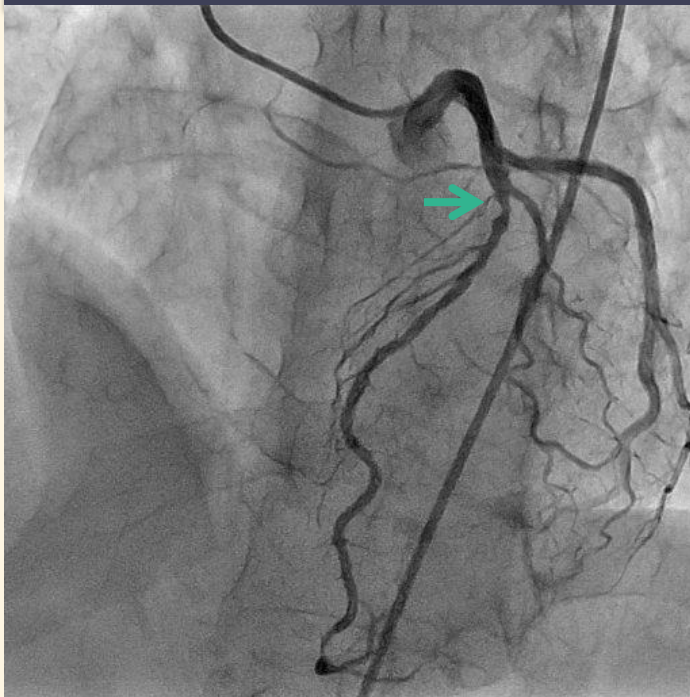


FFR: 0.92

Intervention was Deferred

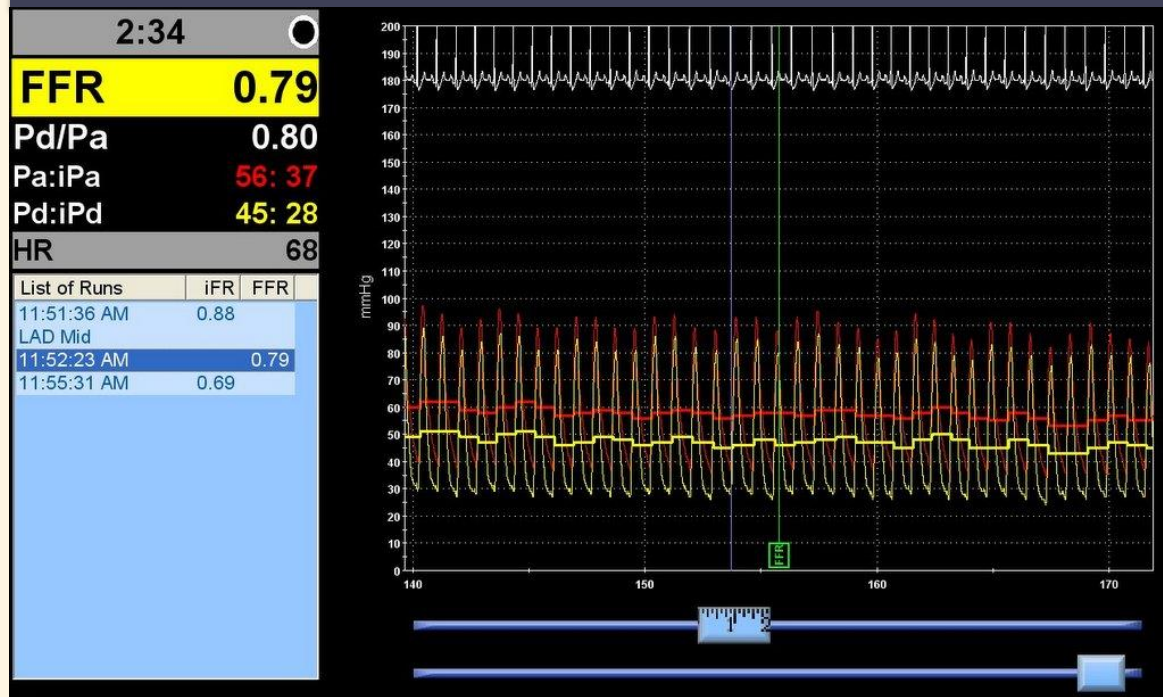
Reverse Mismatch

Imaging



Visual Estimation: 50%

Physiology



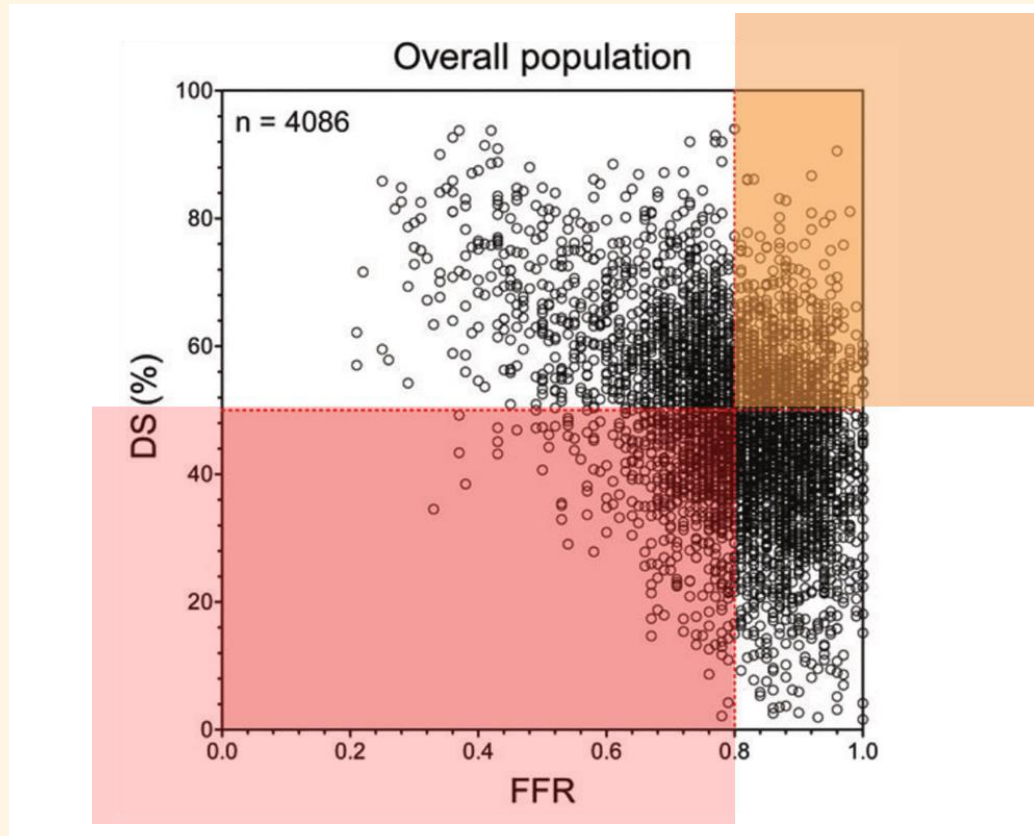
FFR: 0.79

Intervention was Conducted

Imaging and Physiology Sometimes Do Not Agree

- Mismatch
 - = Significant Stenosis, But Negative FFR
- Reverse Mismatch
 - = Insignificant Stenosis, But Positive FFR

Angiography-FFR Mismatch



Sensitivity: 0.61
Specificity: 0.67

Reverse Mismatch

Discordance Between Angiography and FFR = **35%**

IVUS and OCT

Meta-Analysis

15 Studies, 2,581 Patients and 2,807 Lesions

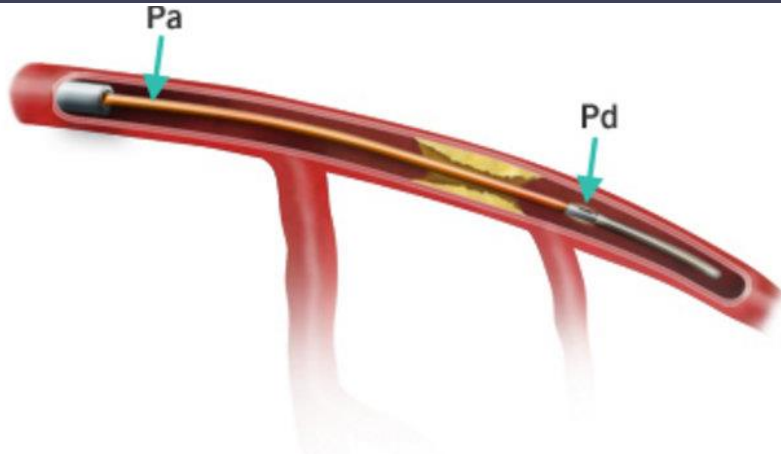
	OCT-MLA	IVUS-MLA
Pooled Sensitivity	0.81 [0.74-0.87]	0.68 [0.65-0.71]
Pooled Specificity	0.77 [0.71-0.83]	0.68 [0.66-0.70]

Despite improvement, IVUS and OCT do not predict functional stenosis, even with dedicated cutoff.

Why Mismatch Happen?

Going Back to the Original Definition of FFR_{myo}

Daily Practice: Pressure is Measured



$$FFR_{myo} = \frac{P_d - P_v}{P_a - P_v} \doteq \frac{P_d}{P_a}$$

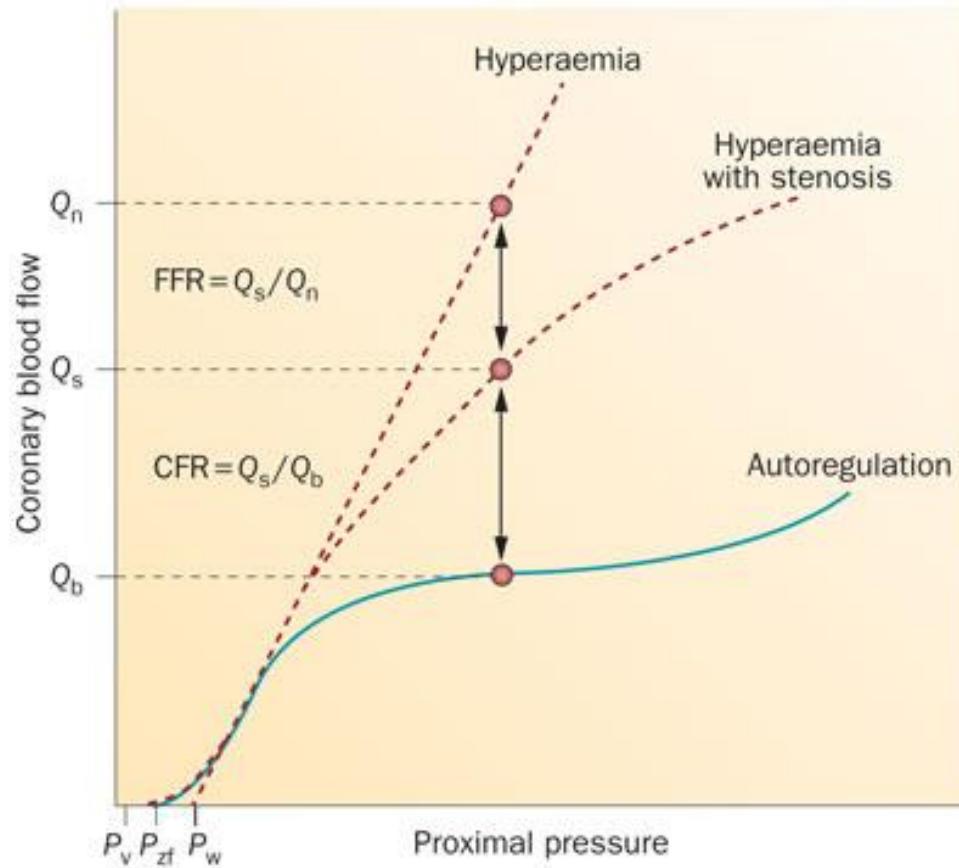
Pressure

Original Definition: Flow is Required

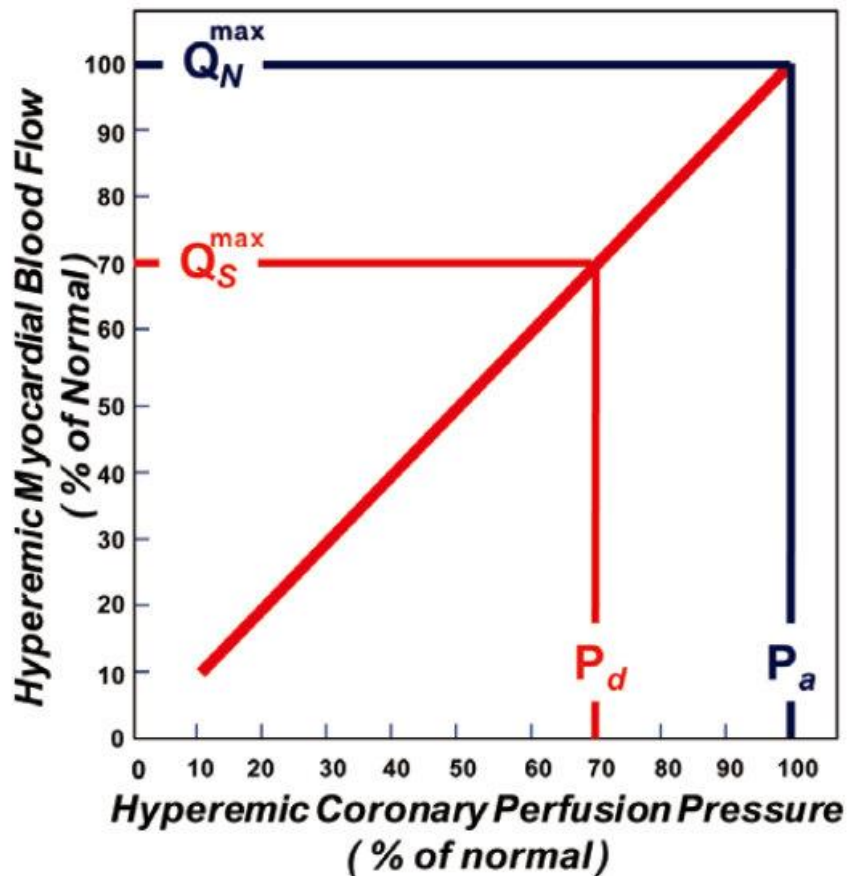
$$\begin{aligned} & FFR_{myo} \\ &= \frac{\text{maximum myocardial blood flow distal to an epicardial stenosis}}{\text{maximum myocardial blood flow if no epicardial stenosis present}} \\ &= \frac{Q}{Q^N} \end{aligned}$$

Flow

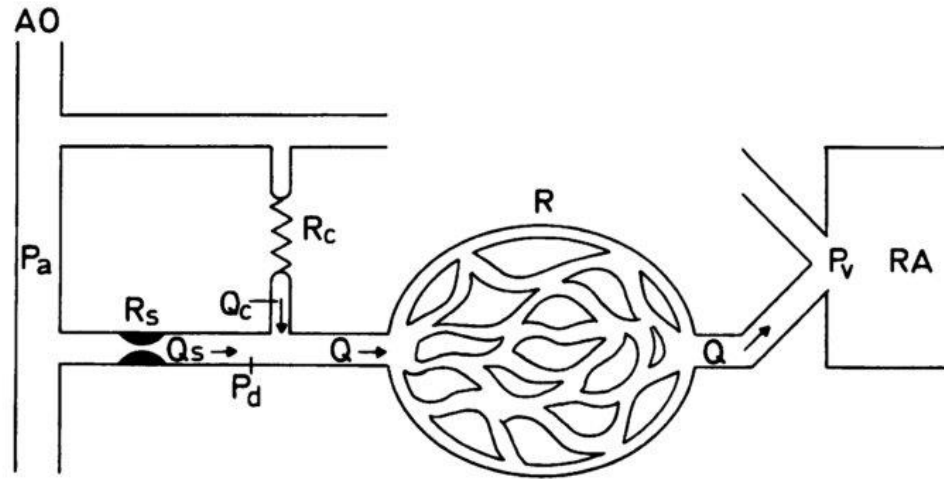
No Autoregulation@Hyperemia



Flow is Proportional to Pressure @Hyperemia

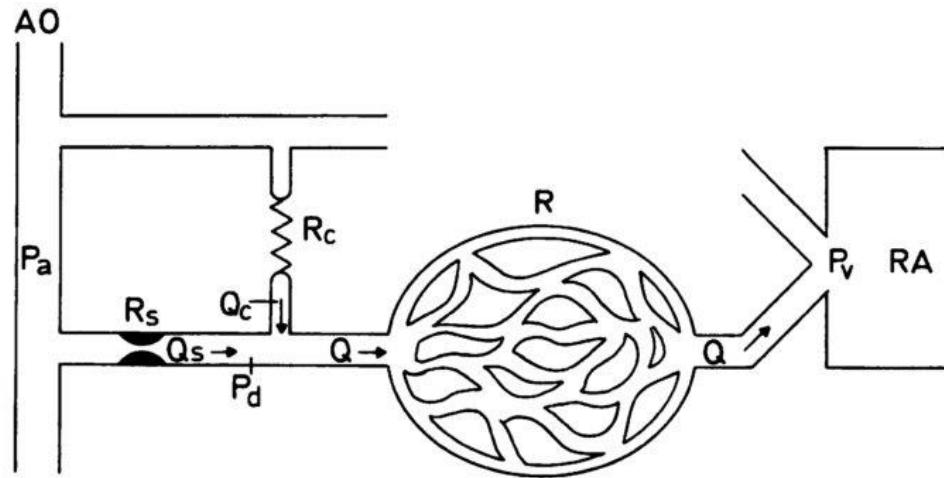


How Pressure is Converted to Flow: $P = Q \times R$



$$FFR_{myo} = \frac{Q}{Q^N} = \frac{\frac{P_d - P_v}{R}}{\frac{P_a - P_v}{R}} = \frac{P_d - P_v}{P_a - P_v} \doteq \frac{P_d}{P_a}$$

FFR_{myo}: Expressed in Terms of Resistance



$$FFR_{myo} = \frac{R(R_s + R_c)}{R_s R_c + R(R_s + R_c)}$$

FFR_{myo} expressed in terms of resistance clearly indicates that FFR_{myo} is determined not only by the stenosis (R_s), but also by the myocardial bed (R) and the collateral circulation (R_c).

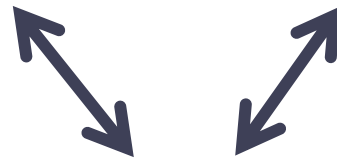
$$P = Q \times R$$

1. Flow

$$FFR_{myo} = \frac{Q}{Q_N} \quad (A)$$

2. Pressure

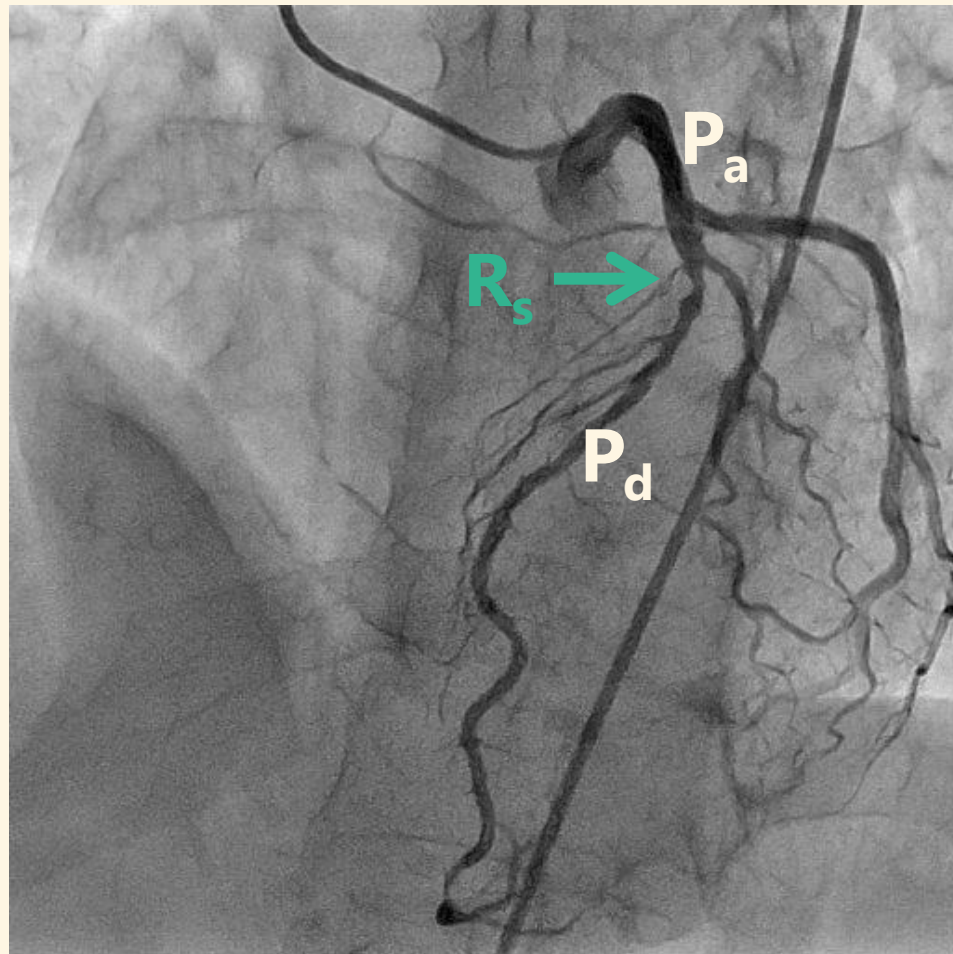
$$FFR_{myo} = \frac{P_d}{P_a} \quad (B)$$



$$FFR_{myo} = \frac{R(R_s + R_c)}{R_s R_c + R(R_s + R_c)} \quad (C)$$

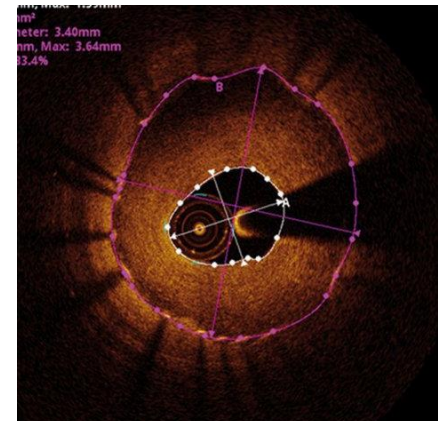
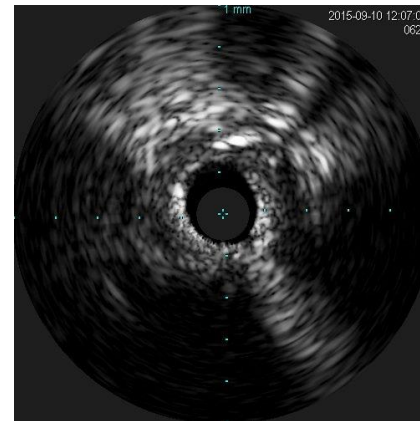
3. Resistance

QCA, IVUS, and OCT Analyze Only R_s



FFR: Pressure

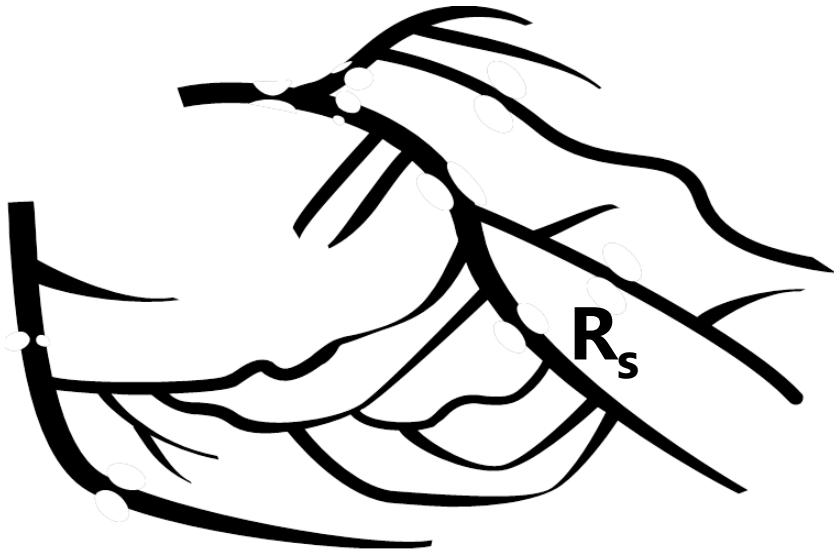
$$FFR_{myo} = \frac{P_d}{P_a}$$



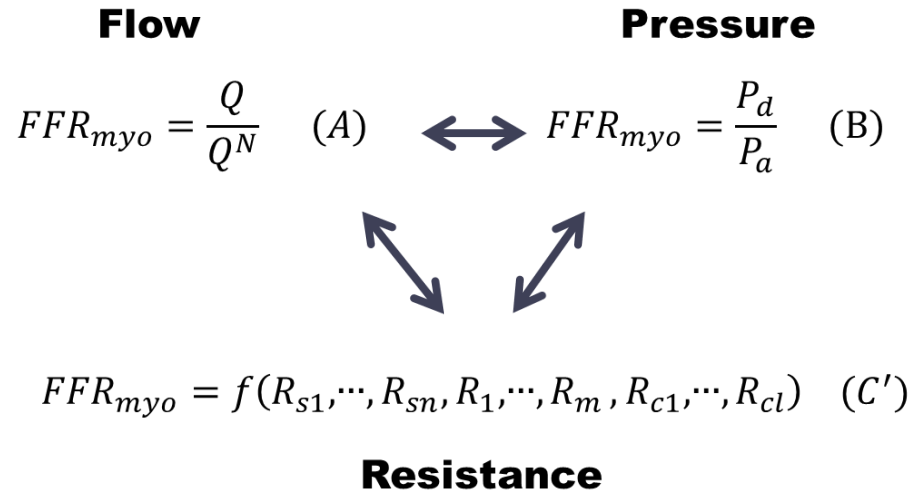
FFR: Resistance

$$FFR_{myo} = \frac{R(R_s + R_c)}{R_s R_c + R(R_s + R_c)}$$

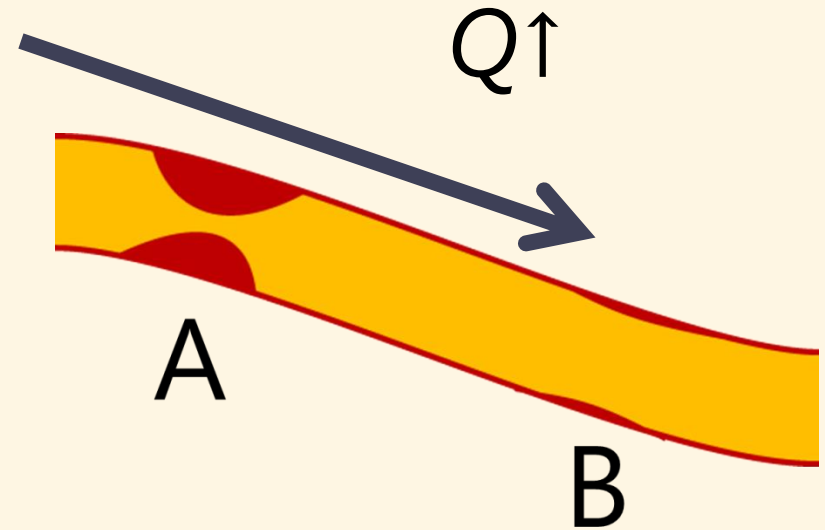
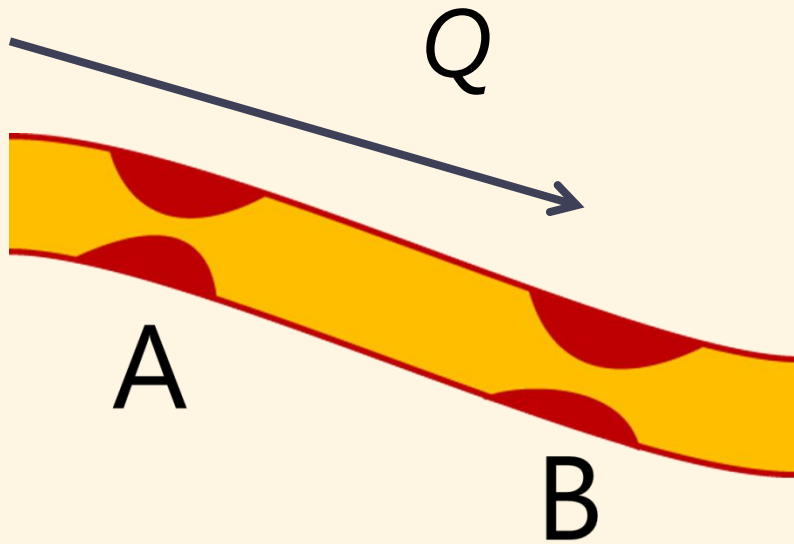
Complex Circulation Model



Epicardial Stenosis = $R_{s1}, R_{s2}, \dots, R_{sn}$
 Myocardial Vascular Bed = R_1, R_2, \dots, R_m
 Collateral Circulation = $R_{c1}, R_{c2}, \dots, R_{cl}$



Example 1. Tandem Lesion

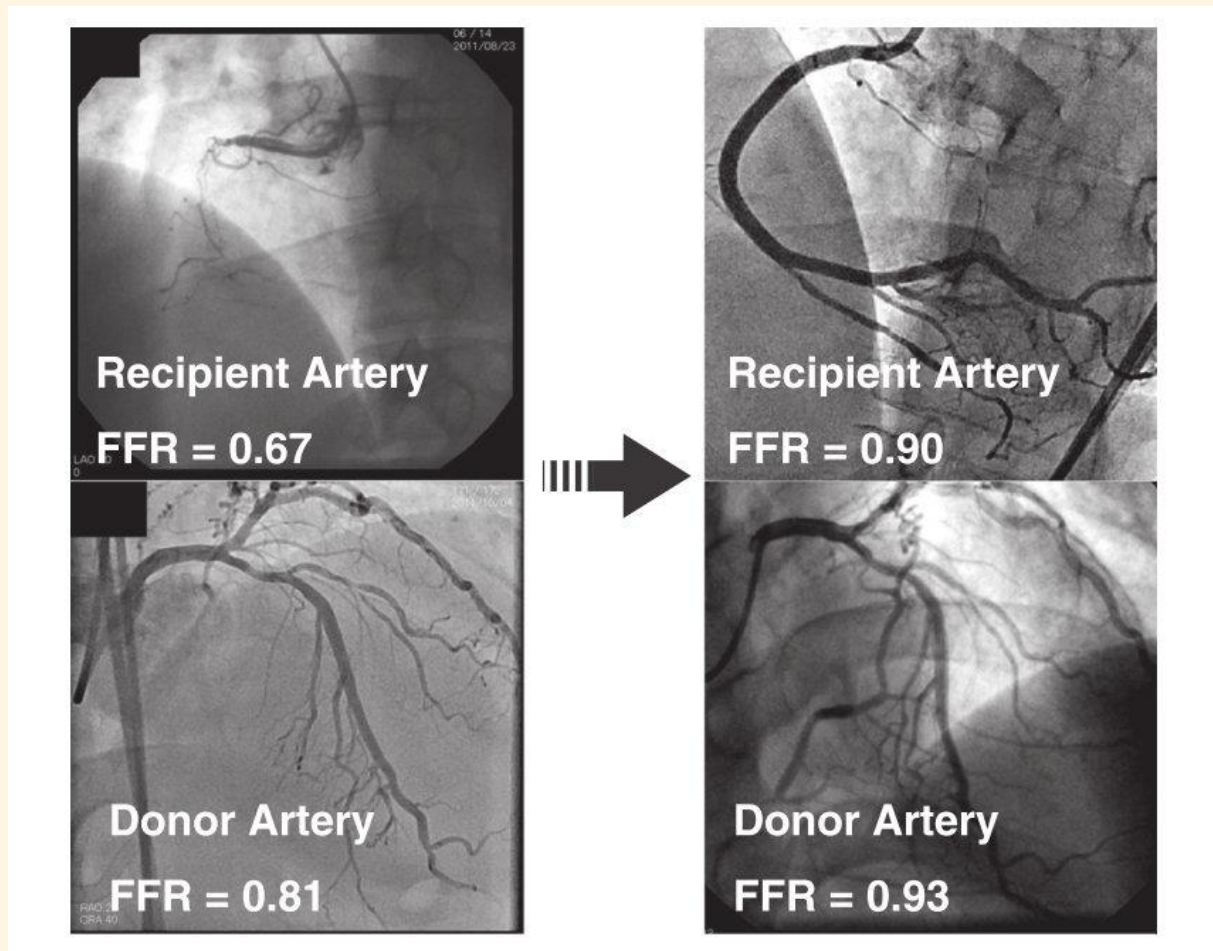


FFR(A) pre

\neq

FFR(A) post

Example 2. CTO Lesion



Example 3. Lesion Location



Pressure Drop Across a Stenosis

Darcy–Weisbach Equation

$$\Delta P = f \cdot \frac{L}{D} \cdot \frac{\rho V^2}{2}$$

Hagen-Poiseuille equation

$$\Delta P = \frac{128\mu L}{\pi D^4} \cdot Q$$

Pressure Drop Across a Stenosis

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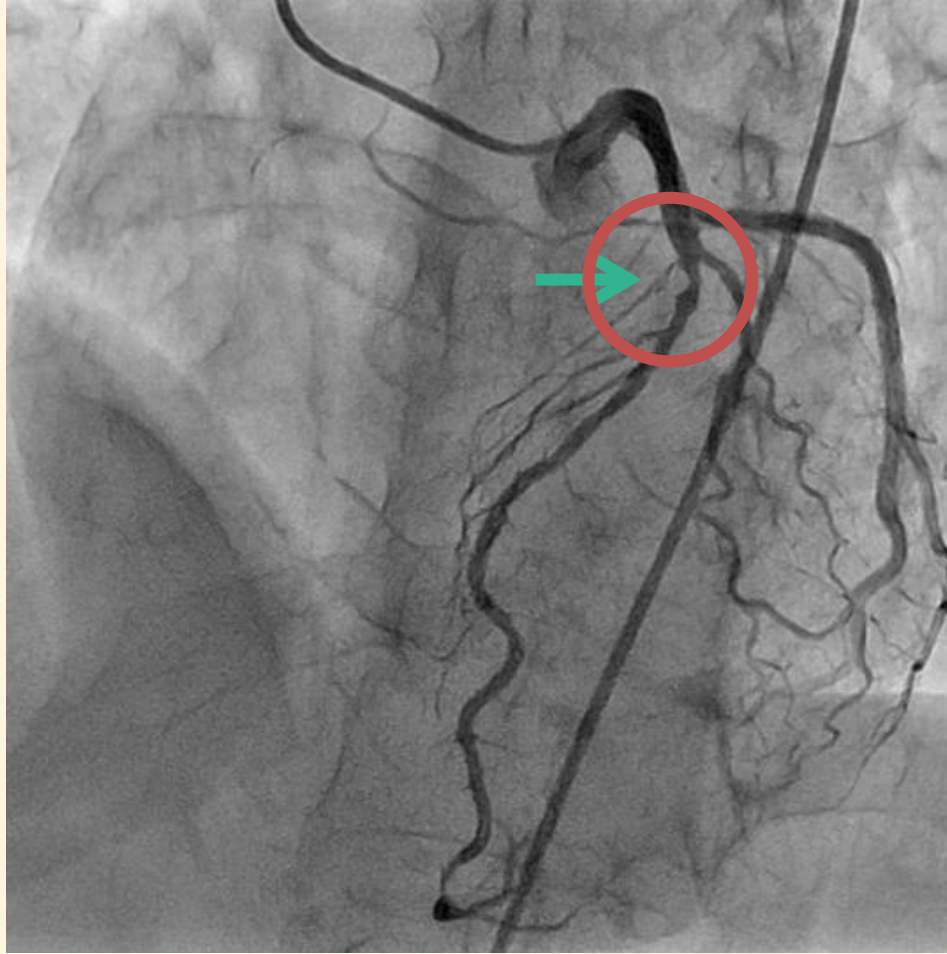
Pressure Drop Across a Stenosis

Darcy–Weisbach Equation

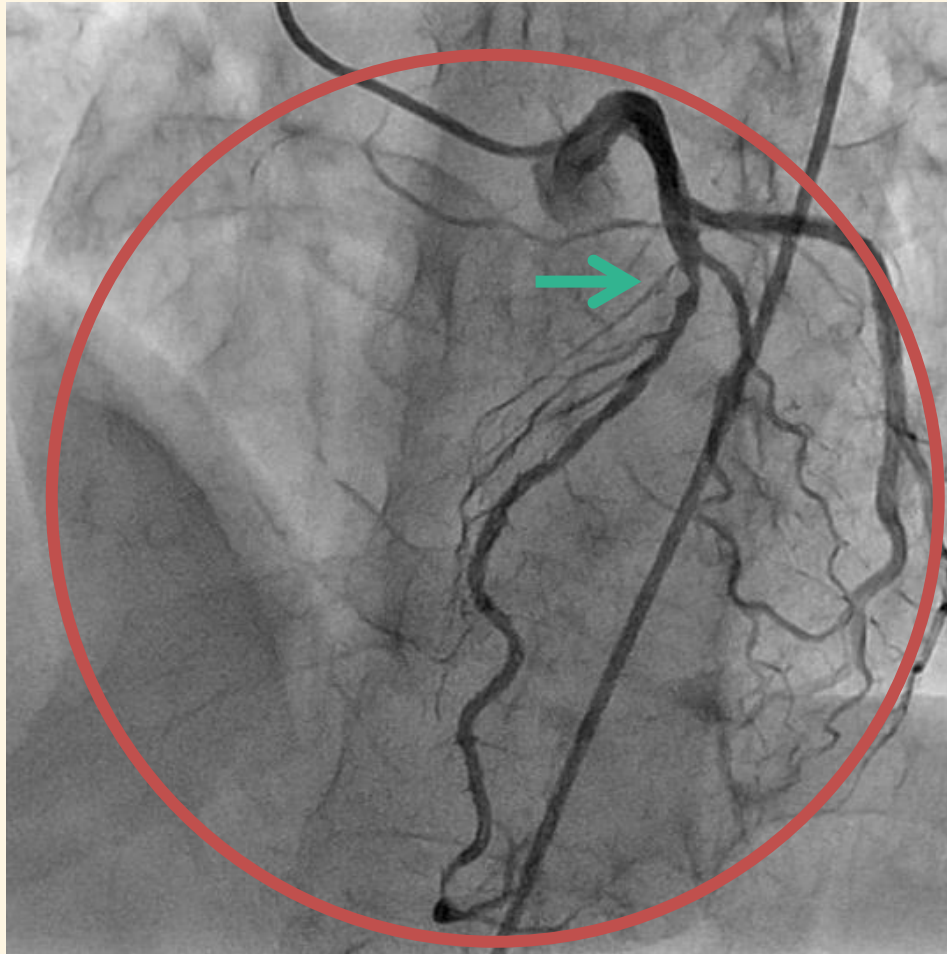
$$\Delta P = f \cdot \frac{L}{D} \cdot \frac{\rho V^2}{2}$$

Hagen-Poiseuille equation

$$\Delta P = \frac{128\mu L}{\pi D^4} \cdot Q$$



*You Have to Consider the Whole Circulation System,
If You Want to Know the FFR of Any Given Lesion.*



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Can't see the wood for the trees



Summary

- QCA, IVUS, and OCT assess only the target epicardial lesion, but FFR_{myo} is influenced by the other parts of the heart. This is very clear when FFR is expressed in terms of resistance:

$$FFR_{myo} = \frac{R(R_s + R_c)}{R_s R_c + R(R_s + R_c)}$$

- You need to see the whole circulation system, if you want to know the functional severity of any given stenosis.

Acknowledgement

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