

# **Future Perspective on Next BRS**

**Yoshinobu Onuma MD. PhD.<sup>1</sup>**

**Yohei Sotomi MD.<sup>2</sup>, Taku Asano, MD.<sup>2</sup>,**

**Erhan Tenecioglu, MD<sup>1</sup>, Yosuke Miyazaki, MD.<sup>1</sup>, Yuki Katagiri, MD<sup>2</sup>**

**Patrick W. Serruys MD. PhD.<sup>3</sup>**

**1. Erasmus University/ Cardialysis, Rotterdam, the Netherlands**

**2. Academisch Medisch Centrum, Amsterdam, the Netherlands**

**3. NHLI, Imperial College London, London, United Kingdom**

# Review

## Bioresorbable Scaffold The Emerging Reality and Future Directions

Yohei Sotomi, Yoshinobu Onuma, Carlos Collet, Erhan Tenekecioglu, Renu Virmani,  
Neal S. Kleiman, Patrick W. Serruys

***Abstract:*** In the era of drug-eluting stents, large-scale randomized trials and all-comer registries have shown excellent clinical results. However, even the latest-generation drug-eluting stent has not managed to address all the limitations of permanent metallic coronary stents, such as the risks of target lesion revascularization, neoatherosclerosis, preclusion of late lumen enlargement, and the lack of reactive vasomotion. Furthermore, the risk of very late stent, although substantially reduced with newer-generation drug-eluting stent, still remains. These problems were anticipated to be solved with the advent of fully biodegradable devices. Fully bioresorbable coronary scaffolds have been designed to function transiently to prevent acute recoil, but have retained the capability to inhibit neointimal proliferation by eluting immunosuppressive drugs. Nevertheless, long-term follow-up data of the leading bioresorbable scaffold (Absorb) are becoming available and have raised a concern about the relatively higher incidence of scaffold thrombosis. To reduce the rate of clinical events, improvements in the device, as well as implantation procedure, are being evaluated. This review will focus on the current CE-mark approved bioresorbable scaffolds, their basic characteristics, and clinical results. In addition, we summarize the current limitations of bioresorbable scaffold and their possible solutions. (*Circ Res.* 2017;120:1341-1352. DOI: 10.1161/CIRCRESAHA.117.310275.)

**Key Words:** bioresorbable scaffold ■ magnesium ■ polymers ■ thrombosis

# Mechanical properties of metal vs. PLLA

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<b>Composition</b>	<b>Tensile modulus of elasticity (Gpa)</b>	<b>Tensile strength (Mpa)</b>	<b>Elongation at break (%)</b>	<b>Degradation time (months)</b>	<b>Products</b>
Poly (L-lactide)	3.1-3.7	60-70	2-6	>24	Absorb (platform), DESolve (platform), Magmaris (coating)
Poly (DL-lactide)	3.1-3.7	45-55	2-6	6-12	Absorb (coating)
Magnesium alloy	40-45	220-330	2-20	1-3	Magmaris (platform)
Cobalt chromium	210-235	1449	~40	Biostable	Xience

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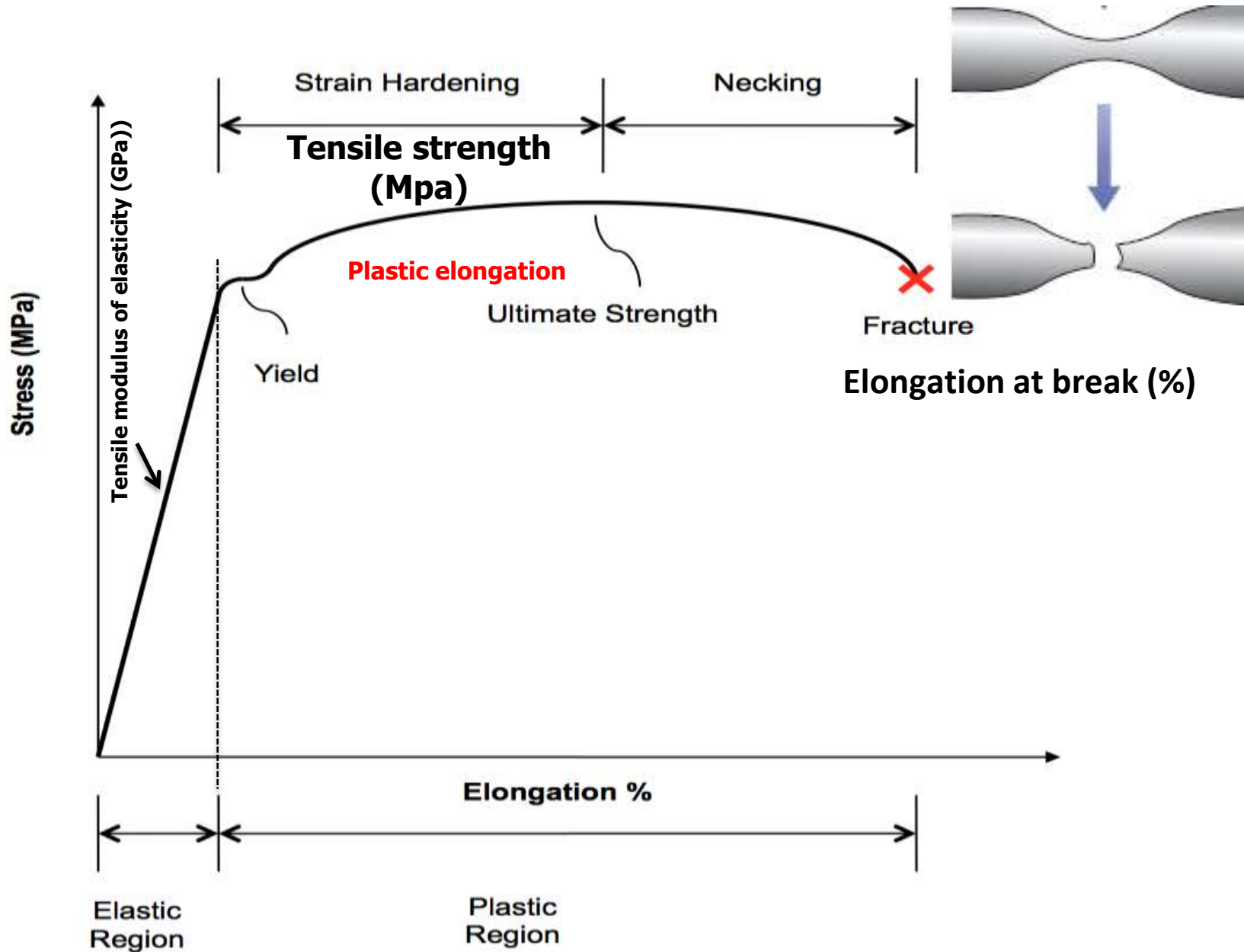
# Current limitation of BRS

If a bioresorbable scaffold is ultimately expected to have the same range of applicability as a durable metal stent, **the gap in mechanical properties** must be reduced.

Currently, three primary limitations exist:

- **Low tensile strength and stiffness** which require thick struts to prevent acute recoil
- **Insufficient ductility** which impacts scaffold retention on balloon catheter and limits the range of scaffold expansion during deployment
- **Instability of mechanical properties** during vessel remodeling if bioresorption is too fast

# Let's take a "crash course" of material science



## Bioresorption process of current CE-mark approved BRSs

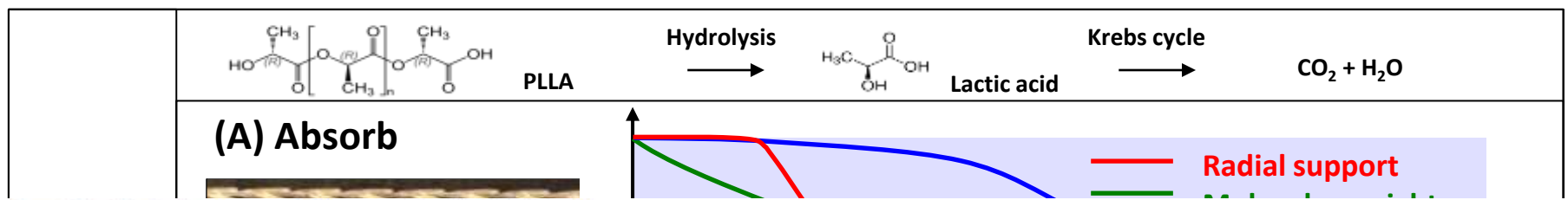
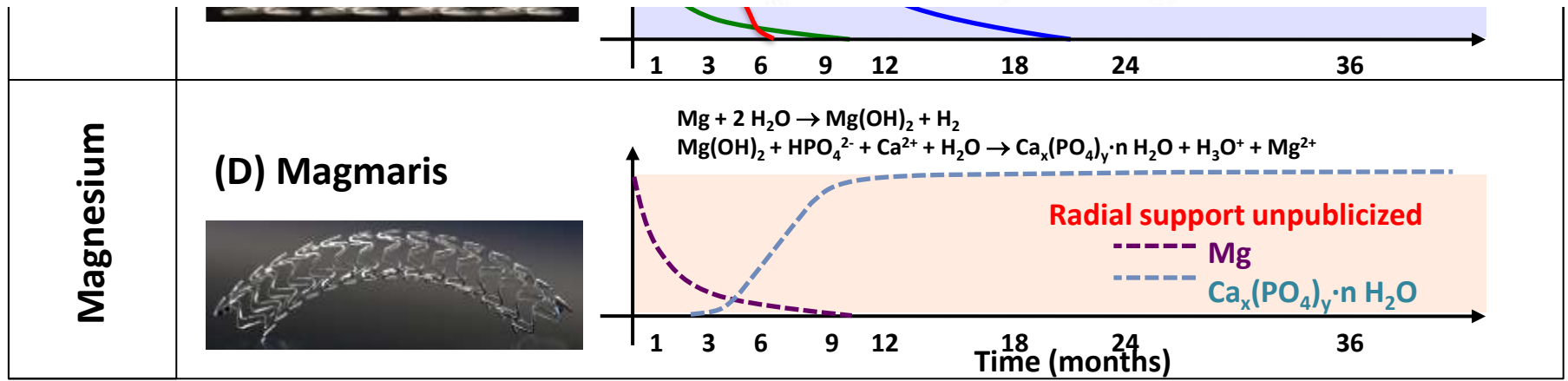


Table 1. CE-Mark Approved Bioresorbable Scaffolds

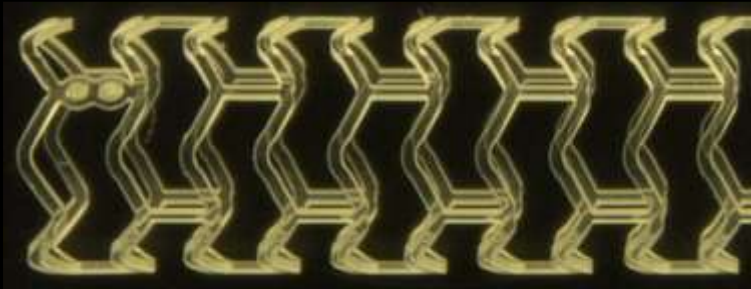
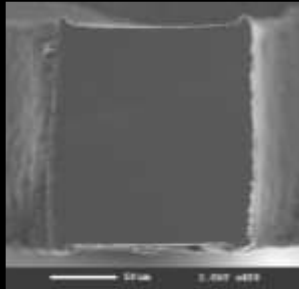
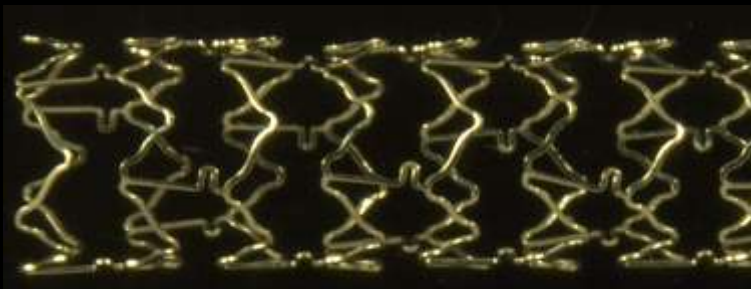

Stent Name (Manufacturer)	Stent Platform	Strut Thickness	Coating Material	Coating Thickness	Drug	Reported Release Profile	Drug Dose
BVS 1.1 (Abbott)	PLLA	157 $\mu\text{m}$	PLLA	2–4 $\mu\text{m}$	Everolimus	75% of loaded everolimus within 30 days	100 $\mu\text{g}/\text{cm}^2$
DESolve (Elixir)	PLLA	150 $\mu\text{m}$	Bioresorbable polymer	<3 $\mu\text{m}$	Novolimus	More than 85% of the drug is released over 4 wk	5 $\mu\text{g}/\text{mm}$
ART Pure (ART)	PDLLA	170 $\mu\text{m}$	...	...	No drug	NA	NA
Magmaris (Biotronik)	93% Mg and 7% rare earth elements	150 $\mu\text{m}$	PLLA	1 $\mu\text{m}$	Sirolimus	Over 3 to 6 mo	1.4 $\mu\text{g}/\text{mm}^2$

BVS indicates bioresorbable vascular scaffold; NA, data not available; PDLLA, poly(L-lactide-co-D,L-lactide); and PLLA, poly-L-lactide.





# Design of Absorb and Xience

	Macroscopic appearance	Material	Cross-section	Strut thickness
<b>Absorb scaffold</b>		PLLA + PDLLA		157 $\mu\text{m}$
<b>Xience V</b>		Co-Cr + durable fluoropolymer		89 $\mu\text{m}$

**Covered vessel wall area (footprint [3.0mm device]):  
26% (Absorb scaffold) vs. 12% (Xience V)**

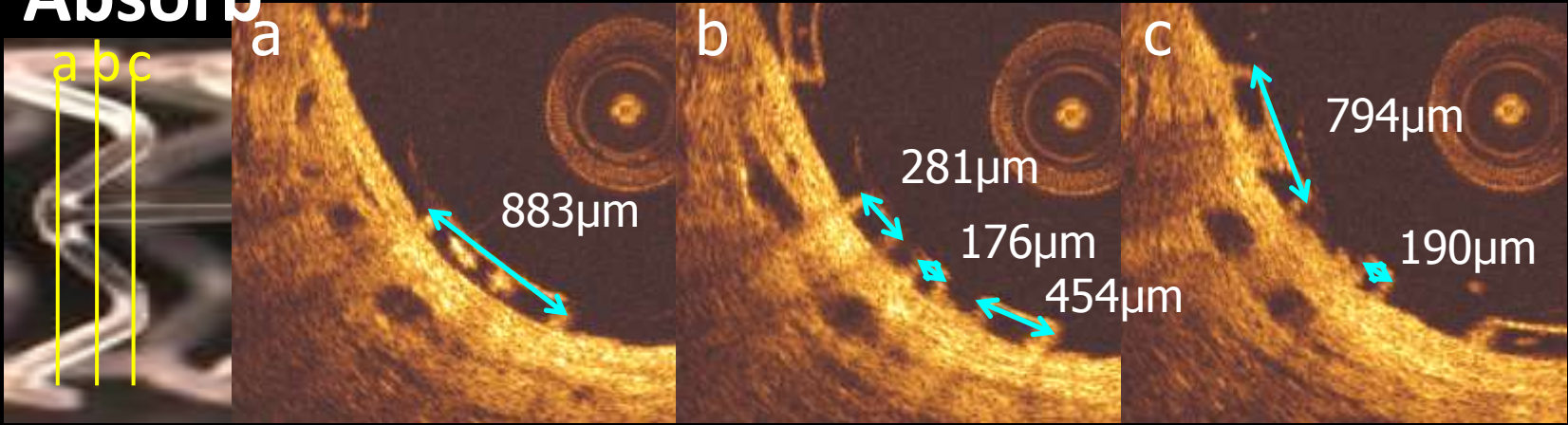
# Snowshoe Versus Ice Skate for Scaffolding of Disrupted Vessel Wall\*



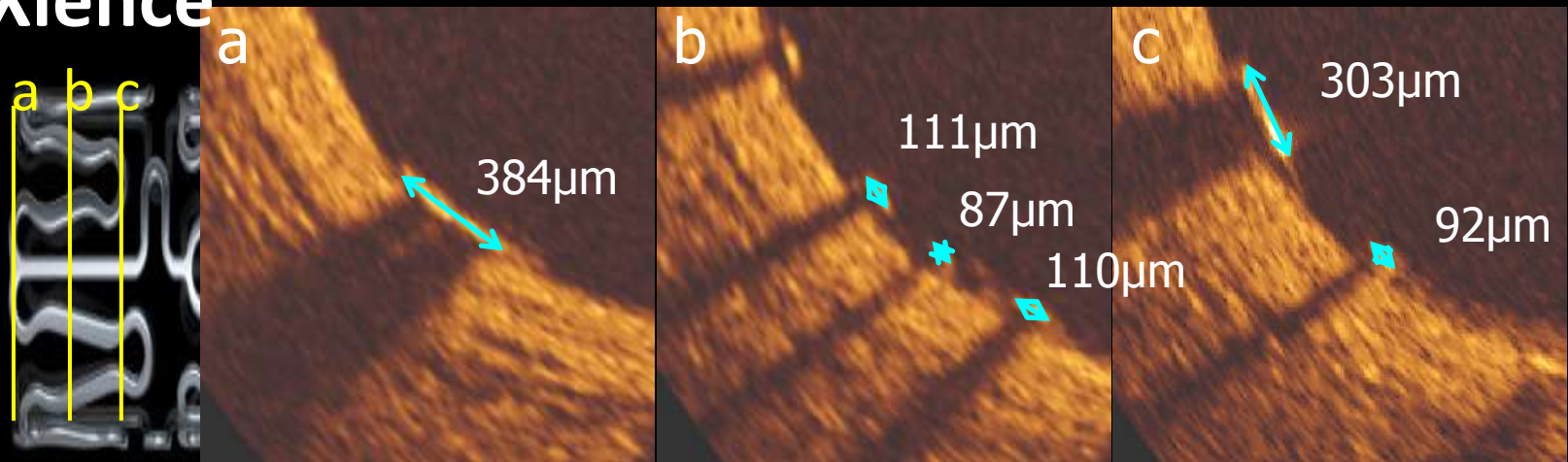
Patrick W. Serruys, MD, PhD,<sup>†</sup> Pannipa Suwannasom, MD,<sup>‡</sup> Shimpei Nakatani, MD,<sup>‡</sup> Yoshinobu Onuma, MD, PhD<sup>‡</sup>

## Difference of Strut Width in each part (Hinge, Link, Ring)

### Absorb



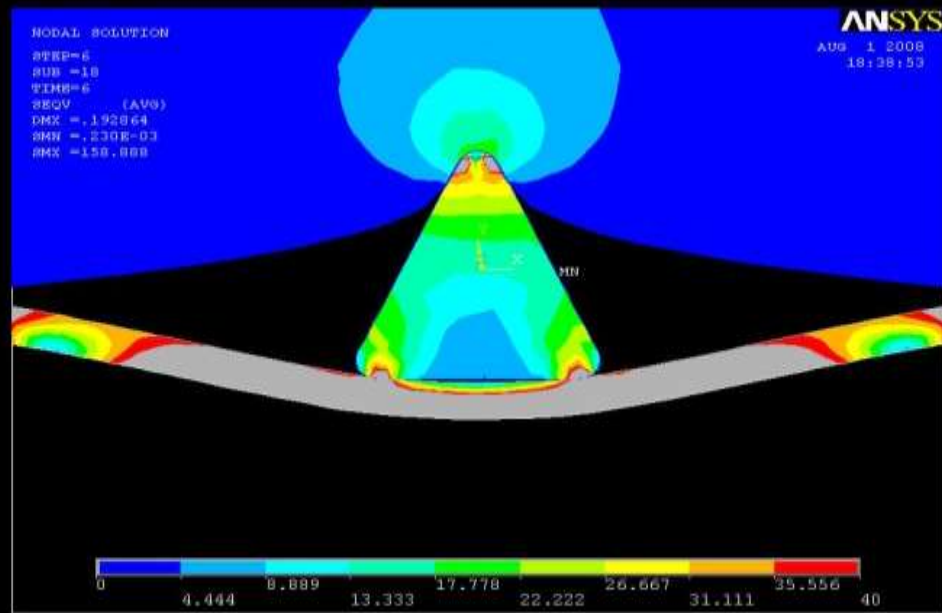
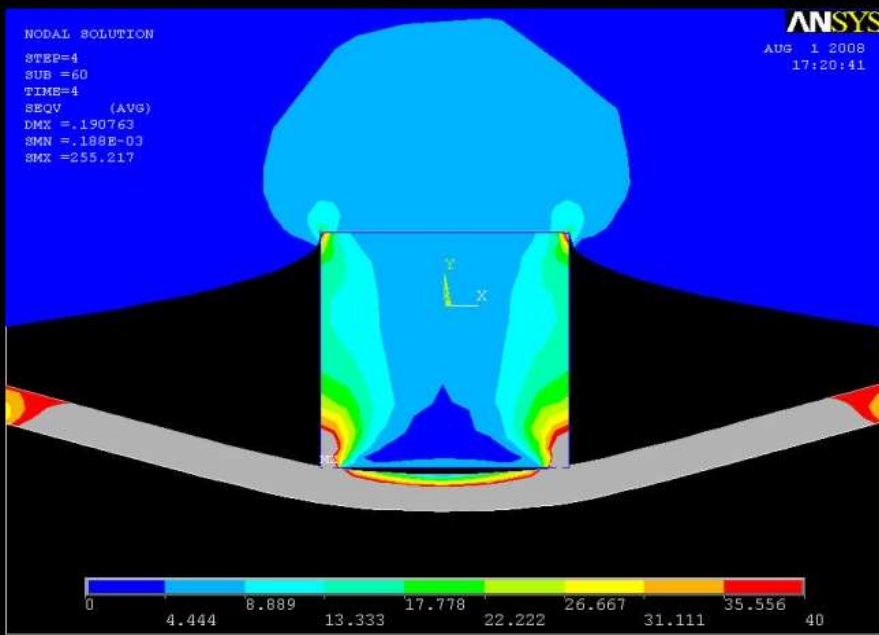
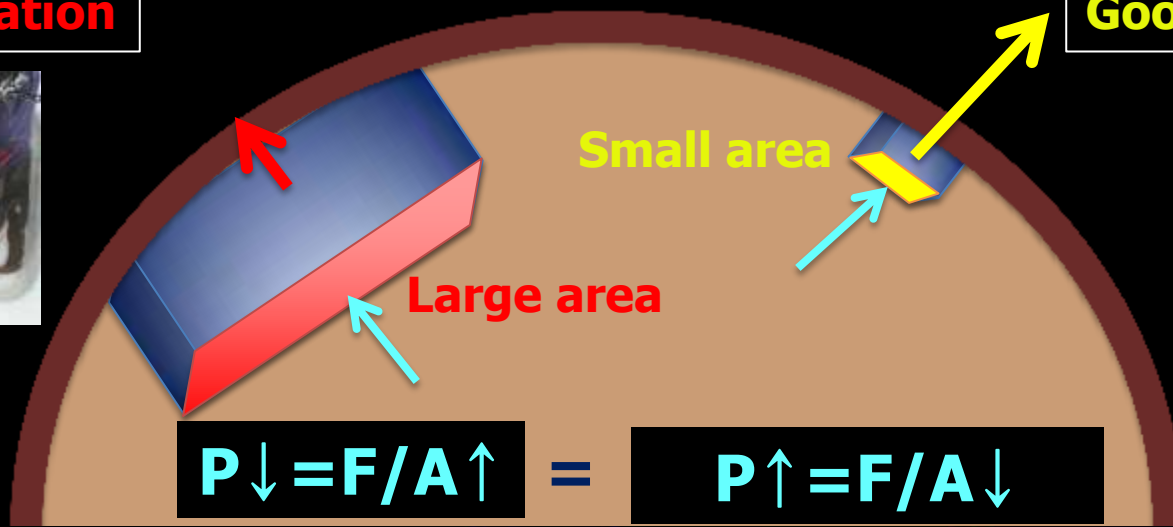
### Xience





**Poor penetration**

**Good penetration**

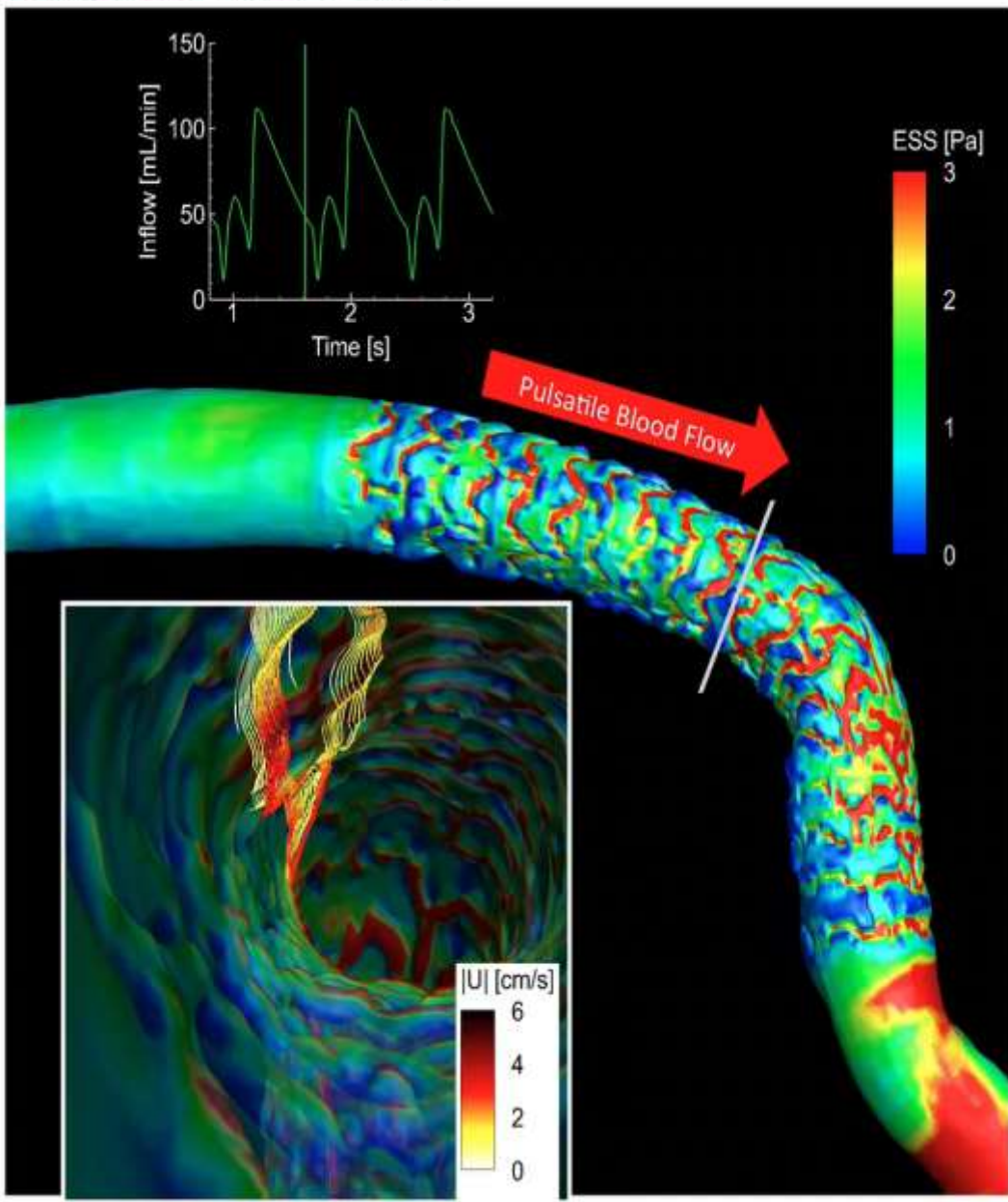


**Large strut area → Poor penetration → Small expansion**

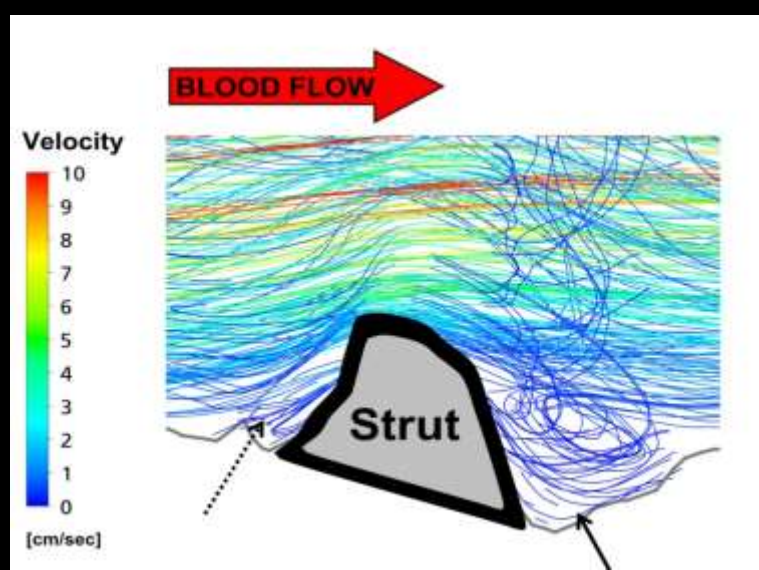
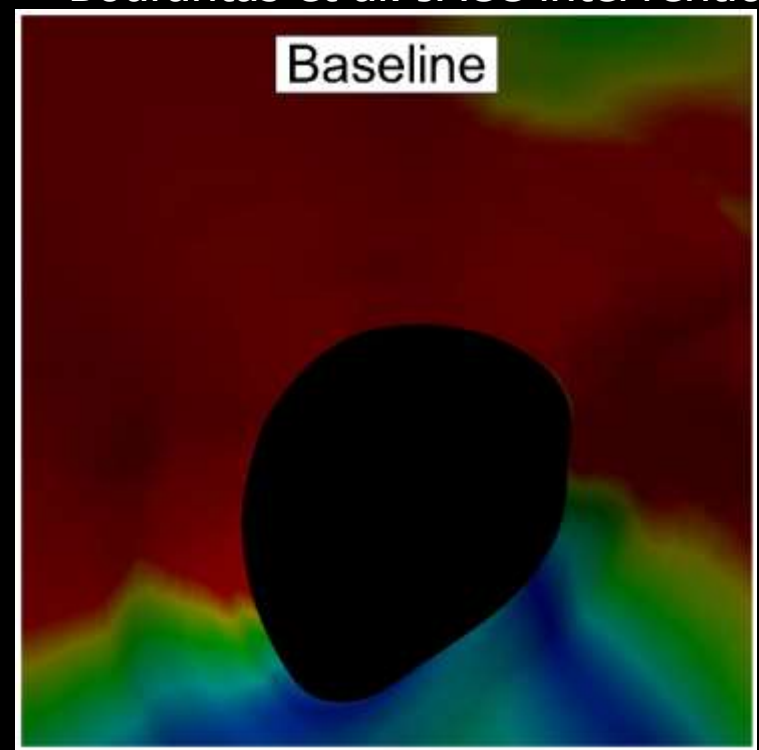
**Small strut area → Good penetration → Large expansion**

# The Nidus for Possible Thrombus Formation

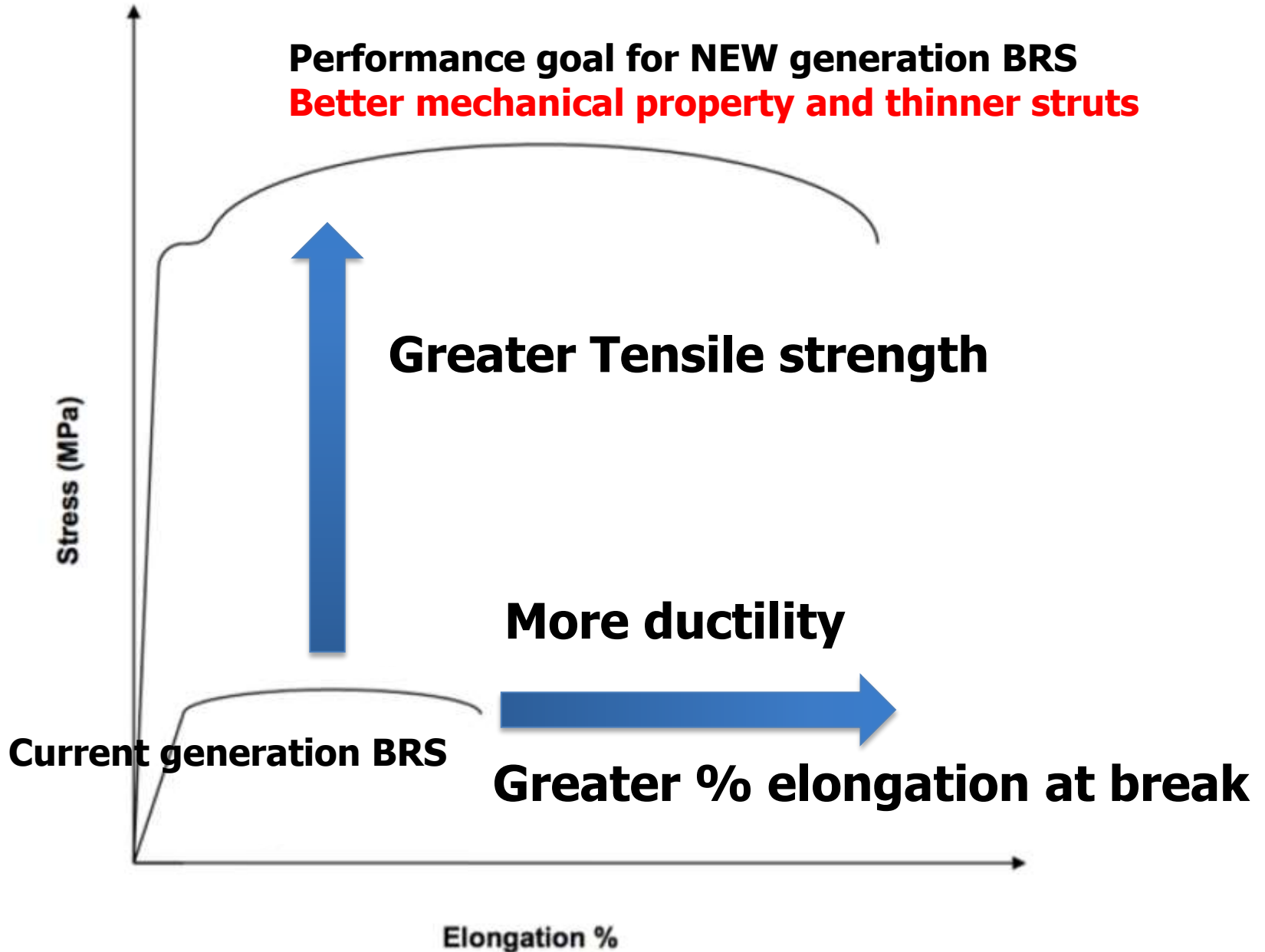
Insight From the Microenvironment of Bioabsorbable Vascular Scaffold



Tenekecioglu et al. JACC intervention 2016  
Bourantas et al. JACC intervention



# Performance goal and mechanical dilemma



# Bioresorbable Scaffolds

From Basic Concept  
to Clinical Applications



Patrick Serruys | Yoshinobu Onuma

**SECTION EDITORS:**

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**Abbott: New generation**  
**Absorb scaffold**

**Arterius**

**Manli**

**Boston Scientific**

**Huaan tech**

**Lepu**

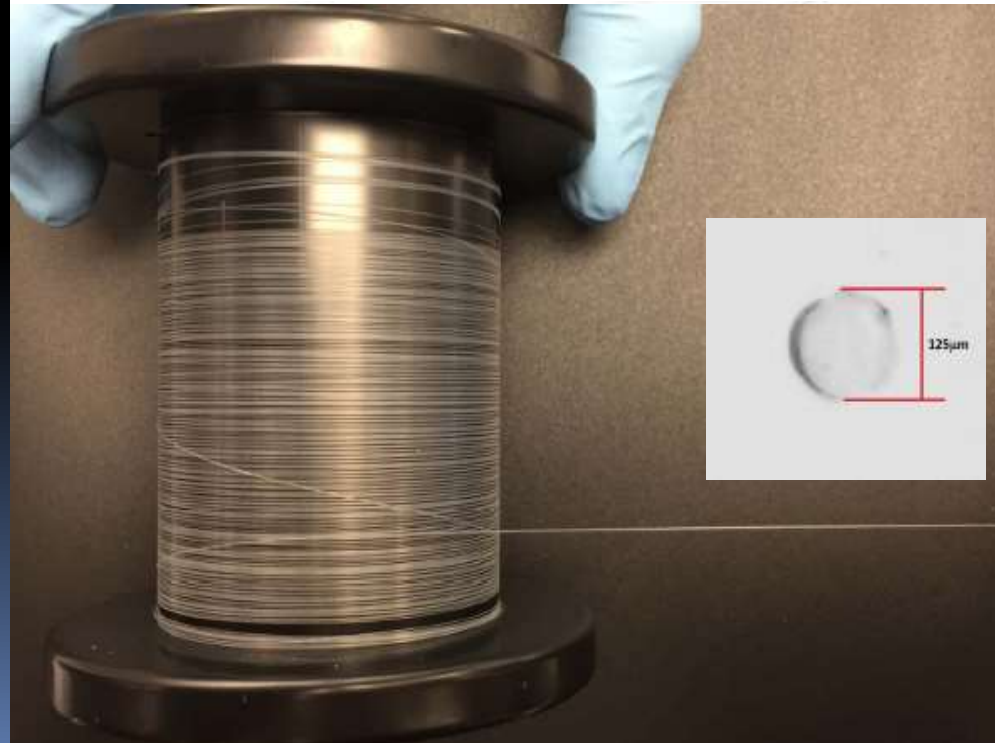
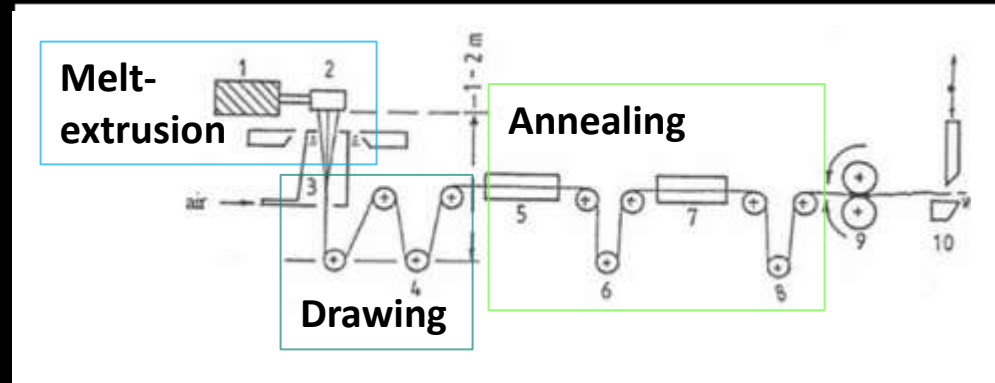


# “Playing” with molecular orientation and mechanical property of PLLA

## e.g. Manli Cardiology’s Microfiber Technology

1. **Highly oriented polylactide constituting a circular monofilament with preferred directional mechanical properties.**
2. **Convert monofilament’s directional mechanical properties into scaffold’s radial mechanical properties.**
3. **Transform circular monofilament into a scaffold with circular strut geometry.**

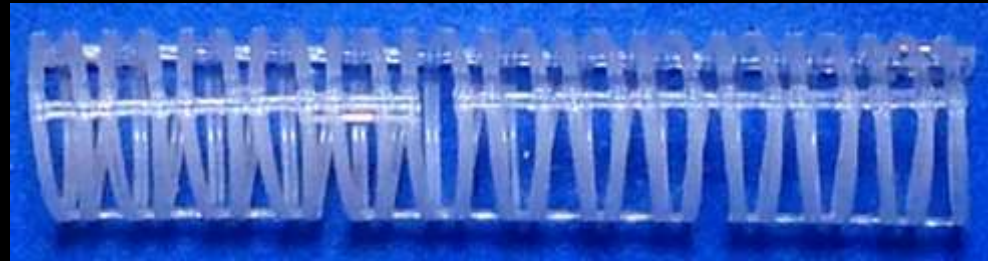
Amorphous Polymer    Oriented Polymer Chain



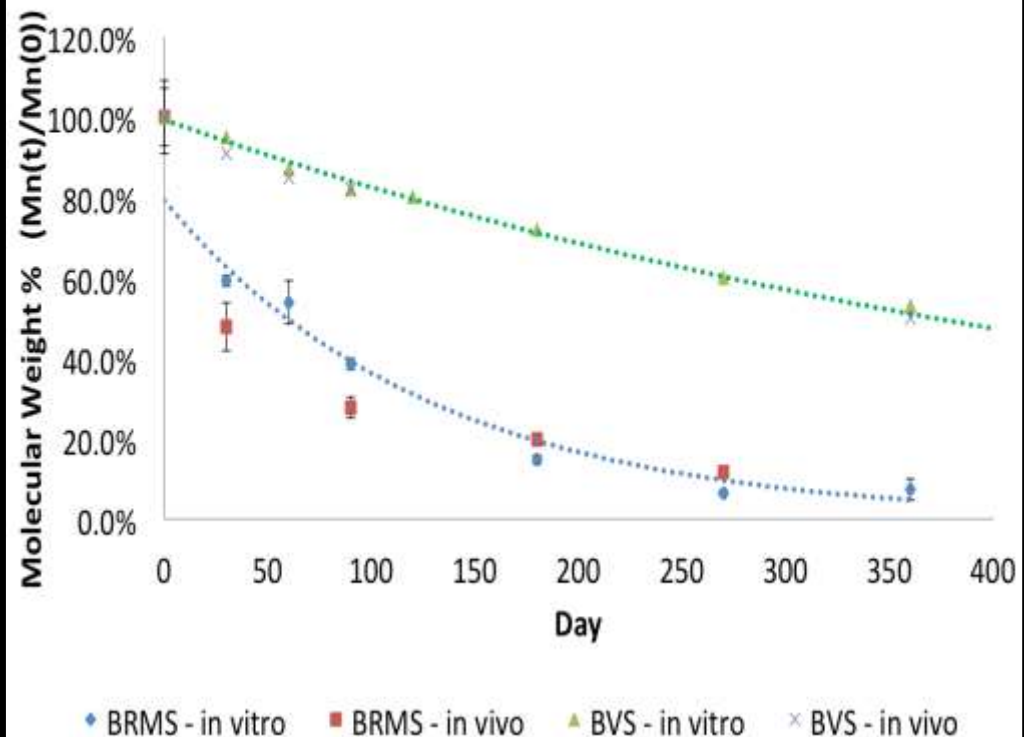


# Manli Cardiology's Microfiber Technology

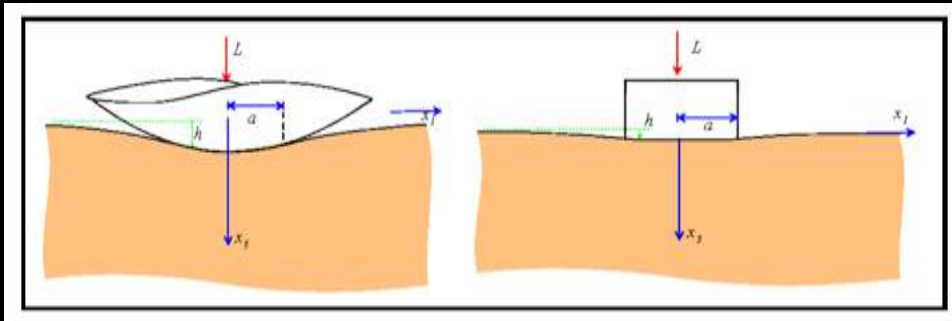
1. Start with highly oriented circular polylactide monofilament with preferred directional mechanical properties.
2. Convert monofilament's directional mechanical properties into scaffold's radial mechanical properties.
3. Make monofilament's circular geometry into scaffold strut's circular geometry.
4. Ambient temperature assembly process



**BRMS MW Degradation Profile**  
*in vitro* and *in vivo*



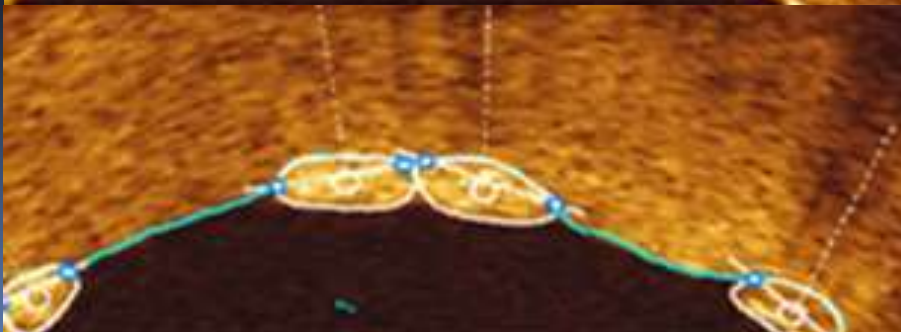
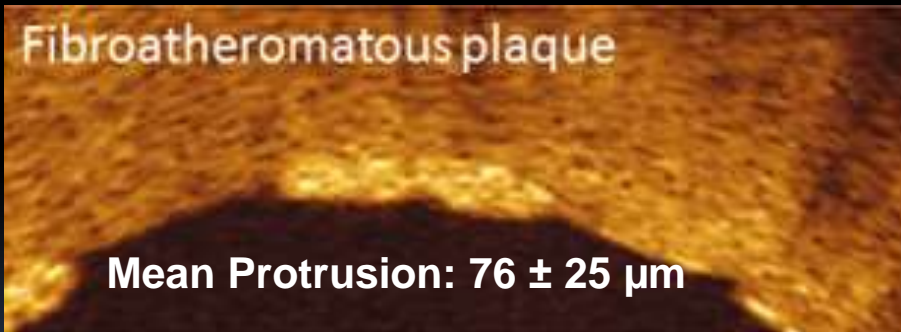
# CIRCULAR STRUTS (mono fiber) PENETRATE INTO THE VESSEL WALL BETTER THAN THE QUADRATIC STRUTS



$$p(\rho) = \frac{2\mu h}{\pi(1-\nu)\sqrt{a^2 - \rho^2}}$$

Axisymmetric contact pressure distribution is in an inverse relation with the initial contact radius (a in the figure).

Green, A.E. and Zerna, W., Theoretical Elasticity. 1968  
 Ting, T. T. C. Anisotropic Elasticity Theory and Applications, 1996





# In a porcine model (n=8), flow and endothelial shear stress simulation differentiated the two devices

Tenekecioglu et al. Int J Cardiovasc Imaging. 2017 Apr 1.

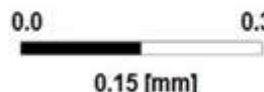
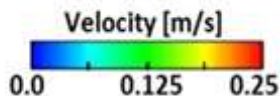
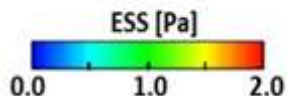
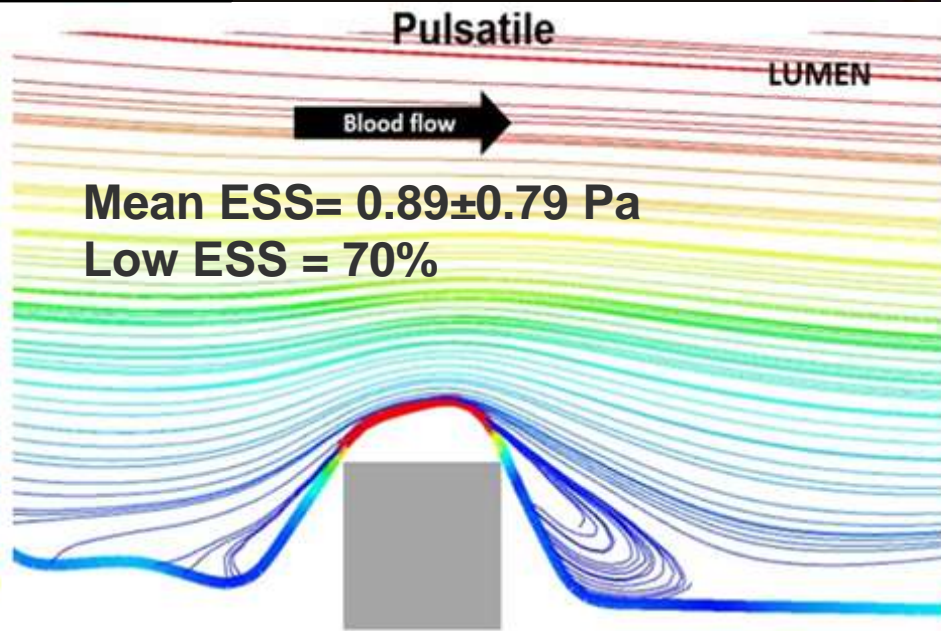
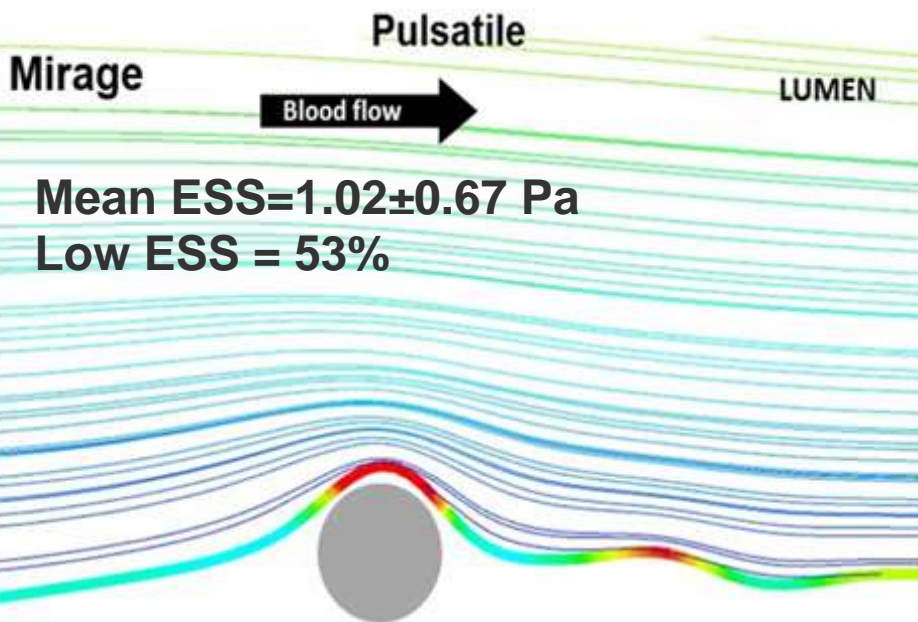
## MIRAGE BRMS (n=11)



## ABSORB BVS (n=6)



Serruys PW, et al. Int J Cardiol. 2017; 227:467-473.



Tenekecioglu, Serruys et al. EuroIntervention;12(10):1296.

Note the intense recirculation area behind the quadratic strut

# Matched OCT Cross-Sections

JACC: CARDIOVASCULAR INTERVENTIONS

VOL. ■, NO. ■, 2017

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ISSN 1936-8798/\$36.00

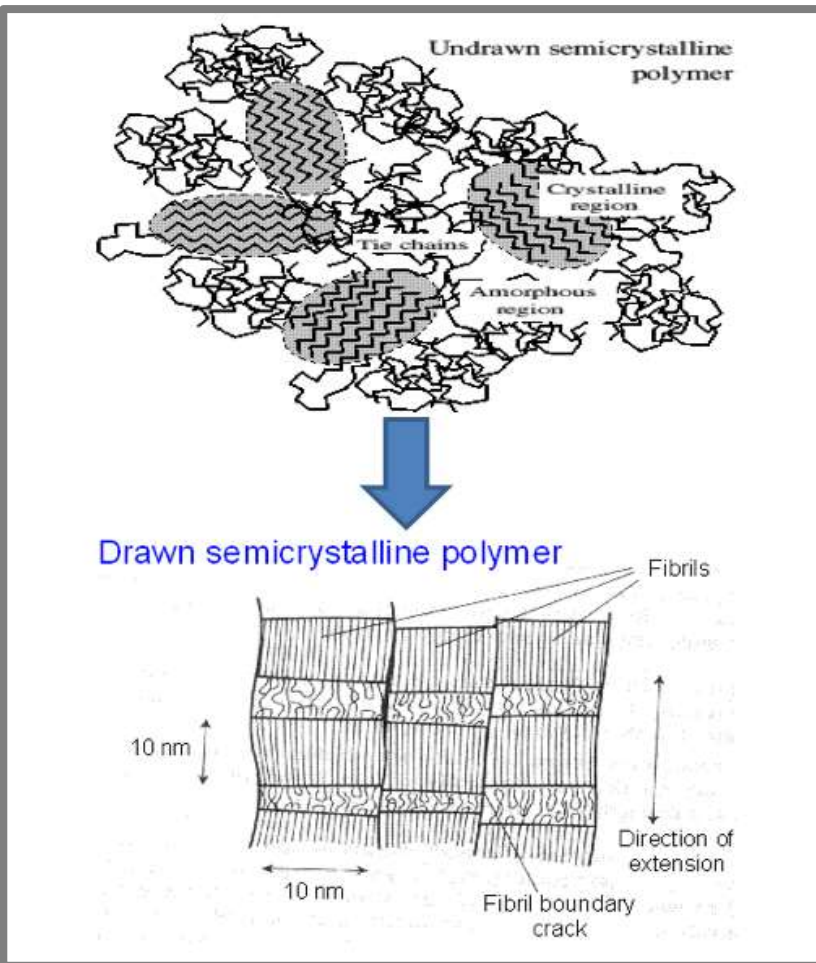
AMERICAN COLLEGE OF CARDIOLOGY FOUNDATION

<http://dx.doi.org/10.1016/j.jcin.2017.03.015>

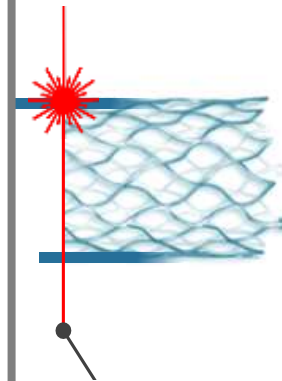
## Randomized Comparison of Absorb Bioresorbable Vascular Scaffold and Mirage Microfiber Sirolimus-Eluting Scaffold Using Multimodality Imaging

Erhan Tenekecioglu, MD,<sup>a</sup> Patrick W. Serruys, MD, PhD,<sup>a,b</sup> Yoshinobu Onuma, MD, PhD,<sup>a</sup> Ricardo Costa, MD,<sup>c</sup>  
Daniel Chamié, MD,<sup>c</sup> Yohei Sotomi, MD,<sup>d</sup> Ting-Bin Yu, PhD,<sup>e</sup> Alexander Abizaid, MD, PhD,<sup>c</sup> Houng-Bang Liew, MD,<sup>f</sup>  
Teguh Santoso, MD, PhD<sup>g</sup>

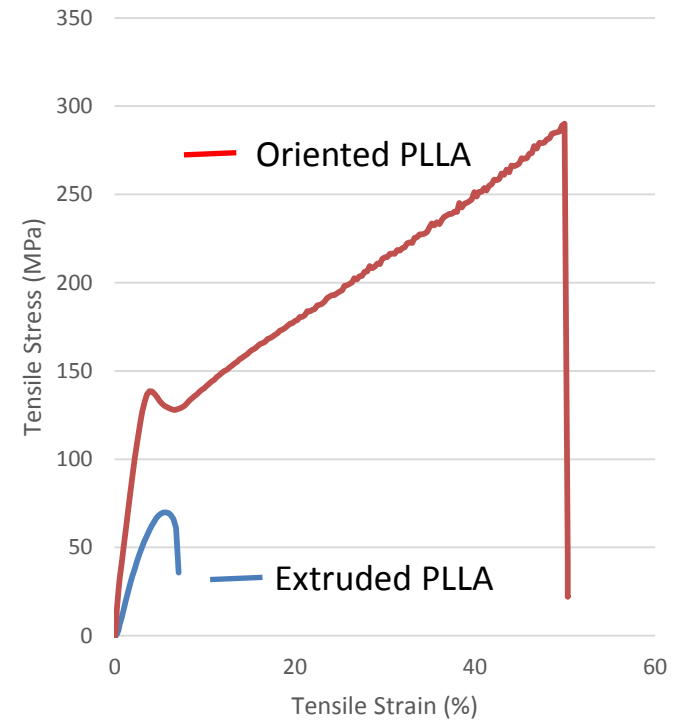
## #2 “Playing” with molecular orientation and mechanical property of PLLA: ArterioSorb™ scaffold of ARTERIUS



Semi-crystalline polymer created by stretching or drawing the fibers



Laser cutting of stent (standard technology)

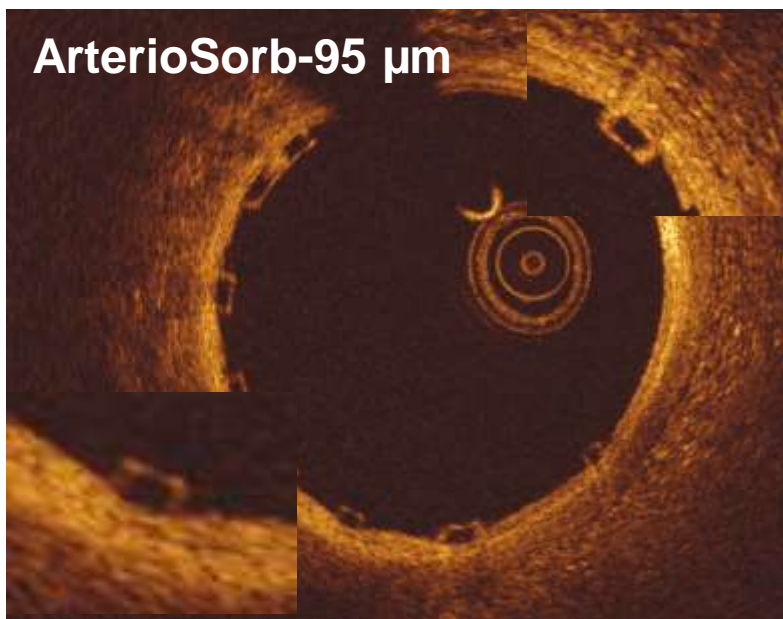


- Tube wall thickness of  $< 95 \mu\text{m}$  can be achieved
- Scaffold tube thickness comparable to metallic DES



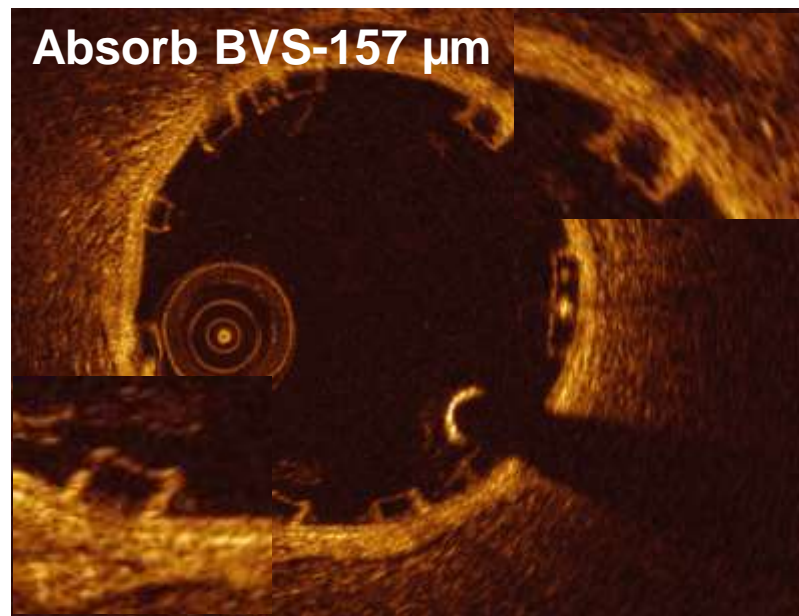
# Reducing the protrusion of the strut (stronger and thinner strut , polylactatide oriented)

Scaffold	Lumen diameter (mm)	Balloon-artery ratio	Scaffold-artery ratio	Acute recoil (%)
Arteriosorb-95 (n=6)	2.97±0.15	1.08±0.06	1.05±0.04	2.7±3.9



Protrusion distance:  $89 \pm 7 \mu\text{m}$

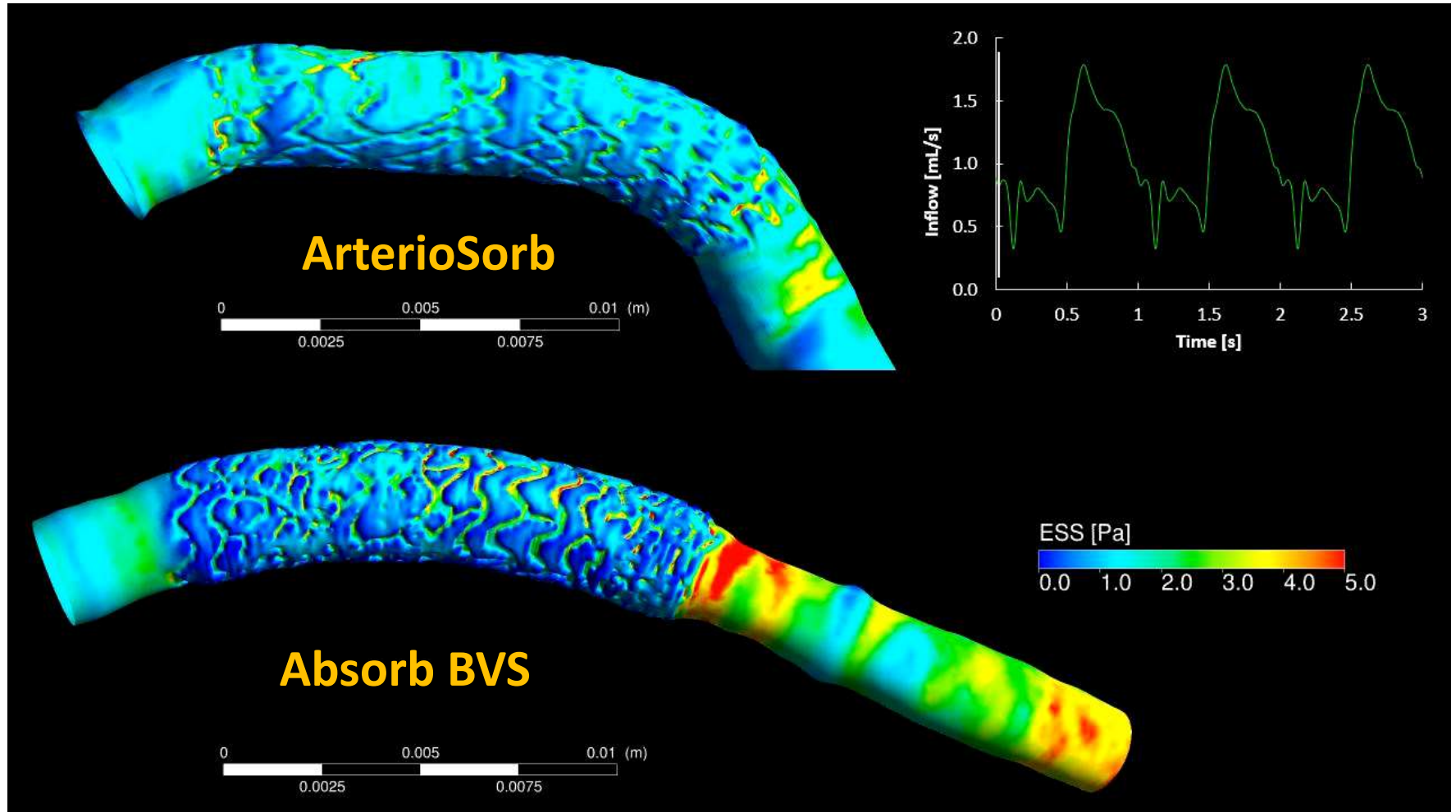
Arteriosorb from Arterius



Protrusion distance:  $150 \pm 9 \mu\text{m}$




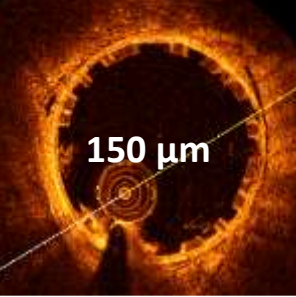


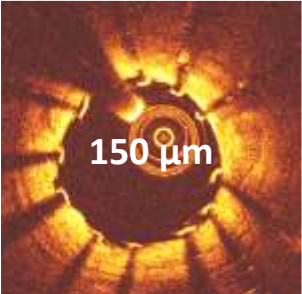
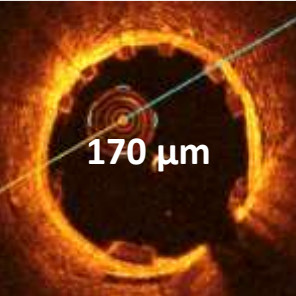
Absorb from Abbot

# Non-Newtonian Pulsatile Simulation of Coronary Flow in Scaffold Implanted Vessel Segments



# Aiming at **thinner struts**

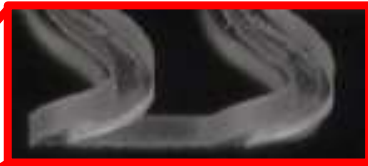
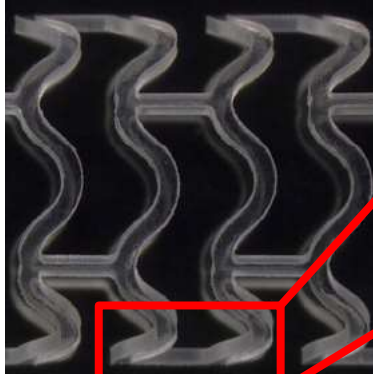
From 150  $\mu\text{m}$  to 100  $\mu\text{m}$ ...

	1 <sup>st</sup> generation BRS	
Scaffold	Absorb BVS 1.1	DESolve
Design		
OCT appearance	 <p>157 <math>\mu\text{m}</math></p>	 <p>150 <math>\mu\text{m}</math></p>
Scaffold	Magmaris	ART
Design		
OCT appearance	 <p>150 <math>\mu\text{m}</math></p>	 <p>170 <math>\mu\text{m}</math></p>

# Next Generation BVS:

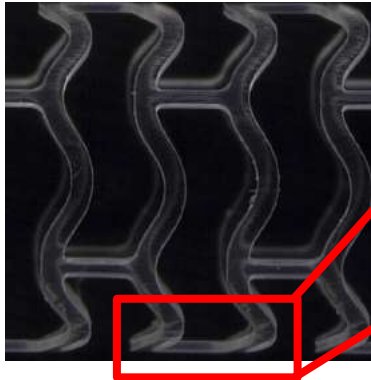
designed to expand the size matrix and Reduce strut thickness

**Absorb GT1™**



Reduced  
strut  
thickness

**Next Gen BVS**



## More Treatment Flexibility

- Broader size matrix, including longer lengths

## Improved Deliverability

- Smaller crossing profile
- **Enhanced catheter**
- **Strut thickness reduced** substantially compared to Absorb GT1™

## Optimized Healing

- Same drug and elution rate as Absorb GT1

# Overview of current status of BRS

Product name	Company	Biodegradable material used for backbone	Coating	Development	Pre-clinical	Clinical	CE mark approved
Absorb	Abbott	PLLA	PDLLA	YES	YES	YES	YES
Absorb GT1	Abbott	PLLA	PDLLA	YES	YES	YES	YES
ART Pure	ART	PDLLA	none	YES	YES	YES	YES
Magmaris	BIOTRONIK	WE43 alloy, 93% Mg, and 7% rare earth elements	PLLA	YES	YES	YES	YES
DESolve 100	Elixir	PLLA	bioresorbable polymer	YES	YES	YES	YES
DESolve 150	Elixir	PLLA	bioresorbable polymer	YES	YES	YES	YES
DESolve XL	Elixir	PLLA	bioresorbable polymer	YES	YES	YES	YES
IGAKI-TAMAI	Kyoto Medical	PLLA	none	YES	YES	YES	YES only for PVD
Fantom	REVA	Desaminotyrosine polycarbonate	Desaminotyrosine polycarbonate	YES	YES	YES	
APTITUDE	Amaranth Medical	PLLA	NA	YES	YES	YES	
FORTITUDE	Amaranth Medical	PLLA	bioresorbable polymer	YES	YES	YES	
FAST	Boston Scientific	PLLA	PLGA	YES	YES	YES	
XINSORB	Huaan	PLA/PCL/PGA	PDLLA+PLLA	YES	YES	YES	
NeoVas	Lepu	PLLA	PDLA	YES	YES	YES	
Mirage	Manli Cardiology	PLLA	PLLA	YES	YES	YES	
MeRes100	Meril	PLLA	PDLLA	YES	YES	YES	
Firesorb	MicroPort	PLLA	PDLLA	YES	YES	YES	
Ideal BioStent	Xenogenics	poly(lactide anhydride mixed with a polymer of salicylic acid with a sebacic acid linker)	Salicilate linked with adipic acid	YES	YES	YES	
ArterioSorb	Arterius	PLLA	Bioresorbable polymer	YES	YES		
ReNATURAL (M)	Cardionovum	(M)=metal, (P)=PLLA	NA	YES	YES		
ReNATURAL (P)							
AMITY	Elixir	PLLA	bioresorbable polymer	YES	YES		
DESolve Cx	Elixir	PLLA	bioresorbable polymer	YES	YES		
IMBIBE	Evison Scientific	magnesium	Nanocarrier layer: Top-coat that comes from the "special" polymer	YES	YES		
LifeTech Iron-based BRS	Life Tech	Nitrided iron		YES	YES		
Mg Spiral	Madtronic	Magnesium	"family of degradable polymers"	YES	YES		
On-AVS	UrbanVed	PLLA/PDLA	PLLA/PDLA	YES	YES		
Unity BRS	QualiMed	Magnesium	PLGA	YES	YES		
Avatar	Scitech	Magnesium	PLGA	YES	YES		
Scitech MBRS	Scitech	Magnesium	NA	YES	YES		
Terumo/ART DCBS	Terumo Corporation	PDLLA	Bioresorbable polymer	YES	YES		
ZMED	Terumo Corporation	Magnesium/PLGA	NA	YES	YES		
Next-Gen Absorb	Abbott	PLLA	PDLLA	YES	YES		
Sahajanand Bioabsorbable	Sahajanand	PLLA	Bioresorbable polymer	YES			
MAGNITUDE	Amaranth Medical	PLLA	Bioresorbable polymer	YES			
Firefalcon	MicroPort	PLLA	NA	YES			
Galaxy	Shanghai Bio-Heart	PLA	Bioresorbable polymer	YES			

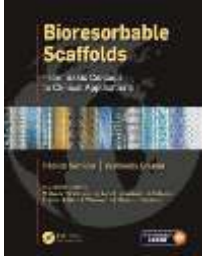
➤ **10 products under evaluation in clinical studies**

➤ **13 products under evaluation in pre-clinical studies**

➤ **5 products still under development**

➤ **28 PLLA products/ 6 magnesium products**





# Summary

- Current version of BRSs still have limited mechanical properties as compared to metallic stents due to its material characteristics. To compensate, the current generation BRS have relatively thick and wide struts.
- To overcome inherent material properties, various modifications to polymer are being attempted. (Stronger and ductile scaffold, Thinner/round struts, Fast resorption without inflammation)
- The development of next generation BRS with thinner struts ( $\leq 100 \mu\text{m}$ ) is ongoing.
- >35 products are currently being in development, or evaluated in pre-clinical and clinical situations.